

Rivacor 3/5/7 ICD Family

VR-T, VR-T DX, DR-T, HF-T, HF-T QP

Function Manual



Table of Contents

1	Characteristics of the ICD Family	3
1.1	Product Description	3
	Intended Medical Use	4
	System Overview	6
	Therapeutic and Diagnostic Functions	14
	Replacement Indications	18
2	Functional Description and Handling	19
2.1	Sensing Functions	19
	Sensing Concept	20
	Automatic Sensitivity Control	21
	Far-Field Protection	24
	Setting sensing parameters	25
2.2	Tachyarrhythmia Detection	28
	General Functional Principles	28
	Detection Algorithms	29
	Detection parameters	46
2.3	Tachyarrhythmia Therapy	
	Status of ICD Therapy	
	Parameters for Tachyarrhythmia Therapy	57
2.4	Bradycardia and Resynchronization Therapy	
	ProgramConsult - selecting programs by indication	
	Pacing Modes	
	Resynchronization Therapy	
	Rate Adaptation	
	Pacing Parameters	
	Timing Functions	
	Attitude vandia Functions	
	Antitachycardia FunctionsPatient Data, Diagnostics, and Home Monitoring	
2.5		
2.5	Home Monitoring Introduction	
	Criteria for the Use of Home Monitoring	
	Home Monitoring Parameters	
	Types of device messages	
	IEGM-Online HD	
2.6	Recordings	
2.0	Objective	

	Recordings, Basics	172
	Memory Management – Details	
	Evaluating Episodes	174
	Evaluating IEGM Episodes	
	Episode List, IEGM Marker Texts	179
	Episode List, Evaluating Details	181
	Evaluating the Shock List	182
	Evaluating the Counter	184
	ATP Statistics	187
2.7	Statistics (Diagnostics)	190
	General Considerations	191
	Statistics Classes	192
	Evaluating Statistics	195
2.8	System Functions	203
	Overview	203
	Tab with Device Name	204
2.9	Follow-Up	206
	Preparing for Follow-Up	207
	Follow-Up Assistant	214
	Performing Manual Follow-Up	223
2.10	ProMRI	249
	Preparing the MRI Scan	249
3	Technical Data	252
3.1	Parameters	252
	Tachycardia	252
	Sensing	257
	Bradycardia/CRT	259
	Home Monitoring	267
	Diagnostics	268
	MRI Program	269
3.2	Technical Data	270
	Mechanical Characteristics	270
	Electrical Characteristics	271
	Battery Data	274
	Legend for the Label	277

1 Characteristics of the ICD Family

1.1 Product Description

Intended Medical Use	. 4
System Overview	. 6
Therapeutic and Diagnostic Functions	14
Replacement Indications	18

Intended Medical Use

Intended use

Rivacor belongs to a family of implantable cardioverter-defibrillators (ICD). The primary objective of the therapy is to prevent sudden cardiac death. Furthermore, the device is capable of treating bradycardia arrhythmias and cardiac resynchronization therapy with multisite ventricular pacing.

ICD implantation as symptomatic therapy has the following objectives:

- Termination of spontaneous ventricular fibrillation (VF) through shock delivery
- Termination of spontaneous ventricular tachycardia (VT) through antitachycardia pacing (ATP); in situations of ineffective ATP or hemodynamically not tolerated VTs, with shock delivery
- Cardiac resynchronization through multisite ventricular pacing (triple-chamber devices)
- Compensation of bradycardia through ventricular (single-chamber devices) or AV sequential pacing (DX, dual- and triple-chamber devices)
 VR-T DX and HF-T/HF-T QP type devices with DX functionality are only indicated for patients that do not require atrial pacing.

Diagnosis and therapy forms

The device monitors the heart rhythm and automatically detects and treats cardiac arrest resulting from ventricular tachyarrhythmia. All major therapeutic approaches from the field of cardiology and electrophysiology are included. BIOTRONIK Home Monitoring gives physicians the ability to manage therapy at any time.

Indications

Rivacor can treat life-threatening ventricular arrhythmias with antitachycardia pacing and defibrillation.

Generally approved differential diagnostics methods, indications, and recommendations for ICD therapy apply to BIOTRONIK devices. See the current guidelines of cardiology associations for guidance.

We recommend observing the indications published by the German Cardiac Society (Deutsche Gesellschaft für Kardiologie, Herz- und Kreislaufforschung, (DGK)) and the European Society of Cardiology (ESC). This also applies to the guidelines published by the Heart Rhythm Society (HRS), the American College of Cardiology (ACC), the American Heart Association (AHA), and other national cardiology associations.

Single-chamber and dual-chamber

Single-chamber and dual-chamber ICDs are indicated for patients with the following risk:

• Sudden cardiac death caused by ventricular arrhythmias

Triple-chamber

Triple-chamber ICDs are indicated for patients with the following risks:

- Sudden cardiac death caused by ventricular arrhythmias
- Congestive heart failure with ventricular asynchrony

Contraindications

Known contraindications:

- Tachyarrhythmia caused by temporary or reversible irritation, e.g., poisoning, electrolyte imbalance, hypoxia, sepsis or acute myocardial infarction
- Very frequent VT or VF requiring therapy causing disproportionately rapid depletion of the device battery
- VT with infrequent, or lack of, clinically relevant symptoms
- VT or VF treatable by surgery
- Concomitant diseases that would substantially limit a positive prognosis
- Accelerated intrinsic rhythm

System Overview

Device family

The complete Rivacor 3/5/7 device family consists of several device types with a DF4/IS-1 or DF4/IS-1/IS4 connection.

The following device variants are available:

Device type	Variants with Home Monitorin	g
Single-chamber	Rivacor 3 VR-T ProMRI Rivacor 5 VR-T ProMRI Rivacor 5 VR-T DX ProMRI Rivacor 7 VR-T ProMRI Rivacor 7 VR-T DX ProMRI	Device type with DF4 connection only
Dual-chamber	Rivacor 3 DR-T ProMRI Rivacor 5 DR-T ProMRI Rivacor 7 DR-T ProMRI	
Triple-chamber	Rivacor 3 HF-T ProMRI Rivacor 3 HF-T QP ProMRI Rivacor 5 HF-T ProMRI Rivacor 5 HF-T QP ProMRI Rivacor 7 HF-T ProMRI Rivacor 7 HF-T QP ProMRI	

Note

Not all device types are included in every device family.

Not all device types are available in every country.

Not all device families and device types are approved in every country.

Not all functions and parameters mentioned in this technical manual are featured in each device type of each device family.

Device

The device's housing is made of biocompatible titanium, welded from the outside and is, therefore, hermetically sealed. The ellipsoid shape facilitates implantation in the pectoral muscle area.

The connections for bipolar pacing and sensing (and unipolar connections for the triple-chamber device) as well as for shock delivery are found in the device header. The two suture holes are used for threading the fixation suture.

The housing serves as a potential antipole during shock delivery or in the case of unipolar lead configuration.

Lead connections

BIOTRONIK offers ICDs with headers for different standardized lead connections.

DF4, DF4/IS-1 and DF4/IS4/IS-1

Note

Suitable leads must comply with the norms.

- A device's DF4 connector port may only be used for connecting leads with DF4 connector that conform to ISO 27186.
- A device's IS4 connector port may only be used for connecting leads with IS4 connector that conform to ISO 27186.
- A device's IS-1 connector port may only be used for connecting leads with IS-1 connector that conform to ISO 5841-3.

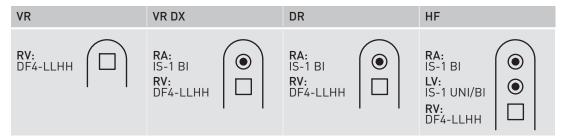
Note

The device and leads have to match.

- Only DX leads for DF4 by BIOTRONIK may be connected to the device type VR DX with DF4.
- When working with DX functionality, DX leads for DF4 by BIOTRONIK may be connected to the device type HF and the device type HF QP with DF4.
- Only quadripolar leads may be connected to the device type HF QP with IS4.

DF4/IS-1

The labeling on each device provides information pertaining to the connector port assignment in the header:



Con- nector port	Lead connect	Configuration or	Implantation site	Device type
RV	DF4	Bipolar and shock coil	Right ventricle	VR, DR, DX, HF
RA	IS-1	Bipolar	Atrium	DR, HF
LV	IS-1	Unipolar, bipolar	Left ventricle	HF

DF4/IS4/IS-1

The labeling on each device provides information pertaining to the connector port assignment in the header:



Con- nector port	Lead connect	Configuration or	Implantation site	Device type
RV	DF4	Bipolar and shock coil	Right ventricle	HF QP
LV	IS4	Unipolar, bipolar	Left ventricle	HF QP
RA	IS-1	Bipolar	Atrium	HF QP

Leads

BIOTRONIK leads are sheathed with biocompatible silicone. They can be flexibly maneuvered, are stable long-term, and are equipped for active or passive fixation. They are implanted using a lead introducer set. Some leads are coated with polyurethane, which is known to increase the sliding properties for the lead. Steroid-eluting leads reduce inflammatory processes. The fractal design of the leads provides for low pacing thresholds.

BIOTRONIK provides a series of adapters to connect a variety of already implanted leads to new devices.

Telemetry

Telemetric communication between the device and the programmer is possible following initialization either by applying the programming head (PGH) to the device or by using wireless wandless telemetry in the programmer.

Programmer

Implantation and follow-ups are performed with the portable BIOTRONIK programmer using PSW software version 1801.A or higher.

The programmer contains an integrated module for wandless telemetry.

Leadless ECG, IEGM, markers and functions are displayed simultaneously on the color display.

The programmer allows for the determination of thresholds and the performance of all tests during an in-office follow-up. In addition, the permanent program can be changed and sent to the implanted device.

Furthermore, the programmer is used to set mode and parameter combinations, as well as for the interrogation and saving of data from the device.

Modes: overview

Note

Not all functions and parameters mentioned in this technical manual are featured in every device type of each device family.

Note

CLS modes are only available in Series 7 devices.

Note

The mode that should be programmed depends on the individual diagnosis. The possible modes that can be programmed specific to each device type are listed in the tables with the order numbers.

Series 3:

Device type	Pacing modes	Standard
VR	VVI; VVIR; V00; OFF	VVI
DR, HF (QP)	DDD; DDDR; DDI; DDIR; D00; VDD; VDDR; VDI; VDIR; VVI; VVIR; V00; AAI; AAIR; OFF	DDD

Series 5:

Device type	Pacing modes	Standard
VR	VVI; VVIR; V00; OFF	VVI
VR DX	VDD; VDDR; VDI; VDIR; VVI; VVIR; V00; OFF	VVI
DR, HF (QP)	DDD; DDDR; DDD-ADI; DDDR-ADIR; DDI; DDIR; D00; VDD; VDDR; VDI; VDIR; VVI; VVIR; V00; AAI; AAIR; OFF	DDD

Series 7:

Device type	Pacing modes	Standard
VR	VVI-CLS; VVI; VVIR; V00; OFF	VVI
VR DX	VDD; VDDR; VDI; VDIR; VVI-CLS; VVI; VVIR; V00; OFF	VVI
DR, HF (QP)	DDD-CLS; DDD; DDDR; DDD-ADI; DDDR-ADIR; DDI; DDIR; D00; VDD; VDDR; VDI; VDIR; VVI- CLS; VVI; VVIR; V00; AAI; AAIR; OFF	DDD

NBD and **NBG** codes

V	Shock	in	the	ventricle

V	Antitachycardia pacing (ATP) in the ventricle
Е	Detection via IEGM analysis

VDE is the NBD code for the antitachycardia pacing mode of the dual-chamber and triple-chamber devices with atrial therapy:

V	Shock in the ventricle
D	Antitachycardia pacing (ATP) in the atrium and ventricle
Ε	Detection via IEGM analysis

DDDR is the NBG code for the antibradycardia pacing mode of the dual-chamber device:

- D Pacing in the atrium and ventricle
- D Sensing in the atrium and ventricle
- D Pulse inhibition and pulse triggering
- R Rate adaptation

DDDRV is the NBG code for the antibradycardia pacing mode of the triple-chamber device:

- D Pacing in the atrium and ventricle
- D Sensing in the atrium and ventricle
- D Pulse inhibition and pulse triggering
- R Rate adaptation
- V Multisite pacing in both ventricles

VDDR is the NBG code for the antibradycardia mode of the single-chamber type DX device:

- V Pacing in the ventricle
- D Sensing in the atrium and ventricle
- D Pulse inhibition and pulse triggering
- R Rate adaptation

WIR is the NBG code for the antibradycardia modes of the single-chamber device:

- V Pacing in the ventricle
- V Sensing in the ventricle
- I Pulse inhibition in the ventricle
- R Rate adaptation

BIOTRONIK Home Monitoring®

In addition to effective pacing therapy, BIOTRONIK provides a complete therapy management system:

- With Home Monitoring, diagnostic and therapeutic information, as well as technical data of the device, are automatically and wirelessly sent to a transmitter via an antenna in the device header. The data is encrypted and sent from the transmitter to the BIOTRONIK Service Center via the cellular phone network.
- The received data is deciphered and evaluated. Each physician can set the criteria for evaluation to be used for each patient and can configure the time of notification via e-mail or SMS.
- A clear overview of the results of this analysis is displayed for the attending physicians on the protected Internet platform Home Monitoring Service Center (HMSC).
- Data transmission from the device is performed with a daily device message.
- Device messages that indicate particular cardiac or device-related events are transmitted immediately.
- A test message can be initiated at any time using the programmer to immediately check the Home Monitoring function.

Rivacor order numbers

Not all device types are available in every country:

Rivacor series 3

Device type	Lead connection	Number of connector ports	Mode	Order number
VR-T	DF4	1	VVE-VVIR	429574
DR-T	DF4/IS-1	2	VVE-DDDR	429573
HF-T	DF4/IS-1/IS-1	3	VVE-DDDRV	429572
HF-T QP	DF4/IS4/IS-1	3	VVE-DDDRV	429571

Rivacor series 5

Device type	Lead connection	Number of connector ports	Mode	Order number
VR-T	DF4	1	VVE-VVIR	429565
VR-T DX	DF4/IS-1	2	VVE-VDDR	429564
DR-T	DF4/IS-1	2	VVE-DDDR	429563
HF-T	DF4/IS-1/IS-1	3	VVE-DDDRV	429562
HF-T QP	DF4/IS4/IS-1	3	VVE-DDDRV	429561

Rivacor series 7

Device type	Lead connection	Number of connector ports	Mode	Order number
VR-T	DF4	1	VVE-VVIR	429536
VR-T DX	DF4/IS-1	2	VVE-VDDR	429535
DR-T	DF4/IS-1	2	VDE-DDDR	429534
HF-T	DF4/IS-1/IS-1	3	VDE-DDDRV	429533
HF-T QP	DF4/IS4/IS-1	3	VDE-DDDRV	429532

Package contents

The storage package includes the following:

- Sterile packaging with device
- Serial number label
- Patient ID card
- Warranty booklet

Note

The technical manual pertaining to the device is either included in hard copy form in the storage package or is available in digital form on the internet.

The sterile packaging includes the following:

- Device, blind plugs (if applicable)
- Screwdriver

Therapeutic and Diagnostic Functions

Diagnostic functions

- Data from implantation and the most recent interrogations and follow-ups, as well as arrhythmia episodes, are recorded; they are stored with other data to assess the patient's condition and the device status at any time.
- To check proper lead function, an automatic impedance measurement is performed in the device using sub-threshold pulses. Continuous impedance measurements of the shock paths and the pacing polarities of the RV lead improve the determination of lead failures.
- Leadless ECG function: For all device types, far-field derivation can be measured without external leads between the right ventricular distal shock coil and housing, which, depending on the implantation site, corresponds to ECG lead II or III (Einthoven).
- When telemetry connection has been established during a test procedure in an in-office follow-up, the leadless ECG and the IEGM are displayed with markers.

Antitachycardia pacing

- The ICD can treat ventricular tachycardia with antitachycardia pacing (ATP);
 ATP can also be delivered in the VF zone (ATP One Shot) when the stability criterion (monomorphic rapid VTs) is met before shock delivery.
- The ICD can also respond to atrial tachycardia with antitachycardia pacing (ATP) in case of stable heart rhythms or with high-rate pacing (HF bursts) in case of unstable heart rhythms.
- Depending on the device type, the device software not only contains the ICD functions, but also all pacemaker functions, for 1, 2 or 3 chambers. The heart rhythm is continuously monitored; each arrhythmia is classified according to the heart rate and the adjustable detection criteria. Depending on the preset values, antibradycardia as well as antitachycardia therapy is inhibited or delivered.

Cardioversion, defibrillation

- The ICD can treat ventricular tachyarrhythmia with cardioversion and/or defibrillation. Shock polarity and energy can be programmed individually. Shock energies between 2.0 J and 40 J are possible. Before delivery of the shock, the ICD can be set to only deliver a shock when ongoing tachyarrhythmia is confirmed. During this time period, the device can identify spontaneous conversion of the tachyarrhythmia and abort the charge if necessary.
- The shock paths can be set between the different shock coils (SVC/RV) and/or the housing.

Antibradycardia pacing

- Rate hysteresis, automatic sensor functions, and a night program promote the patient's intrinsic rhythm, avoid overdrive pacing, and facilitate adaptation of the device to the individual needs of the patient.
- Both atrial and ventricular thresholds can be determined automatically in the
 device. Additionally, (not applicable to Series 3), capture control is used to set
 the pulse amplitudes so that pacing is performed with the optimum atrial and
 ventricular amplitude for patients with each change of the pacing threshold.
- Setting an upper rate for the atrium prevents unspecific atrial pacing, thus reducing the risk of pacemaker-mediated tachycardias.
- Positive AV hysteresis functions support the physiological contraction sequence by promoting intrinsic conduction. Negative AV hysteresis functions support the cardiac resynchronization therapy by maintaining pacing during stress situations.
- Additional, special form of rate adaptation with devices from series 7: An
 increased cardiac output requirement is detected using physiological
 impedance measurements. The measuring principle is based on contractile
 changes (ionotropy) of the myocardium (CLS function: closed loop
 stimulation). Rate adaptation is automatically initialized and optimized in CLS
 mode
- Ventricular pacing suppression with devices from Series 5 and 7: Unnecessary ventricular pacing is avoided by promoting intrinsic conduction (Vp suppression function). The device can thereby adapt to conduction changes and switch between an ADI(R) and a DDD(R) mode.

Cardiac resynchronization therapy

- For resynchronization of the ventricles, triple-chamber devices have functions for multisite ventricular pacing with possible VV delays in either direction.
- To ensure that no additional surgery is necessary in case of a left-sided increase of pacing threshold or undesired phrenic nerve stimulation, different pacing polarities can be set for the left ventricular lead with a triple-chamber device. Up to 20 vectors are available with the HF QP device type.
- With the HF QP device type of Series 7: Two stimuli can be configured for the left ventricle to improve the resynchronization of the ventricles. The stimuli can be delivered sequentially or simultaneously.
- The effectiveness of resynchronization can be improved if intrinsic AV delays exist: The function CRT AutoAdapt measures the intracardiac conduction times every minute, sets up the pacing configuration on BiV or LV (with activated LV capture control) and adapts the AV delay automatically.

Storing programs

There are different therapy programs:

- For the most common pacemaker indications there are preset parameters (ProgramConsult).
- Up to 3 therapy programs can be stored for individual parameter settings.

ProMRI devices recognize magnetic resonance imaging scanners

The static magnetic field of an MRI scanner is reliably recognized with the aid of a sensor. The sensor can be activated for a maximum of 14 days using the MRI AutoDetect function during an in-office follow-up.

If the patient is in the vicinity of an MRI scanner during the programmed time duration, the device recognizes the static magnetic field and automatically activates the preset MRI program. Reprogramming to the permanent program also occurs automatically when the patient leaves the scanner.

Home Monitoring functions

- The device automatically sends information to the transmitter once a day. It
 also sends messages related to events, which are immediately forwarded to
 the Home Monitoring Service Center (HMSC). In addition, test messages can
 be initiated using the programmer.
- Important medical information in the device messages include the following:
 - Atrial and ventricular arrhythmias
 - Parameters relevant to leads in the atrium and ventricle: pacing thresholds, sensing amplitudes, impedances
 - Current statistics
 - IEGM Online HD with up to 3 high-definition channels
- The following remote functions are possible via the Home Monitoring Service Center:
 - Appointments for Home Monitoring-supported follow-ups can be scheduled.
 - Applies to series 7: Current device data can be requested by the
 Home Monitoring Service Center using the QuickCheck function. Provided
 that the patient is in the vicinity of the CardioMessenger transmitter, the
 usual data for a Home Monitoring-supported follow-up is compiled, an
 IEGM is added, and data transfer takes place in a timely manner. This
 process is called "interrogation-on-demand" and normally runs within a
 maximum of 15 minutes.

Replacement Indications

Possible battery levels

- BOS: Beginning of Service: > 90% charge
- ERI: Elective Replacement Indication (i.e., RRT: Recommended Replacement
- EOS: End of Service

Elective Replacement Indication (ERI)

Elective Replacement Indication can be detected by Home Monitoring.

Caution

Temporally limited therapy

If ERI occurs shortly after follow-up and is only detected during the subsequent follow-up, then the remaining service time can be much less than 3 months.

- Replace device soon.
- The device can monitor the heart rhythm for at least 3 more months.
- At least 6 maximum energy shocks can be delivered until EOS occurs.
- The set parameters in the device do not change.

EOS replacement indication

End of Service can be detected by Home Monitoring.

★ WARNING

Patient at risk of death

If EOS replacement indication occurs before replacement of the device, then the patient is without therapy.

- Replace device immediately.
- Monitor patient constantly until immediate replacement of the device!
- VT and VF detection and all therapies are deactivated!
- The antibradycardia function remains active in the WI mode:
 - Ventricular pacing: RV; basic rate 50 bpm; without special pacemaker functions such as hysteresis, etc.
 - Pulse amplitude of 6 V; pulse width of 1.5 ms
 - Cycle duration for BIOTRONIK Home Monitoring: 90 days

2 Functional Description and Handling

2.1 Sensing Functions

Sensing Concept	20
Automatic Sensitivity Control	21
Far-Field Protection	24
Setting sensing parameters	25

Sensing Concept

Function

The device continuously analyzes the heart rate in order to be able to initiate suitable therapy when necessary.

In order to do this, the leads in the atrium and ventricle sense P and R waves.

The scan rate is 128 Hz.

The device uses various criteria to determine whether or not an arrhythmia has to be treated (detection). For example, sinus tachycardias or supraventricular tachycardias are arrhythmias that do not require therapy. This prevents exposing the patient to inadequate therapy.

- Sensing in the atrium: devices of type VR-T DX, DR, and HF
- Sensing in the right ventricle: devices of type VR, VR-T DX, DR, and HF
- Sensing in the left ventricle: HF devices

Note

Proper sensing by the ICD is required for safe and effective implementation.

Measurement of the P and R amplitudes should be performed again subsequent to each modification of the input stage settings. This ensures that the signals suffice for adequate detection of tachycardias. It may be necessary to carry out another DFT test to verify the effectiveness of the modified sensing settings.

Note

If no atrial or left ventricular lead is connected, sensing must be deactivated in these chambers.

If atrial or left ventricular sensing is deactivated, then IEGM transmission and recordings are also deactivated in these chambers.

Left ventricular sensing

Left ventricular sensing is only evaluated for:

- IEGM recordings
- LV T-wave protection
- Event statistics
- CRT AutoAdapt

Left ventricular sensing is not evaluated for VT/VF detection and timing of pacemaker functions.

Automatic Sensitivity Control

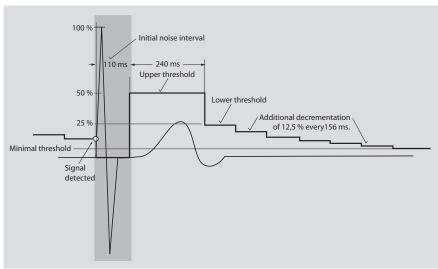
The input stages of the ICD are adjusted to signal sensing in the range between sinus rhythm, atrial fibrillation and ventricular fibrillation. Noise is suppressed during signal sensing.

Sensitivity in the atrium, the left and the right ventricle can be adjusted separately.

The standard settings are adequate for most signals experienced in practice.

If the standard settings are not sufficient for sensing and assessing signals adequately, then fine tuning can be carried out for each chamber using the [Show sensing expert parameters] function.

Automatic sensitivity control



Technical principle

Automatic sensitivity control is based on the principle of having two adaptive thresholds.

As part of the standard settings, the upper threshold is calculated as 50% of the R amplitude and the lower threshold is calculated as 25% of the R amplitude in the ventricle based on a sensed R wave.

After a sensed event, the upper threshold, 50% of the previous R amplitude, is active for the upper threshold duration of 350 ms following a sensed event and 400 ms following a paced event so that no T waves are sensed in the ventricle. A lower sensitivity is effective during the waiting period of the T wave following delivery of pace.

After the upper threshold duration of 350 ms after a sensed event and 400 ms after a paced event, the signal sensing is switched with increased sensitivity to the lower threshold at 25% of the previous R amplitude so that a subsequent fibrillation event with a low amplitude can be sensed.

In beat-to-beat adjustment, each sensed amplitude is measured again and the upper and lower thresholds are set again accordingly.

A minimum threshold can be set to prevent signal noise if sensitivity is too high. This limits a decrease in the threshold in the case of low amplitudes and thus prevents noise.

Settings

When clinically applied, it is easy to have sensitivity controlled automatically by selecting predefined settings:

- Standard
- Enhanced T-wave suppression
- Enhanced VF sensitivity

Sensing is adjusted individually as soon as the **[Show sensing expert parameters]** function is selected and a parameter is reprogrammed.

Standard

This setting is recommended for patients, for whom an R amplitude over $3\,\mathrm{mV}$ has been measured with the device in the standard setting.

Enhanced T-wave suppression (TWS)

Note

Set enhanced T-wave suppression only if T-wave oversensing occurs frequently and regularly.

Enhanced T-wave suppression is especially effective due to more narrowly defined values. At the same time, the upper threshold is increased to 75% of the measured R wave.

Enhanced T-wave suppression is less suitable in cases of sinus rhythm with low signal amplitudes (< 3 mV) or cases of ventricular fibrillation signals with highly fluctuating signal amplitudes, because R amplitudes that are too low accompanied by low-frequency signal components can additionally be restricted due to the stricter filter range.

For patients with long QT syndrome, the upper threshold duration after sensing can be extended from 350 ms to 500 ms. This serves to prevent switching to the lower threshold too early during the escape time of the delayed T wave.

Enhanced VF sensitivity (VFS)

The enhanced VF sensitivity setting enhances VF detection, especially in cases of highly fluctuating VF signal amplitudes.

This setting is recommended if the VF detection time exceeds 5–6 seconds due to intermittent marker failures.

This setting is less suitable for patients with large T waves. Enhanced VF sensitivity is achieved by way of a shortened upper threshold duration after detection and pacing as compared to the standard setting. Thus, the upper threshold is left prematurely.

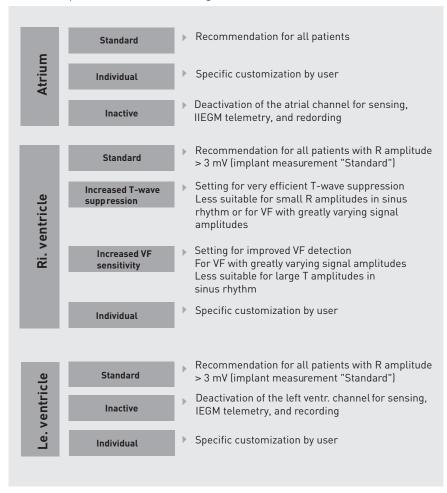
Detection features

The input stage is effective due to the following features:

- High resolution of amplitudes up to 25 mV
- Fast adaptation of sensitivity due to non-linear decrement

Parameter sets

Predefined parameter sets for sensing



Far-Field Protection

Function

Far-field protection prevents spontaneous or paced ventricular events from being incorrectly sensed in the atrium.

Blanking periods follow atrial and ventricular events to guarantee adequate sensing.

The following functions determine the blanking periods in the atrium:

- Far-field protection after Vp (VA-cross blank after Vp)
- Far-field protection after Vs (far-field blanking)
- Blanking after atrial pacing

Far-field sensing from the ventricular channel can cause problems with mode switching and during rhythm evaluation by SMART.

The setting Refractory period/Blanking \rightarrow Far-field protection after Vs \rightarrow AUTO optimizes the sensing behaviour when VT/VF events occur. See Optimization of SVT sensing using automatic far-field protection [Page 38].

Therefore, preventing far-field sensing is especially important.

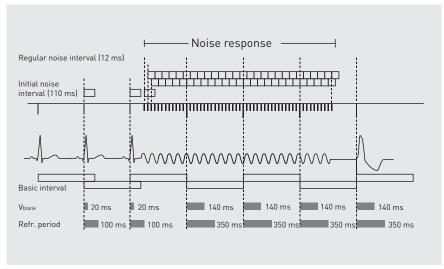
A blanking period is also initiated in the ventricle after atrial pacing to prevent farfield sensing in the ventricle. The user can adjust the value for the right ventricle and the value for the left ventricle as fixed.

Note

Sensed events within an interference interval are not evaluated as tachycardia rates. If a sensed event occurs in an initial noise interval (110 ms), the regular noise interval (12 ms) is started subsequently. The interference interval can be retriggered.

Constantly restarting the interference interval leads to asynchronous pacing.

Noise response



Setting sensing parameters

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Sensing

Objective

Differentiated setting of the sensing function serves the following purposes:

- Setting the input stage sensitivity of the respective channel
- Activating or deactivating sensing in the respective channel, e.g. in the left ventricle
- Setting the minimum sensing threshold

Sensing in the atrium

The following parameters can be set for sensing in the atrium:

Channel	Setting	Description
Atrium	Standard (Std.)	The standard setting for sensing in the atrial channel has been selected.
	Disabled (OFF)	This setting disables sensing, real-time IEGM, and recording in the atrial channel for diagnostic purposes.

Sensing in the ventricle

The following parameters can be set for sensing in the ventricle:

Channel	Setting	Description
Right ventricle	Standard (Std.)	The standard setting for sensing in the right ventricular channel has been selected.
	Enhanced T- wave suppres- sion (TWS)	This setting causes T-wave sensing to be severely suppressed.
		However, this setting is not particularly beneficial for a sinus rhythm with low signal amplitudes and a VF with strongly fluctuating signal amplitudes.
	Enhanced VF sensitivity (VFS)	This setting enhances VF detection, especially in cases of strongly fluctuating signal amplitudes. However, this setting is less suitable for a sinus rhythm with high T wave amplitudes.
	Individual (Ind.)	This setting is displayed by the system if the parameters for the sensing function differ from standard settings – or in other words have been changed individually.

Channel	Setting	Description
Left ventricle	Standard (Std.)	The standard setting for the left ventricular lead has been selected.
	<pre>Individual (Ind.)</pre>	This setting is displayed by the system if the parameters for the sensing function differ from standard settings – or in other words have been changed individually.
	Disabled (OFF)	In this setting, sensing, real-time IEGM, and recording for diagnostic purposes are disabled in the left ventricular channel.

Parameters for thresholds

The following parameters can be set for sensing thresholds:

Parameter	Description
Upper threshold	The relationship expressed as a percentage of the upper threshold with the maximum measured amplitude; amplitudes below this threshold are not evaluated.
Upper threshold duration after sens.	The interval within which the upper threshold is retained as the sensing threshold; amplitudes below this threshold are not evaluated.
Upper threshold duration after pacing	
Lower threshold RV	The relationship expressed as a percentage of the lower threshold with the maximum measured amplitude; amplitudes below this threshold are not evaluated.
Post pace T- wave suppres- sion	Altered sensitivity for the defined time period.

Parameters for blanking periods

The following parameters can be set for the blanking periods:

Blanking	Description
after atrial pace	After atrial pacing, sensing of signals in the RV and LV is suppressed.
after RV pace	After right ventricular pacing, the sensing of signals in the right ventricle (in-channel blanking) is suppressed, and also for the left ventricle (cross channel blanking) in the case of triple-chamber devices.
after LV pace	For triple-chamber devices, after left ventricular pacing, the sensing of signals in the left (in-channel blanking) and also in the right ventricle (cross channel blanking) is suppressed.

DX sensing

A DX lead can be connected to triple-chamber devices. To do this, DX sensing must be switched on.

Note

Before switching on DX $\,$ sensing, make sure that a DX lead is connected to the device.

Minimum threshold

The set value determines the minimum sensitivity at which signals are sensed. The minimum threshold is the absolute lower limit. The upper and lower thresholds are the boundaries for evaluating P and R waves from beat to beat, between maximum amplitude and minimum threshold. See also: Parameters for thresholds [Page 26] and Parameters for blanking periods [Page 27].

General Functional Principles

The ICD differentiates, depending on the frequency, between sinus rhythm, atrial and ventricular fibrillation, as well as fast and slow tachycardia in the ventricle.

Each arrhythmia zone has a configurable frequency range. This range extends from the lower frequency of a zone to the lower frequency of the next higher zone, whereby the arrhythmia zones overlap. A therapy sequence is mapped to each zone.

A VT1 zone can also be programmed without therapy, so that the episodes are recorded in this rate range only for diagnostic purposes (monitoring zone).

In addition to the ventricular arrhythmia zone, an atrial AT/AF arrhythmia zone can also be configured with the ICD, which can be assigned to the atrial therapy zones.

Ventricular detection always takes precedence over the atrial detection.

Detection Algorithms

Ventricular tachycardia detection

The ICD classifies an RR interval as tachycardic using the criteria rate (bpm) or interval (ms) in the VT/VF zones.

The ICD checks the validity of this classification using five adjustable functions that can also be combined:

- Detection/redetection counter
- Onset
- Stability
- Sustained VT
- SMART detection for devices of type DR-(T), HF-(T), and VR-(T) DX
- MorphMatch for devices of type DR-(T), HF-(T), and VR-(T) DX

MorphMatch is usually intended for the single-chamber detection [VR-[T] DX] which can of course be set as detection method in multi-chamber devices as well. The single-chamber detection method refers to the counter that counts the events within a tachyarrhythmia zone and to the detection criteria onset, stability, and MorphMatch.

With multi-chamber devices, however, SMART is the method of choice.

You can either set MorphMatch or SMART detection, but not both functions at the same time.

Detection counter

The following features are especially used to avoid unnecessary shock deliveries:

- Large range of values for the X-out-of-Y counters for the VF range to enable longer detection times
- Large range of values for the forward/backward counters for the VT1 and VT2 zones
- Exclusive counting for the VT and VF zones to clearly discriminate tachyarrhythmia
- Separately adjustable redetection parameters for the VF zone
- Standard values for all counters

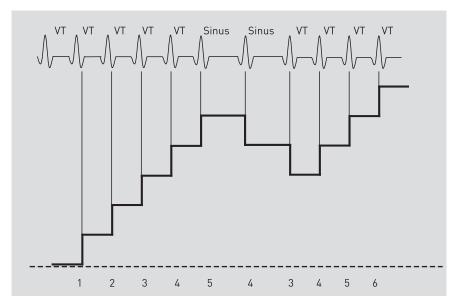
A tachycardic RR interval starts counting within a VT zone.

The ICD detects a tachycardia when the number of tachycardic RR intervals has reached the set value of the detection counter.

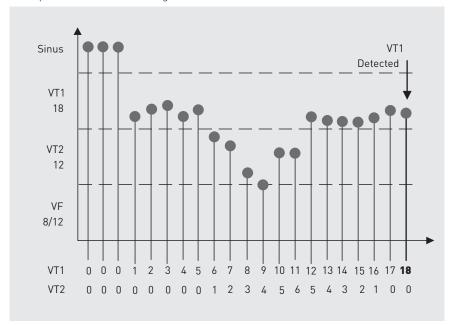
Each RR interval that is not tachycardic sets the counter back by the value one (forward/backward counter). If five consecutive intervals prior to initial detection are not tachycardic, the detection counter is reset and restarted.

The ICD distinguishes between individual short intervals (extrasystoles, couplets, runs) and a tachycardia using the detection counter.

Example of VT counter



Example of detection counting within the VT and VF zone

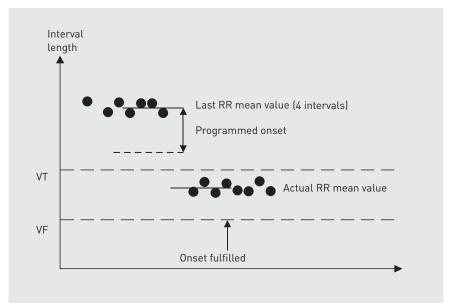


Onset If the onset criterion is switched on, then it has to be fulfilled in addition to the detection counter criterion.

The ICD enhances rhythm evaluation using the onset criterion and excludes signals of gradually accelerating tachycardias like sinus tachycardias from the decision for therapy. To do this, it forms a sliding RR mean value from the last four measured RR intervals.

The criterion is considered fulfilled if the difference between the last RR mean value and the current RR interval is larger than the onset parameter and this is confirmed by comparing the last RR mean value with the current RR mean value. Onset is set in [%] as a value relative to the RR mean value.

Onset criterion



Onset is also an integral feature of the SMART detection algorithm.

Stability

If the stability criterion is switched on, it has to be fulfilled in addition to the detection counter criterion.

The stability criterion is another factor that serves to enhance rhythm evaluation. Signals from irregularly conducted atrial tachycardia, such as atrial fibrillation, are excluded from detection and distinguished from stable ventricular reentry tachycardia.

If fluctuation between the durations of the last three tachycardia intervals remains within the set range of fluctuation, the stability criterion is considered to have been met for the current interval. The range of fluctuation can be specified in [ms] or [%].

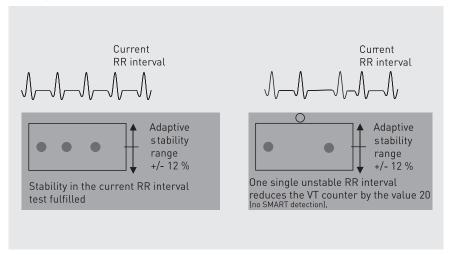
The percentage of the stability criterion refers to the heart rate. The interval is considered stable if the value set for stability is \pm 12% and none of the last 3 RR intervals deviates from the current interval by more than \pm 12%.

If SMART detection is switched off, an unstable RR interval reduces the VT counter by the value 20. If the value of the VT counter is less than 20, the counter is set to 0.

If SMART detection is switched on, detection of an unstable RR interval reduces the VT counter by the value provided by the SMART decision pathway.

The stability criterion is checked for each interval.

Stability criterion



Stability is also an integral feature of the SMART detection algorithm.

With and without SMART detection, the stability criterion is programmed as a percentage [%]. The stability criterion thus adjusts adaptively to the current heart rate. Additionally, when SMART is deactivated, the stability criterion can be programmed in [ms].

Sustained VT

The ICD uses the sustained VT criterion to detect and deliver therapy for sustained ventricular tachycardias that do not meet the onset or stability criterion, or do not meet a combination of the two.

The sustained VT function has a timer, which starts within the VF zone or one of the VT zones with two consecutive RR intervals. Once the timer has been started, it can only be reset by fulfilled termination detection, magnet application or initial detection with immediate therapy delivery.

If no termination detection occurs during the duration programmed for sustained VT, redetection is initiated. Upon redetection the additional inhibiting criteria onset and stability do not take effect.

The sustained VT function cannot be switched on if SMART detection is activated. The function can be implemented if the following conditions apply:

 Sustained VT for devices of type VR(-T), VR(-T) DX, DR(-T), and HF(-T): use of onset and stability

Due to increased dependency of tachyarrhythmia detection on the onset and/or stability criteria in the case of VT detection without SMART, all individual conditions have to be met to achieve detection.

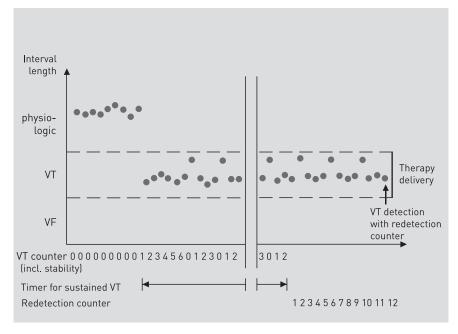
Consequences:

This results in the risk of non-detection. If one criterion is only not fulfilled because, for example, a disadvantageous limit has been programmed for stability, no therapy is delivered even though the tachycardic rhythm continues.

The sustained VT function can be used to override the checking of logically AND-linked criteria and to introduce therapy.

- SMART = OFF
- Onset and/or stability = ON

Detection of a sustained VT



Recording of non-sustained tachycardia (short intervals/ nsT counter) The device family has the ability to count and record non-sustained ventricular tachycardia as well as very short intervals to detect lead failures, connection failures between the device and lead, and other sources of interference.

1. Counter of short intervals

What is counted?

- Short intervals are recorded only on the RV lead (tip-ring).
- All events occurring in a time window (standard value: 110–140 ms) of 30 ms after noise interval are counted.

What is recorded in the device?

- Daily trend recording of short intervals that occur.
- Cumulative counter since implantation.
- Triggering of an IEGM recording if 30 short intervals are reached within 24 hours. This is followed by transmission via Home Monitoring.
- During follow-up, the IEGM recording can be accessed on the programmer in the Recordings window and in the Home Monitoring Service Center.

The data is accessible in the Recordings (Episodes tab) and Diagnostics (More diagnostics tab) windows as well as in the Home Monitoring Service Center.

Possible causes of short intervals are:

- Interference due to lead failures
- Interference due to incorrect connection of leads to the device
- Interference with external cause
- Recording of individual VF events

The short intervals counter cannot be deactivated. There is no special alarm when numerous short intervals occur. However, a new IEGM will be available in the HMSC and on the follow-up page of the programmer.

2. Non-sustained tachycardia (nsT)

What is counted?

- Non-sustained tachycardia that are too short to fulfill the VT/VF detection condition for the Counter parameter.
- Each interval sensed in the programmed arrhythmia zones increments the counter by the value one.
- Each interval that is not sensed in the programmed arrhythmia zones decrements the counter by the value one.

How are non-sustained tachycardias (nsT) detected?

- If five consecutive slow intervals are sensed outside the programmed arrhythmia zones and the counter value is still one or higher, this is declared as non-sustained tachycardias (nsT).
- A distinction is made between slow and fast nsTs:
 - Criterion for fast nsTs: the smallest weighted mean value of four consecutive intervals is less than 220 ms.
 - Criterion for slow nsTs: the weighted mean value of four consecutive intervals is always greater than 220 ms.
- nsT events are recorded only if no tachycardia detections occurred within this
 episode.

What is recorded in the device?

- Daily trend recording of nsT that occur.
- Cumulative counter of nsT.
- Triggering of an IEGM recording when an nsT occurs. This is followed by transmission via Home Monitoring.
- During follow-up, the IEGM recording can be accessed on the programmer in the Recordings window and in the Home Monitoring Service Center.
- When the parameter for nsT is set to OFF in the Parameters window (Diagnostics tab), IEGM recording and the associated counters and statistics will also be switched off.

The data is accessible in the Recordings (Episodes tab) and Diagnostics (More diagnostics tab) windows as well as in the Home Monitoring Service Center.

Possible causes of nsTs are:

- Interference due to lead failures
- Interference due to incorrect connection of leads to the device
- Interference with external cause
- Recording of individual VF events
- Non-sustained tachycardias that are too short to fulfill the VT/VF detection condition for the Counter parameter.

SMART detection

The SMART detection algorithm should use atrial rhythm evaluation to differentiate between ventricular tachycardia and a number of supraventricular tachyarrhythmias, for which therapy from the device is not required or not desired.

SMART detection is a discrimination algorithm that uses both atrial and ventricular signals to classify tachyarrhythmias. The classification of heart rhythms is accomplished by utilizing several main tests within the SMART detection algorithm. These are:

- Atrial and ventricular rate
- Rate stability
- Multiplicity (numeric ratio of atrial to ventricular signals)
- Stability of AV conduction
- Sudden changes in ventricular rate (onset)

Scope of validity

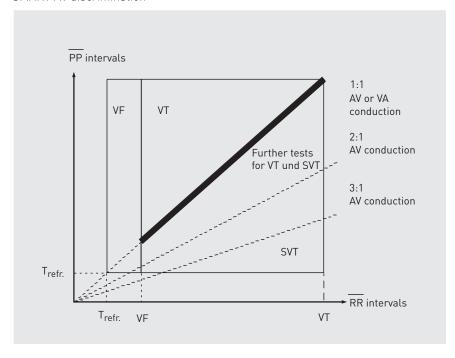
SMART detection is only applied to the VT1 and VT2 arrhythmia zones. If a ventricular rhythm meets the VT1 or VT2 criteria, the SMART detection algorithm provides an additional detection test. If the corresponding tachycardia originates in the atrium, ventricular therapy delivery is inhibited. If an arrhythmia fulfills the VT criteria, however, therapy is delivered.

Conditions

SMART detection can be applied selectively to the VT1 and VT2 arrhythmia zones:

- If SMART is only set in the VT1 zone, the counter is increased for VT1 once an interval falls within the VT1 zone and the SMART decision is VT.
- If SMART is only set in the VT2 zone, the counter is increased for VT2 once an interval falls within the VT2 zone and the SMART decision is VT.
- If SMART is set in the VT1 zone and the VT2 zone, the counter is increased for VT1 once an interval falls within the VT1 or VT2 zone and the SMART decision is VT.
- If SMART is set in the VT1 zone and the VT2 zone, the counter is increased for VT2 once an interval falls within the VT2 zone and the SMART decision is VT.

SMART AV discrimination

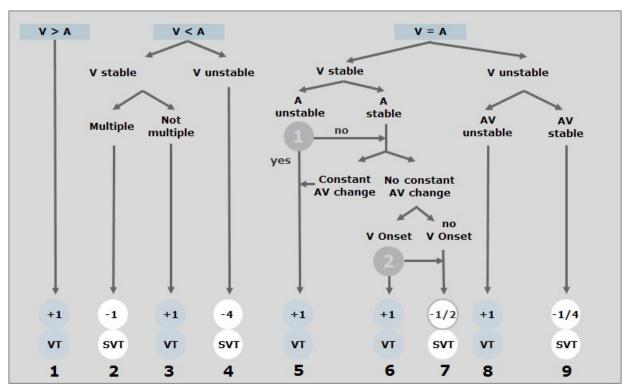


SMART detection algorithm functioning

The SMART detection algorithm is based on ongoing comparison of averaged atrial and ventricular intervals. These are calculated using four separate intervals in each case.

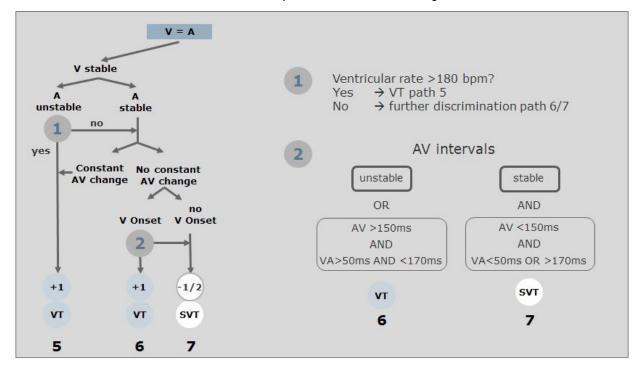
The SMART decision tree has been extended by two interrogations, see path 5 (position 1) and path 6 (position 2) in the graphic.

SMART decision tree



The extended interrogations position 1 and 2 apply under the conditions V = A and V = stable. These interrogations are only effective for initial detection, but not for redetection.

SMART decision paths with extended interrogations



If the ventricular rate is higher than the atrial rate, then the ICD increments the VT counter forward without further tests and delivers VT therapy.

If the atrial rate is higher than the ventricular rate and no exceptions apply, then the ICD assumes a supraventricular cause. For the exception rule, the ICD also tests RR stability and atrioventricular multiplicity.

If the averaged intervals in the atrium and ventricle are equal, then corresponding 1:1 decision trees are available, which include tests of the onset criterion as well as PP and PR stability.

The discrimination algorithm determines whether each RR interval within the VT zone is of supraventricular or ventricular origin.

In the case of ventricular origin, the VT counter is increased by 1. In the case of atrial origin, the VT counter is decremented by 0.25, 0.5, 1, or 4.

Note

SMART onset is preset to: 20%. SMART stability is preset to: 12%.

Optimization of SVT sensing using automatic far-field protection

The specificity of the SVT sensing is increased for the SMART algorithm by activating the automatic far-field-protection:

- Far-field protection
 - Far-field protection prevents atrial leads in dual-chamber modes from detecting events in the ventricle (far-field sensing) and interpreting them incorrectly as events in the atrial channel.
 - Events that are sensed in the far-field protection interval do not affect device timing.
 - Far-field protection always has a 16 ms time lead over the ventricular event
 - When the parameter far-field protection after Vs is programmed to AUTO, the algorithm behaves as follows:

If the patient's heart rate is below the programmed VT rate, the value of the far-field blanking = 75 ms.

If the patient's heart rate is above the VT rate, the value of the far-field blanking = 25 ms. This algorithm reduces unnecessary shock deliveries by specifying the atrial sensing behavior.

The automatic change from 75 ms to 25 ms occurs when VT/VF events are first detected. Two consecutive events shorten the FFB.

The VT/VF termination (short termination and episode termination) causes automatic change from 25 ms to 75 ms.

MorphMatch

Overview

The MorphMatch function employs an analysis algorithm to discriminate between ventricular tachycardia and supraventricular tachyarrhythmia for which device intervention is not necessary or desired.

MorphMatch can be used in both VT zones but not in the VF zone.

You can either set MorphMatch or SMART detection, but not both functions at the same time.

Since ventricular tachycardia (VT) originates in the ventricle, there is a significant difference between VT, sinus, and SVT morphology. The function makes use of this fact by evaluating the morphological characteristics of all intrinsic QRS complexes below the VF zone.

Classification of QRS complexes

The QRS complexes are classified by evaluation of certain morphological characteristics consisting of the following elements:

• A QRS complex is any sensed RVs that is slower than the defined VF zone. This is evaluated morphologically in the far-field channel. In addition, a time window of 250 ms triggered by the near-field channel (RV tip-RV ring) is evaluated. This time window extends across a time 100 ms prior to sensing and 150 ms after sensing of the QRS complex.

Note: Due to the observation window of 250 ms, the setting for the upper value of the VF zone is limited to a maximum of 231 bpm.

- Calculation of three morphological characteristics for each QRS complex
 - Normalized area: Areas under the morphology curves are calculated and divided by the value of the maximum amplitude, which normalizes them.
 - Normalized vector: A vector is composed of four peaks on the morphology curve and is divided by the value of the highest peak.
 - Maximum peak: determination of the maximum peak.
- From the three morphological characteristics for the individual QRS complexes below 100 bpm, a reference is formed for each morphological characteristic and provides an average reference value. This reference value represents the average QRS morphology in the sinus rhythm. By also taking into account the natural variance between the individual sinus morphologies, MorphMatch determines the MorphMatch threshold. The reference value and the MorphMatch threshold are updated on a beat-to-beat basis.
- Valid for intervals of the VT zone:

Each of these three morphological characteristics of the current QRS complex is compared (beat-to-beat) with the corresponding reference value, which corresponds to the average sinus QRS complex morphology. The differences in these three morphological characteristics are then summed and subsequently compared to the MorphMatch threshold.

- An integrated, permanent signal check ensures that any artifacts and signal distortions are filtered out.
- The reference curve is reset after termination of the episode or every 24 hours.

VT morphology counter

The VT morphology counter evaluates every sensed event and adds or subtracts every event as follows:

- Counter + 1: morphology difference > morphology threshold in the VT zones
- Counter ± 0: morphology difference < morphology threshold in the VT zones or event in the VF zone
- Counter 1: rate slower than defined VT zones, RVp
- Reset:
 VT counter reset or counter number = 0

VT therapy decision

For VT therapy decision, MorphMatch uses two different counters:

- VT counter
- VT morphology counter

Once the VT counter function meets the defined criterion, the VT morphology counter function checks whether a VT or a SVT has occurred. This is done according to the following criteria:

- VT morphology counter > 50% VT counter = VT is confirmed and the therapy is delivered
- VT morphology counter < 50% VT counter = SVT is confirmed and therapy is withheld

VT and SVT counters are reset after MorphMatch confirms an SVT.

A VT detection following immediately thereafter is not a redetection but still a detection using valid initial detection counters.

Limitations of the morphology criterion

The morphology criterion is limited in the following cases:

- Use in triple-chamber devices unless left ventricular pacing is deactivated
- Use in patients with intermittent or rate-dependent bundle branch block
- If MorphMatch has made the VT decision and a therapy has been delivered, the function is deactivated for the redetection time and is only available again after termination of the episode.

Recording MorphMatch decisions

MorphMatch decisions are stored in episode details and can be accessed there. These can be used to change the parameter value of the MorhMatch threshold if necessary.

The result of the morphology of the counter is shown in %. For significance of the value, see above VT therapy decision.

MorphMatch threshold parameter

The MorphMatch threshold parameter is used to adjust the parameter accordingly in case of MorphMatch wrong decisions, see MorphMatch – details [Page 51].

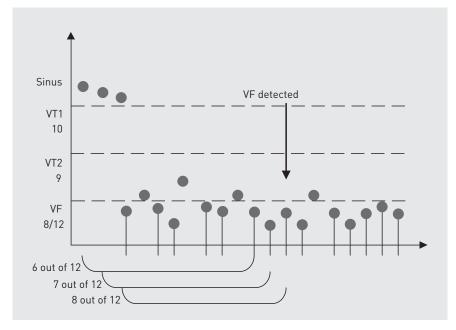
Ventricular fibrillation detection

VF detection

The ICD evaluates a heart rate as fibrillation if a minimum number X is less than the set VF interval out of a number Y of consecutive RR intervals. In this case, the unit is milliseconds [ms]. If [bpm] is selected instead of [ms] for the rate limit, a minimum number X out of the number Y from the consecutive signals must be above the set limit [bpm].

The VF detection uses this X-out-of-Y algorithm. An inhibiting criterion cannot be programmed for the VF zone because a ventricular fibrillation always requires therapy.

VF detection



Hysteresis after VF detection

The VF detection has a hysteresis function which extends the limit of the VF zone by $60~\mathrm{ms}$.

Mode of functioning

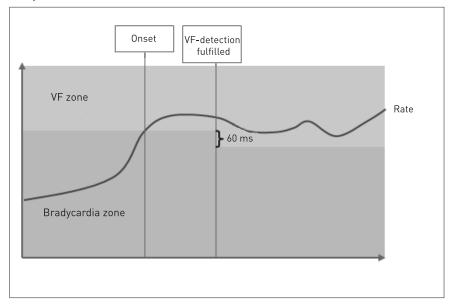
- Tachyarrhythmic rates that oscillate around the threshold of the VF zone no longer terminate shocks with confirmation during the charging phase of the capacitors.
- This function is effective only during the charging phase for shocks with confirmation.

Example

- Limit of VF zone: 200 bpm = 300 ms.
- VF was detected.

The shock with confirmation is terminated only when 3 out of 4 intervals are less than 360 ms = 167 bpm.

VF hysteresis



Ventricular redetection and termination

Redetection

Redetection begins as soon as a detected tachyarrhythmia episode has been delivered therapy but not terminated. A tachycardic RR interval then starts the counting. In the VT/VF zones, the parameters can be configured independently.

Therapy is delivered again if the number of tachycardic RR intervals reaches the set value in the redetection counter function. Each RR interval that is not tachycardic reduces the counter by the value one.

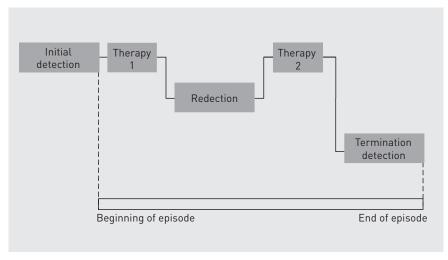
If the stability criterion is switched on, then this also applies to redetection.

If SMART detection is activated in the respective VT zone, the SMART redetection algorithm is automatically activated. SMART redetection cannot be switched off separately.

Termination detection

The ICD classifies a tachyarrhythmia episode as terminated if at least 12 out of 16 consecutive RR intervals are greater than the VT/VF interval of the lowest VT/VF zone (X out of Y not programmable).

Redetection and termination detection



Note

If VT1 is set up as a monitoring zone and initial detection is carried out in VT2 or VF, the limit for termination is not VT1, but VT2 or VF.

Forced termination

If a supraventricular tachycardia continues after successful VT/VF therapy, it has to be ensured that therapy is made available again in the case of repeated VT or VF.

An episode with sustained atrial fibrillation and tachycardic ventricular rate is considered terminated after the set duration has elapsed.

An episode with forced termination is saved in **[Recordings]**. The Forced termination parameter is a default setting and thus acts as a hidden parameter that is not visible on the user interface.

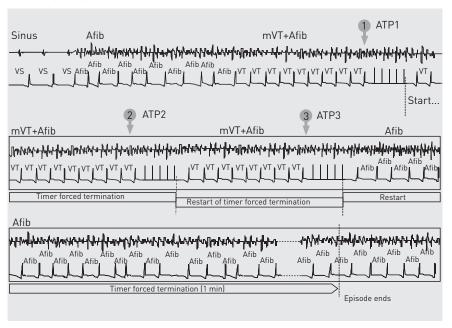
The following settings are required for an episode with sustained atrial fibrillation to be considered terminated:

- SMART = ON
- Forced termination = 1 min (fixed, non-programmable)

or

- SMART = OFF
- Onset and/or stability have to be activated in a VT zone.
- Sustained VT = OFF

Forced termination



Atrial rate classification

AT/AF rate classification

If the detection criterion **[bpm]** has been set instead of **[ms]** for atrial episodes, the AT/AF rate classification function continuously classifies each PP interval. An atrial episode starts when at least 36 out of 48 consecutive PP events have a higher rate than the set AT/AF rate. An atrial episode is considered terminated if 20 out of 24 consecutive PP events have a lower rate than the set AT/AF rate.

If the detection criterion **[ms]** has been set instead of **[bpm]** for atrial episodes, the number of intervals with a lower value than the set interval limit must also be 36 out of 48. An atrial episode is considered terminated if 20 out of 24 consecutive PP events have a higher value than the set AT/AF interval limit.

AT/AF event message via Home Monitoring

A timer is started at the beginning of an atrial episode. If no termination of the atrial episode occurs during this time, then a device message is transmitted pertaining to the sustained atrial episode.

SVT episodes

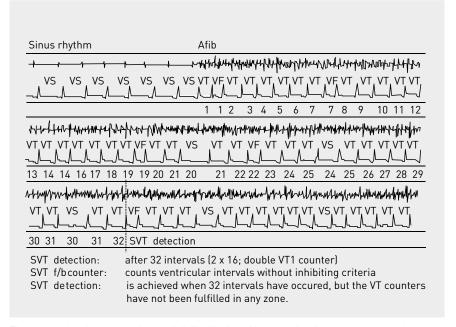
The supraventricular tachycardia counter cannot be set. This counter is defined as double the value of the VT1 counter. The VT1 counter can be set. If the VT1 counter has been set to 16, the value 32 automatically applies to the SVT counter.

SVT episodes are saved. A detection criterion is specified, which classifies an episode as a supraventricular tachycardia.

SVT detection is based on a forward-backward counter principle. All RR rates that are higher than the rates of the lowest VT zone are counted. Classification using inhibiting additional criteria such as onset or SMART is not carried out here.

An SVT episode is considered fulfilled if the SVT counter has reached the specified counter number, but the VT counter detection criterion is not fulfilled in any VT zone.

SVT detection



The example shows sudden atrial fibrillation. Upon activating the onset and stability criteria, the VT counter does not reach the required 16 events even if SMART is activated due to lack of stability of the RR intervals. The VT counter is repeatedly reset or repeatedly counted backwards by SMART.

The SVT counter, by contrast, reaches 32 intervals despite several negative counter steps caused by individual slower sinus intervals. Individual VF intervals stop the SVT counter.

The time of fulfilled SVT detection is the trigger event that is used to store the IEGM. SVT episodes are not only stored in dual- and triple-chamber ICDs, but also in single-chamber ICDs.

There is a second way to detect SVT episodes, see MorphMatch [Page 38].

Detection parameters

bjective	46
em	47
escription of detection parameters	47
nterval - details	48
etection and redetection counter - details	49
MART detection – details	49
nset – details 5	ō0
ustained VT – details 5	ō0
tability - details5	<u>5</u> 1
orced termination – details5	<u>5</u> 1
1orphMatch – details 5	51

Navigation: Parameters ightarrow Tachycardia ightarrow Detection

Objective

Detection parameters are used to allocate arrhythmias to an atrial (AT/AF) or ventricular arrhythmia zone (VT1 ... VF) and if necessary, decide on therapeutic options.



⚠ WARNING

Static magnetic fields: inactive detection and therapy

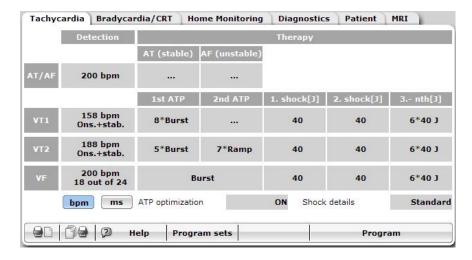
If the device's magnetic sensor detects magnetic fields beyond a magnetic flux density of approx. 1.5 mT, VT and VF detection as well as the respective therapies are deactivated.

If the magnetic sensor detects magnetic fields below 1 mT, VT and VF detection as well as the respective therapies are activated again.

Note

If VT/VF detection and therefore ICD therapy has been deactivated for more than 5 min in the 8 hours prior to the interrogation by applying a magnet or by the use of static magnetic fields (Acticor, Ilivia Neo, Intica Neo, Rivacor), a message text indicates that ICD therapy was temporarily deactivated. You can then set the status of the ICD therapy in the dialog window of the message text.

Item



Description of detection parameters

Parameter	Description
Interval (bpm) or Rate (ms)	Sets the limits of an arrhythmia zone; for more information see: Interval - details [Page 48].
Detection counter; Redetection counter	Distinguishes individual short intervals (extrasystoles, couplets, runs, etc.) from tachycardia; for more information see: Detection and redetection counter - details [Page 49].
SMART detection	Differentiates between ventricular and supraventricular tachyarrhythmia: ICD intervention is not necessary or desirable for the latter; for more information, see: SMART detection – details [Page 49].
Onset	Differentiates between gradually accelerating tachycardias and sudden tachycardias; for more information, see: Onset – details [Page 50].
Stability	Makes a distinction between conducted supraventricular tachycardias (atrial fibrillation, for example) and ventricular tachycardias that require therapy; for more information see: Stability - details [Page 51].

Parameter	Description
Sustained VT	Increases sensitivity, in case inhibiting criteria prevent detection of sustained VT; for more information see: Sustained VT – details [Page 50].
Forced termina- tion	The time period after which a detection or re-detection counts as terminated so that any new detection will have all therapies available; for more information see: Forced termination – details [Page 51].
MorphMatch	Helps to distinguish between supraventricular tachycardias and ventricular tachyarrhythmias through the morphological evaluation of the QRS complex; for more information see: MorphMatch – details [Page 51].

Interval - details

Navigation: Parameters \rightarrow Tachycardia \rightarrow Detection \rightarrow VT1, VT2, or VF

Effect of PP intervals

The parameter Interval (or Rate) has the following effect on PP intervals:

- If a PP interval is shorter (or a PP rate greater) than the parameter value programmed for an arrhythmia zone (AT, AF), the PP interval is assigned to the respective arrhythmia zone.
- A PP interval is limited by either an As, Ars, or Ap.

Effect of RR intervals

The parameter Interval (or Rate) has the following effect for RR intervals:

- If an RR interval is shorter (or an RR rate greater) than the parameter programmed for an arrhythmia zone (VT1, VT2 or VF), the RR interval is assigned to the respective arrhythmia zone.
- An RR interval is limited by either a Vs or a Vp.

The following are Vs:

- RVs
- PVC
- RVrs

The following are Vp:

- RVp (with right ventricular or biventricular pacing)
- LVp (with left ventricular pacing)
- If the value OFF is programmed, the ICD does not detect in the relevant arrhythmia zone.
- The parameter value also applies for redetection.

Detection and redetection counter - details

Navigation: Parameters ightarrow Tachycardia ightarrow Detection ightarrow VT1, VT2, or VF

Effect The detection counter and redetection counter parameters have the following effect:

• For AT/AF detection:

- If 36 of 48 consecutive tachycardia PP intervals are smaller than or equal to the programmed value of the AT/AF interval parameter, the rhythm is considered AT or AF.
- The Stability parameter differentiates between AT and AF; for more information see: Stability details [Page 51].

• For VT detection:

- The criterion is met if the number of tachycardiac RR intervals is greater than or equal to the programmed value of the detection or redetection counter parameter.
- Every RR interval that is greater reduces the counter by one. The smallest value is 0.
- Different values can be programmed for detection and redetection.

• For VF detection:

- If a minimum number (X) of the total number of consecutive RR intervals
 (Y) is greater than or equal to the programmed value of the detection or
 redetection counter parameter VF (X out of Y), the rhythm is considered
 as VF.
- Different values can be programmed for detection and redetection.

SMART detection - details

 $\textbf{Navigation: Parameters} \rightarrow \textbf{Tachycardia} \rightarrow \textbf{Detection} \rightarrow \textbf{VT1, VT2, or VF}$

Description

- SMART detection can be set separately for VT1 and VT2.
- By classifying the atrial rhythm, the SMART detection algorithm is designed to discriminate between ventricular tachycardias and a variety of supraventricular tachyarrhythmias (SVTs) for which device intervention is not required.
- If the RR interval is within VT1 or VT2, SMART detection checks whether an SVT is the cause of the tachycardia according to the following criteria:
 - Stability
 - Onset
 - Multiplicity
 - Comparison of atrial and ventricular rates

Effect

The SMART detection algorithm is based on a continuous comparison of the mean atrial and ventricular intervals obtained. These are calculated using four separate intervals in each case.

- If the ventricular rate is higher than the atrial rate, then the ICD increments the VT counter forward without further tests and delivers VT therapy.
- If the atrial rate is higher than the ventricular rate and no exceptions apply, then the ICD assumes a supraventricular cause. For the exception rule, the ICD also tests RR stability and atrioventricular multiplicity.
- If the averaged intervals in the atrium and ventricle are equal, then corresponding 1:1 decision trees are available, which include tests of the onset criterion as well as PP and PR stability.

DX devices

If the ICD assumes that there is under-sensing in the atrium, then SMART detection is not deployed and Onset/Stability is used instead to distinguish between SVT and VT.

Onset - details

Navigation: Parameters ightarrow Tachycardia ightarrow Detection ightarrow VT1, VT2, or VF

Effect

The onset parameter has the following effects:

- The programmed percentage relates to the difference between the following measurements:
 - Mean value from the last four RR intervals after onset
 - Mean value from the last four RR intervals before onset
- The criterion is met when the difference is greater than the programmed value
- In order to be effective, the onset criterion must be met in addition to the detection counter criterion.
- The criterion is only effective for initial detection. Onset is always considered fulfilled for redetection.
- For onset, there is only one common value for VT1 and VT2.

Sustained VT - details

Navigation: Parameters \rightarrow Tachycardia \rightarrow Detection \rightarrow VT1, VT2, or VF

Effect

The Sustained VT parameter works as follows:

- The counter is started by an initial VT1, VT2, or VF interval.
- The following events will stop and return the set time to zero:
 - VT or VF initial detection
 - Termination detection
 - Expiration of the set time
- If no VT, VF or termination is detected during the set sustained VT time, the following happens when the time expires:
 - Redetection with the respective parameter values is started.
 - Onset, stability and MorphMatch are not effective.
- The programmed value always applies uniformly to VT1 and to VT2.

Stability - details

Navigation: Parameters \rightarrow Tachycardia \rightarrow Detection \rightarrow VT1, VT2, or VF

Effect on atrial detection

The Stability parameter has the following effect on atrial detection:

- Prerequisite: Of 48 consecutive tachycardia PP intervals, 36 are equal to or less than the programmed value of the AT/AF interval parameter.
- If 5 of the last 8 tachycardia PP intervals differ by 40 ms or less from the preceding intervals for these 8 tachycardia PP intervals, the atrial tachycardia is considered stable and therefore as AT.
- If 3 of the last 8 tachycardia PP intervals are smaller than 200 ms (interval) or faster than 300 bpm (rate), the atrial tachycardia is considered unstable and therefore as AF.

Effect on ventricular

The Stability parameter has the following effect on ventricular detection:

- If the current interval remains within the defined range (range of fluctuation) of the previous three tachycardia intervals' fluctuations, this criterion is considered met for the current interval.
- Detected instability affects detection or redetection counters as follows:
 - If SMART detection is switched off, then:
 The VT counter for detections and redetections is reduced by 20. If less than 20, the counter is rounded to zero.
- If SMART Detection is switched on: The counters are adjusted individually, depending on the SMART decision pathway.
- If SMART detection is activated for VT1 and VT2, the programmed value for stability applies both to VT1 and to VT2.
- The value programmed for stability is effective for initial detection and redetection.

Forced termination - details

Navigation: Parameters \rightarrow Tachycardia \rightarrow Detection \rightarrow VT1, VT2, or VF

Effect Note

The parameter value for Forced termination cannot be set individually. It is preset to 1 min by the system.

The parameter value sets the time limit after which the episode is terminated:

- Prerequisites:
 - SMART detection is switched on.
 - For single-chamber modes: Stability is switched on for detection and redetection.
- Response without forced termination: If a VT has ended but an underlying SVT is still going on, then no termination detection takes place, but neither is any redetection made.
- In this case, the episode is forced to terminate after 1 min so that the entire range of therapy is available in the event of a new VT/VF.

MorphMatch - details

Navigation: Parameters \rightarrow Tachycardia \rightarrow Detection \rightarrow VT1, VT2, or VF

Effect

Prerequisite:

• The detection counter, onset, and stability criteria are fulfilled.

If Morphology = ON, the criterion works as follows:

If	Then
50% or more of the evaluated VT intervals show VT morphology,	the episode is classified and treated as VT, followed by a redetection or termination detection.
less than 50% of the evaluated VT intervals show VT morphology,	the episode is classified as an SVT episode. Therapy is withheld, the counter for VT, SVT, and MorphMatch are restarted, followed by redetection or termination detection.

- If MorphMatch = Monitoring, then the criterion works as follows:
 - The details, evaluation and course of the tachycardia are recorded.
 - The evaluation does not have an effect on therapy decisions.
- The evaluation based on the MorphMatch function is saved in the episode details data (MorphMatch counter; see also: Evaluating episode details [Page 181]).

Restrictions

- It cannot be used for redetection after an initial VT or VF detection
- Only if SMART detection is switched off
- Triple-chamber devices: in dual-chamber mode only (RV pacing only)
- In VT2 = ON , only if in VT1 MorphMatch = ON

MorphMatch

For VT1 and VT2 the following can be set individually:

Parameter setting	Effect
ON	Classification and therapy
Monitoring	Classification only The assessment is stored in the episode details, the decision on therapy options is not affected.

MorphMatch threshold

Parameter values and their effect:

Parameter setting	Effect
Std.	Standard value for the compliance level between the current QRS complex and the morphology reference upon which the decision on VT morphology is based
High	Larger morphological difference required for classification as a VT morphology
Low	Smaller morphological difference required for classification as a VT morphology

Note

Observe the following possible effects of the parameter values:

- The High setting can reduce the number of VTs detected.
- The Low setting can increase the number of undetected SVTs.

Status of ICD Therapy	54
Parameters for Tachyarrhythmia Therapy	57

Status of ICD Therapy

Activating and Deactivating ICD Therapy

Objective

In the ICD therapy group box, you can enable or disable the detection and therapeutic functions of the ICDs by clicking once on the **[ON]** or **[OFF]** button.



Activating the function will make the settings made in the Tachycardia tab effective.

⚠ WARNING

ICD therapy = [OFF] = inactive: no VT or VF therapy

If ICD therapy is switched off, the ICD does not perform any VT/VF therapy, regardless of the set values shown as detection and therapy parameters.

When the ICD therapy is switched on, ensure that arrhythmia zones and therapies are programmed effectively.

Messages The following messages can be displayed after interrogating the device:

Message	Meaning
Enabled	The ICD therapy is enabled according to its programmed detection and therapy parameters.
Disabled	ICD therapy is disabled. VT/VF therapies cannot be delivered regardless of the set and displayed values for detection and therapy parameters.
Temporarily active	ICD therapy is temporarily active. For DFT testing, the therapies set in the DFT tab are temporarily enabled. After the DFT test, the ICD can only begin delivering regular tachyarrhythmia therapies once the temporary program has been closed.
Temporarily inactive	ICD therapy is temporarily inactive. This is the case with tests on the follow-ups that are executed as a temporary program without enabling ICD therapy and with the DFT test when all temporary therapies have already been delivered.
Pending	The status of the ICD therapy could not be detected during device interrogation.

Programming Head and Magnet Application

General Considerations

The detection and therapy behavior of an ICD is different when the programming head (PGH) or the permanent magnet is applied.

Detection and therapy when programming head applied

If	Then
the PGH is applied, connection with the programmer is established and ICD therapy is activated,	detection and therapy are both: active and: temporarily inactive: during diagnostic tests temporarily active: during the DFT test
the PGH is applied, connection with the programmer is established and ICD therapy is not activated,	detection and therapy are both: inactive.
the PGH is applied for an interrogation or to establish wandless telemetry contact,	detection and therapy are always temporarily inactive. The last programmed state of ICD therapy is activated after the interrogation.

★ WARNING

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH: Raise the programming head by at least 30 cm; the device will switch automatically to the permanent program.
- In the case of wandless telemetry: Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

Detection and therapy when magnet applied

Note

Use the BIOTRONIK M-50 permanent magnet.

If	Then
a permanent magnet is applied,	detection and therapy of tachycardia events are interrupted.
a permanent magnet is applied for more than 8 hours,	the device automatically reactivates detection and therapies to prevent accidental permanent deactivation.

If you intend to actively interrupt detection and therapy for longer than 8 hours, the permanent magnet must be raised before the eight hours have elapsed in order to restart the time window again.

Note

If VT/VF detection and therefore ICD therapy has been deactivated for more than 5 min in the 8 hours prior to the interrogation by applying a magnet or by the use of static magnetic fields (Acticor, Ilivia Neo, Intica Neo, Rivacor), a message text indicates that ICD therapy was temporarily deactivated. You can then set the status of the ICD therapy in the dialog window of the message text.

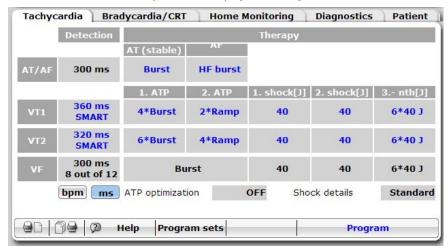
Parameters for Tachyarrhythmia Therapy

Objective

The ICD uses therapy sequences programmed by means of the tachyarrhythmia therapy parameters to terminate tachyarrhythmia in the zones AT, AF, VT1, VT2, and VF.

Navigation

Select $Parameters \rightarrow Tachycardia$ to display the Tachycardia tab:



Description

The therapy parameters can be configured on the user interface:

Therapy parameters	Meaning of parameters
AT/AF	For terminating atrial tachyarrhythmias each
	• 1 ATP attempt
	- AT (stable): ATP: Burst or Ramp
	- AF (unstable): HF burst
VT1 and VT2	For terminating ventricular tachyarrhythmias up to:
	• 2 ATP sequences with up to max. 10 ATP attempts each
	8 therapy shocks
VF	For terminating ventricular fibrillation up to:
	• 1 ATP attempt
	8 therapy shocks

Therapy sequence pattern

General functional principles

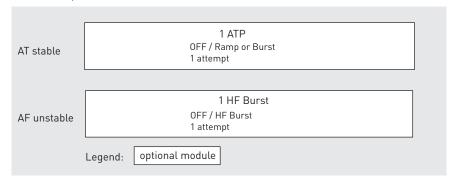
The ICD uses the following functions to treat atrial and ventricular tachyarrhythmias:

- Atrium: therapy by antitachycardia pacing (ATP) or HF burst
- Ventricle: therapy by antitachycardia pacing (ATP) followed by one or more shocks if necessary
- Ventricle: therapy by defibrillation with adjustable energy, polarity, and shock waveform, with or without confirmation

Atrial therapies

A therapy can be programmed for each of the arrhythmia zones AT or AF. The following therapies are available in the AT/AF zones:

Atrial therapies



Note

Atrial therapy rules

- a) Atrial therapy is successful if the episode is terminated within one minute. One therapy attempt is possible per episode.
 In case of failure, the function is blocked for the current episode.
- b) A maximum of 5 therapy attempts can be made per day.
- c) Apply the stability criterion (40 ms) to discriminate between stable and unstable atrial tachycardia.
- d) Ventricular backup stimulation is possible (standard value = OFF).
- e) Automatic shutoff until next in-office follow-up if an atrial episode lasts > 48 h or atrial therapy results in accelerated rhythm within one minute (VT/VF detection).

Ventricular therapy sequences

A therapy sequence consisting of scaled-strength therapies can be set up for each of the arrhythmia zones VT1, VT2, and VF.

VT1/VT2 therapy sequence

The therapy sequence for VT1 and VT2 consists of a combination of antitachycardia pacing sequences and/or shocks:

The following therapy sequences are available in the VT zones:	
1.	One ATP sequence with adjustable number of therapy deliveries and selectable ATP type.
2.	Two consecutive ATP sequences with independently adjustable number of therapy deliveries and selectable ATP type.
3.	A shock with adjustable energy, polarity, shock waveform, and confirmation.
4.	Two shocks with independently adjustable energy. Polarity, shock waveform, and confirmation are programmable, but are identical for both shocks.
5.	Two shocks with independently adjustable energy and up to six additional shocks with maximum energy. Polarity, shock waveform, and confirmation are programmable, but are identical for all shocks.
6.	Combinations of one or two ATPs and up to eight subsequent shocks.

VT monitoring zone:

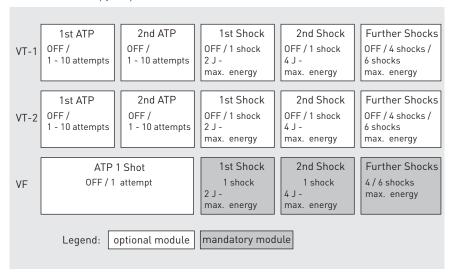
The VT1 zone can also be used solely as a monitoring zone even without a therapy sequence.

VF therapy sequence

The therapy sequence for VF consists of one ATP One Shot as a therapy option and/or forced shocks:

The following therapy sequences are available in the VF zone:			
1.	ATP One Shot as an attempt to terminate a stable VF without pain and is followed by a shock sequence if not successful.		
2.	Therapy sequence with two shocks with adjustable energy. Polarity, shock waveform, and confirmation are programmable, but are identical for both shocks.		
3.	Therapy sequence as in item 2 with up to six additional shocks with maximum energy.		

Ventricular therapy sequences

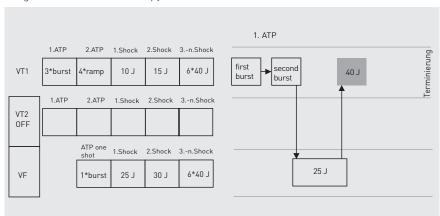


Progressive course of therapy

This function is a fixed setting in all arrhythmia zones. During the course of an episode, if redetection occurs in another arrhythmia zone, then only the therapies with a higher energy than the last delivered shock or the last ATP are still delivered.

The ICD blocks any ATP sequences for the current episode if a shock has already been delivered during its course.

Progressive course of therapy



If, in exceptional cases, no shock has been set in the VT1 zone (slow VT treatment) and an ineffective shock has been delivered in another zone, the progressive course of therapy in the case of redetection in the VT1 zone leads to the fact that, contrary to the previously described behavior, ATP therapies can be delivered again in the VT1 zone.

Tachycardia therapy parameters

Objective

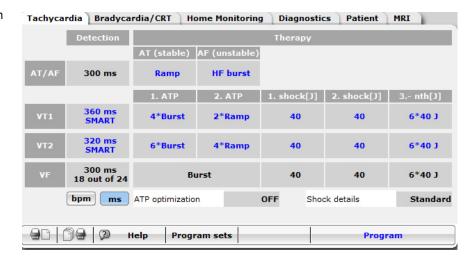
With the help of the parameters for tachycardia therapy, the therapy sequences to be used in the ICD are set in order to terminate tachycardias. The following therapy sequences are possible:

- ATP and burst therapies for AT/AF
- ATP and shock therapies for VT
- ATP One Shot and shock therapies for VF

Note

You must have activated detection parameters before you can set therapy parameters.

Item



Structure of the tachycardia tab

The following can be set in the Tachycardia tab:

- On the left: parameters for detection (for more information see: Detection parameters [Page 46]).
- On the right: parameters for therapy (for more information see: Tachycardia therapy parameters [Page 61]).

Setting parameters

To set the parameters, proceed as follows:

- 1. Select **[bpm]** or **[ms]**, depending on whether the limit of the arrhythmia zone is to be programmed as rate or interval.
- 2. Evaluate and change, if necessary, the preset parameter values.
- 3. Transmit the modified parameters to the device with **[Program]**.

Meaning of therapy parameters

Parameter	Description
AT (stable), AF (unstable)	 Therapy runs: Per detection: 1 Per day: 5 For more information see: AT and AF therapies – details [Page 62]
ATP optimization	The higher the rate of success of an ATP therapy, the earlier in the sequence it should be placed. For more information see: ATP optimization – details [Page 68]
Shock details	Set the shock waveform, polarity and path in detail to achieve optimal effectiveness. For more information see: Therapy shock parameters: configuring zones separately [Page 78]
ATP One Shot	ATP One Shot can be used as an initial low-energy therapy for VF. For more information see: ATP One Shot [Page 69]
[ATP help]	Displays the course of the ATP therapy sequences graphically. For more information see: Display ATP therapies graphically (ATP help) [Page 67]
Progressive course of therapy	If a shock has been delivered during the course of a tachyarrhythmia episode, the delivery of ATP therapies (including ATP One Shot) will be blocked for the remainder of this episode. The emission of further shocks always either requires a higher level of energy than the previous one or the maximum energy.
	If, in exceptional cases, no shock has been set in the VT1 zone (slow VT treatment) and an ineffective shock has been delivered in another zone, the progressive course of therapy in the case of redetection in the VT1 zone leads to the fact that, contrary to the previously described behavior, ATP therapies can be delivered again in the VT1 zone.
Surge guard	This function prevents detections caused by ineffective therapies from swinging to and from between the arrhythmia zones. For more information see: Surge guard – details [Page 79]

AT and AF therapies - details

Navigation: Parameters ightarrow Tachycardia ightarrow Therapy ightarrow AT/AF

Therapy concept

The following therapies can be used:

- For atrial tachyarrhythmia (AT): ATP (for more information see: ATP parameters [Page 70])
- For atrial fibrillation (AF): HF burst (for more information see: HF burst parameters [Page 71])

The following applies during the course of atrial therapies:

- If an atrial therapy that has not subsequently been terminated led to the detection of a VT or VF (tachycardiac rhythm in the ventricle), then atrial therapies are blocked until the next follow-up.
- For the follow-up, the physician will receive a corresponding message and actively decide whether to reactivate atrial therapies.

ATP therapy

Antitachycardia pacing (ATP)

Overview

The ICD can use various forms of antitachycardia pacing to deliver therapy of ventricular tachyarrhythmias. ATP can be configured individually so as to allow for creating ATP therapy sequences of various aggressiveness levels and integrating these in the therapy sequence.

Up to two ATP therapy sequences can be set up in the VT1 and VT2 zones. ATP One Shot can be set as a one-time therapy option in the VF zone.

ATP types

Numbers and types can be specified for each ATP. Two different ATP types, each with up to 10 therapy deliveries, can be selected:

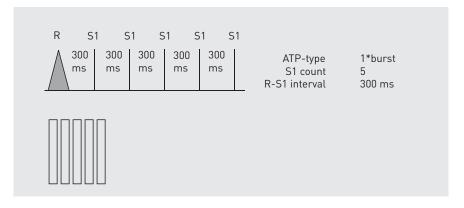
- Burst
- Ramp

Note

The bars in the following graphics are also displayed in the ATP help on the user interface.

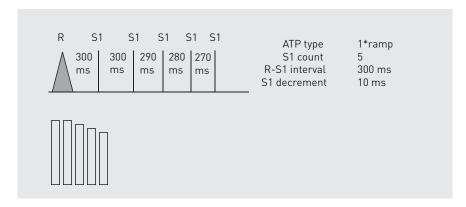
Burst

A number of S1 follows the R-S1 coupling interval at equal intervals.



Ramp

Pulses whose intervals change constantly follow the R-S1 coupling interval. The S1 decrement is the decisive element in determining change.



ATP parameters

Setting the ATP parameters

The various different antitachycardia pacing parameters are defined as adaptive to the last RR mean value. Depending on the set ATP type, the ICD changes the corresponding parameters from one delivery to the next.

Note

The ventricular pacing parameter can be used for triple-chamber ICDs to specify whether ATPs are only delivered to the right ventricle, the left ventricle, or both ventricles.

Number S1:

The number S1 defines the number of stimuli of an ATP.

Add. S1

Add. S1 causes the second and each following ATP to be extended by one stimulus each.

R-S1 interval:

The coupling interval R-S1 is at the beginning of each ATP. It defines the interval between the last R wave and the first S1 stimulus. The second stimulus always follows the first at the same interval. This parameter can be set as a percentage value of the last RR interval.

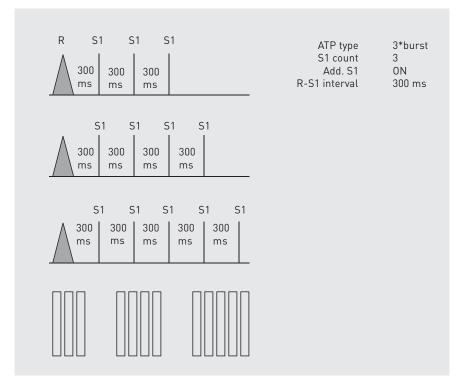
S1 decrement:

The S1 decrement continuously reduces the pacing interval within an ATP, beginning after the second stimulus. This parameter generates the Ramp ATP type.

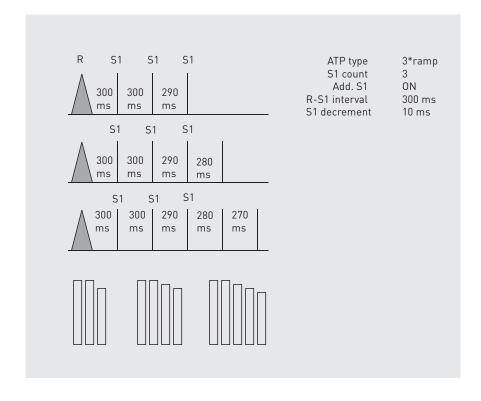
Scan decrement:

Scan decrement is used to specify shortening of the R-S1 interval with each additional pulse delivery.

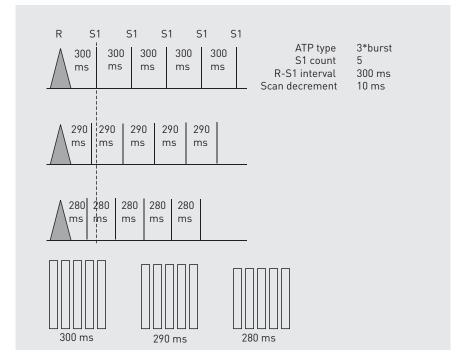
Burst with Add. S1



Ramp with Add. S1



Burst with scan decrement



Minimum interval:

This parameter specifies the minimum possible interval duration for ATP. This prevents a shorter interval, which could theoretically result from applying S1 decrement or scan decrement. The minimum interval applies to both ATP sequences. The minimum interval is set to a fixed value of 200 ms.

Minimum interval



ATP optimization

In order to optimize future therapies, the ICD stores ATP settings that have resulted in termination in the VT1 or VT2 zone. These settings are used for future ATP sequences at the beginning of the sequence. In the background, a counter stores the success or failure of each ATP therapy with the value +1 or -1 and sets the order of the ATP therapies according to their stored success counters. Effective ATP therapies are delivered first and ineffective ones are delivered last.

Upon later detection in a VT zone, in which a successful ATP sequence is already stored, this is delivered first. If not successful, the counter for this ATP is reduced by one (-1) for the corresponding zone and the therapy sequence in the same zone begins with the next successful therapy. The sequence of ATP therapies is thus continuously optimized by the use of the dynamic ATP therapy memory, which sorts and delivers the ATP therapies according to their success.

Upon detection in another arrhythmia zone, the therapy sequence is started with an ATP therapy that has been optimized and stored there.

ATP optimization is activated or deactivated together for the VT1 and VT2 zone.

The ATP surge guard runs in the background and ensures that rhythmaccelerating ATP therapy sequences are permanently blocked for the current episode and until the next ATP reprogramming.

ATP One Shot

ATP One Shot is intended to attempt one-time, painless termination of a stable VF and thus reduce the number of delivered shocks.

In the VF zone, an attempt to terminate fibrillation using ATP can be made once before shock delivery.

The ATP is only delivered if the VF fulfills the fixed stability criterion of 12% of the VT zone.

The shock following the ATP is always delivered with shock confirmation so that shock delivery can be prevented in the case of successful ATP.

If the ATP One Shot is not successful, the first shock in the VF zone is delivered without waiting for redetection.

ATP One Shot: early ATP delivery

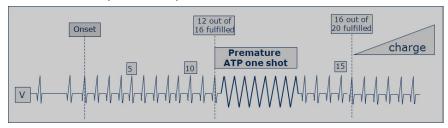
The additional function ATP One Shot – early ATP delivery is likewise intended to attempt one-time, painless termination of a stable VF and thus reduce the number of delivered shocks.

For detection conditions in the VF zone, see Early ATP delivery [Page 69].

If ATP One Shot – early delivery is unsuccessful, the VF counter for arrhythmia detection continues to run. Delivery of the ATP is not counted towards counting/fulfilling the VF counters, i.e., after ATP delivery in the example given below it would continue to count after 13. This first fulfillment of the programmed VF counters is marked as redetection, though it is actually the initial detection and causes delivery of the first shock.

Together with the shorter detection times, this is the main difference from ATP One Shot without early ATP delivery.

ATP One Shot, early ATP delivery



Display ATP therapies graphically (ATP help)

Navigation: Parameters \rightarrow Tachycardia \rightarrow Therapy

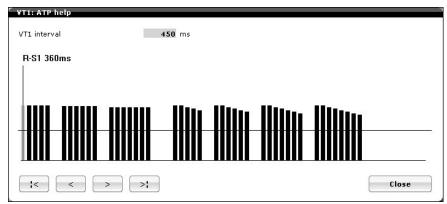
Display ATP help

To open the ATP help window, proceed as follows:

1. Select VT1, VT2, or VF in the tab: [ATP help...].

ATP therapy display

The ATP help window contains the following information:



- The graph displays the course of the ATP therapy sequences for the respective VT zone as groups of bars.
- The bars are grouped as follows:
 - Two blanks on the X axis mark the change to the next ATP attempt.
 - Four spaces on the X axis mark the changeover to the 2nd ATP in the sequence.
- Each bar represents an interval, portraying its relative size. The types and numerical sizes of an interval are entered into a caliper, which you can move from bar to bar using the arrow keys.

Related topics

See: ATP types – details [Page 69] and Antitachycardia pacing – details [Page 70]

ATP optimization - details

Navigation: Parameters o Tachycardia o Therapy

Function

- To optimize future therapies, the ICD continuously evaluates the success achieved by an ATP therapy in terminating a tachyarrhythmia in a therapy sequence in the VT1 or VT2 zone. In the background, the ICD automatically reconfigures the position of ATP therapy in the sequence according to its success rate: The higher the success rate, the farther ahead the particular therapy is placed in the sequence.
- The effective parameter setting of the therapy (e.g., Burst; Ventricular pacing: BiV; Number S1: 5; R-S1 interval: 320 ms, etc.) is also used in the new position (if applicable) in the sequence.
- ATP therapies that accelerate a tachyarrhythmia into a higher zone are blocked until the next follow-up.
- Reprogramming the ATP therapies resets ATP optimization.

Note

Note: Use the ATP statistics tab to display an overview of the therapy success or failure of the delivered ATP attempts.

Navigation: Recordings \rightarrow ATP statistics

See also: ATP Statistics [Page 187]

ATP types - details

Process

ATP types are subjected to the following process:

ATP type	Description
Burst	The R-S1 interval is followed by a programmed number of equidistant S1 pulses:
Ramp	The R-S1 interval is followed by pulses with constantly changing intervals. The S1 decrement is the decisive element in determining change:

Related topics

See: Antitachycardia pacing – details [Page 70]

ATP One Shot

Navigation: Parameters ightarrow Tachycardia ightarrow Therapy

ATP One Shot

ATP One Shot works as follows (if Early ATP delivery = OFF):

- If VF has been detected and the stability criterion has been met, ATP One Shot is used once prior to a shock.
- The capacitors are charged immediately after delivery of the ATPs. If the ATPs were delivered successfully, the capacitor charging is interrupted and shock delivery is prevented.

Early ATP delivery

Early ATP delivery is employed under the following premises:

- Early ATP delivery = ON.
- The value programmed for the detection counter is 16 out of 20 or greater.
- The stability criterion is met.
- The detection counter has classified 12 out of 16 intervals as VF.

Under the above-listed preconditions ATP is delivered on a one-off basis with the following further progression:

The shock capacitors are not charged immediately after ATP delivery, and the ICD continues to detect.

If the following occurs after delivery of ATP	Then
Termination is detected.	 The capacitors are not charged. For the time being, there is no therapy delivery.
VF is still detected.Detection counters are met.	 The capacitors are charged and the programmed shock therapies are delivered. The first shock requires a confirmation.

Medium-term impact assessment

If ATP One Shot remains ineffective for 4 consecutive tachyarrhythmias and the tachyarrhythmias were terminated without ATP employment, then ATP One Shot is automatically deactivated until the next follow-up. The function is then automatically reactivated at the next follow-up.

Antitachycardia pacing – details

ATP parameters

The parameters mean the following:

Parameter	Description
Attempts	Defines the number of ATP attempts.
ATP type	Defines the type or form of stimuli: burst or ramp.
Ventricular pacing	Defines the pacing location of a triple-chamber device: Right ventricle Left ventricle Biventricular
Number S1	Defines the number of stimuli of an ATP sequence.
Add S1	Number S1 increases by 1 with every ATP. The interval to the additional pulse depends on the size of the S1 decrement and the scan decrement.
P-S1 interval or R-S1 interval	Programmable coupling interval at the beginning of every ATP. It defines the interval between the last sensed P wave (not available for: Inlexa 1) or R wave and the first stimulus (S1). The second stimulus always follows the first one with the same interval.
S1 decrement	Continuously reduces the pulse interval of the ATP from the second stimulus on, so that the ATP type takes on the form of a ramp.
Scan decrement	Reduces the R-S1 interval from scan to scan after redetection.

HF burst parameters

The parameters mean the following:

Parameter	Description
Therapy	Therapy with AF: HF burst (high-rate burst)
Rate	HF burst rate
Duration	HF burst duration

Parameters for backup pacing

The parameters mean the following:

Parameter	Description
Backup stimulation	Basic rate of backup pacing
Mode (not programmable)	Mode of backup pacing

Defibrillation therapy

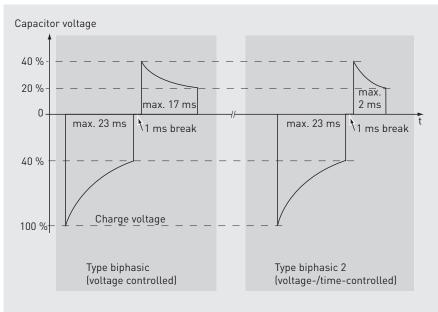
Shock therapy

For VT and VF therapy, the ICD can deliver defibrillation shocks. A maximum of eight shocks with different shock energies can be set for each VT and VF zone. Polarity, shock waveform, confirmation, and shock path are also adjustable, but these then have the same settings for all shocks in a zone.

Shocks

Shocks are delivered based on voltage and time. Switching and cut-off voltages as well as phase duration of the shocks are values that have been optimized within the course of clinical testing and cannot be modified. The energies of the first and second shocks can be set between two Joules and maximum energy. All shocks following the second shock in a particular zone are delivered with the maximum energy.

Shock waveform with normal polarity



The shock waveform can be set to biphasic, biphasic 2, or alternating, beginning with biphasic or biphasic 2, and selection can be made between normal, reverse, or alternating polarity, beginning with normal or reverse polarity. The ICD automatically limits the duration of the shock phases.

The parameters for the VT1, VT2, or VF zone can be configured individually by checking the box under **Tachycardia** \rightarrow **Standard** \rightarrow **Configure zones separately**.

Configuration options:

- Therapy shock parameters: confirmation [Page 75]
- Therapy shock parameters: polarity and shock form [Page 75]
- Therapy shock parameters: shock path [Page 77]
- Therapy shock parameters: configuring zones separately [Page 78]

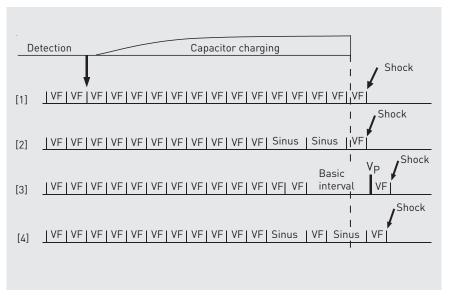
Charging process

If the ICD evaluates a cardiac rhythm as VF or VT, and if shock therapy has been programmed for these zones, the capacitors are charged.

Defibrillation with confirmation

For defibrillation with confirmation, the ICD evaluates the cardiac rhythm even while the capacitors are charging. The device does not deliver a shock if it detects an intrinsic rhythm below the VT1 zone or a bradycardia during the charging period. In all other cases, it will attempt to synchronize the defibrillation shock with the first tachycardic event after charging is complete. If no tachycardic intervals have been detected after charging is complete, shock delivery is inhibited.

Shock confirmation



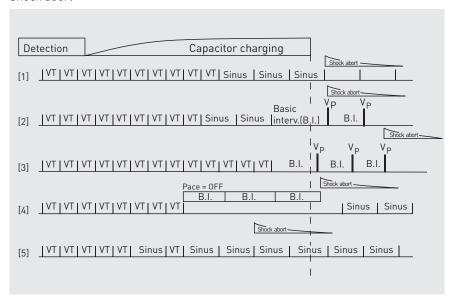
The diagram includes examples of defibrillation with confirmation based on different events of rhythm evaluation.

The abort criterion requires that three out of four consecutive intervals show a sinus rhythm or a bradycardia while charging. In these examples, the abort criterion is not fulfilled.

The shock is always delivered at the first tachycardic event after charging is completed. If an interval below the VT1 zone is detected at this time and the abort criterion is not fulfilled, the shock is delayed. The following intervals are subsequently classified.

The shock is delivered as soon as an interval is detected within a VT1 zone. Otherwise the shock is inhibited. However, the maximum duration between the end of charging and the shock is 2 seconds.

Shock abort



The diagram above shows the shock abort criteria of defibrillation with confirmation based on various events of rhythm evaluation.

The abort criterion requires that three out of four consecutive intervals show a sinus rhythm or a bradycardia.

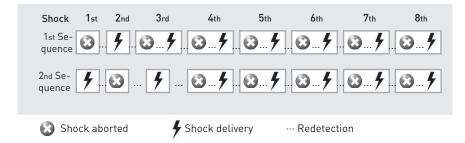
The rhythm is evaluated during the charging procedure. In the examples, the abort criterion is fulfilled. If, at the end of the charging period, the interval is not within the VT1 zone, the device waits for a tachycardia interval and the shock is delayed by up to two seconds maximum.

If the abort criterion has already been fulfilled before charging is completed, the charging process is stopped prematurely. The charged shock energy is then discharged through an internal resistance.

Note

Shocks with confirmation that were aborted after the charging are again available in the respective VT or VF zone, so that, for example, after aborting 8 programmed shocks, 7 remain available.

Shocks that the function skipped due to lack of confirmation are delivered from the third programmed shock at the same location after redetection:



When shocks with confirmation are performed, two sequences of shock deliveries can result in a VT or VF zone that are influenced by the starting behavior on shock delivery. In sequence 1, the first shock was aborted, while in sequence 2 the first shock was delivered.

Defibrillation without confirmation

If the ICD is set to defibrillation without confirmation, it will deliver a defibrillation shock after charging. The cardiac rhythm is not evaluated while the capacitors are charging. The ICD attempts to synchronize the defibrillation shock with an R wave. If synchronization does not succeed within two seconds, the ICD delivers the shock without synchronization.

Post-shock pacing

Post-shock blanking:

During post-shock blanking, the ICD will not evaluate the cardiac rhythm. This will suppress interference signals from post-shock potentials.

Post-shock pacing:

If the cardiac rhythm following a shock is bradycardia or asystole, the ICD paces according to the post-shock pacing parameters. At the same time, the cardiac rhythm is evaluated again.

If the episode has not been terminated, the ICD will initiate further therapy. The therapy sequence will only be concluded if termination or the maximum number of set therapies has been reached, Post-shock pacing parameters, p. 76.

Progressive course of therapy

The progressive course of therapy function works in the background and cannot be switched off. This function has the following effect:

- The ICD prevents further shocks from being delivered with lower energy after a shock. Instead, only shocks with higher energy are delivered.
- The ICD blocks all ATP therapies for the current episode if a shock has already been delivered during its course.

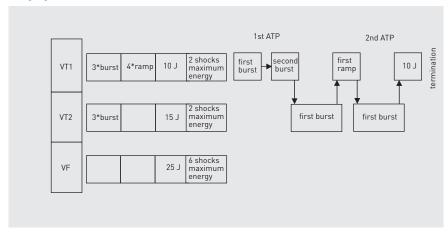
If, in exceptional cases, no shock has been set in the VT1 zone (slow VT treatment) and an ineffective shock has been delivered in another zone, the progressive course of therapy in the case of redetection in the VT1 zone leads to the fact that, contrary to the previously described behavior, ATP therapies can be delivered again in the VT1 zone.

Surge guard

The ICD uses this function to prevent the heart rhythm from fluctuating between the respective arrhythmia zones without achieving termination due to alternating accelerating and decelerating therapies. A therapy that causes acceleration is no longer used during an episode.

The Surge guard function cannot be programmed, see Surge guard – details [Page 79].

Surge guard VT1/VT2



Therapy shock parameters: confirmation

Navigation: Parameters \rightarrow Tachycardia \rightarrow Shock details

Confirmation parameters

The parameter settings are defined as follows:

Parameter setting	Description
ON	The ICD continues to evaluate the cardiac rhythm while the capacitors are charging.
	 The ICD does not deliver any shock when it detects a non-tachycardia rhythm during charge time.
	 Otherwise, the ICD tries to synchronize the defibrillation shock with an R wave.
	 If synchronization is unsuccessful, or if no tachycardiac intervals are detected after charging, shock delivery is withheld.
OFF	 The cardiac rhythm is not evaluated while the capacitors are charging. The ICD attempts to synchronize the defibrillation shock with an R wave. If synchronization is not possible, the ICD will deliver an asynchronous shock.

Therapy shock parameters: polarity and shock form

Navigation: Parameters \rightarrow Tachycardia \rightarrow Shock details

Polarity

Normal:

	1st phase	2nd phase
RV shock coil	Negative	Positive
SVC shock coil or active housing	Positive	Negative

Reversed:

	1st phase	2nd phase
RV shock coil	Positive	Negative
SVC shock coil or active housing	Negative	Positive

Polarity, alternating

Normal → alternating:

- The shock sequence starts with Normal polarity.
- With the second maximum energy shock, the polarity changes to Reversed and in the course of all subsequent shocks alternates between Reversed and Normal.

Reversed → alternating:

- The shock sequence starts with Reversed polarity.
- With the second maximum energy shock, the polarity changes to Normal and in the course of all subsequent shocks alternates between Normal and Reversed.

Shock waveform

The parameter settings are defined as follows:

Waveform	Biphasic	Biphasic 2
Pause duration	1 ms	1 ms
Energy	Variable	Variable
End voltage 1st phase	40%	40%
Time 1st phase	Max. 23 ms	Max. 23 ms
End voltage 2nd phase	20%	Variable
Time 2nd phase	Max. 17 ms	2 ms

Shock waveform, alternating

Biphasic \rightarrow alternating:

- The shock sequence starts with Biphasic.
- With the second maximum energy shock, the shock waveform changes to Biphasic 2 and in the course of all subsequent shocks alternates between Biphasic 2 and Biphasic.

Biphasic $2 \rightarrow \text{alternating}$:

- The shock sequence starts with shock waveform Biphasic 2.
- With the second maximum energy shock, the shock waveform changes to Biphasic and in the course of all subsequent shocks alternates between Biphasic and Biphasic 2.

Polarity and shock waveform alternate

When both Polarity and Waveform are programmed as alternating, then the shock sequence starts with the set primary values, and then the polarity changes first, only changing the shock waveform in its turn after that.

For example, if Polarity = Normal → alternating plus Waveform = Biphasic → alternating:

1st	Normal	Biphasic
2nd	Reversed	Biphasic
3rd	Normal	Biphasic 2
4th	Reversed	Biphasic 2

After 4th the shock sequence restarts with 1.

Therapy shock parameters: shock path

Navigation: Parameters ightarrow Tachycardia ightarrow Shock details

Shock path parameters

The parameters have the following meanings:

Shock path	Meaning
RV → Can+SVC	Distal RV \rightarrow housing + proximal (1)
RV → Can	Distal RV \rightarrow housing (2)
RV → SVC	Distal RV \rightarrow Proximal (3)

⚠ WARNING

In case of wrong shock path: no delivery of the required therapy

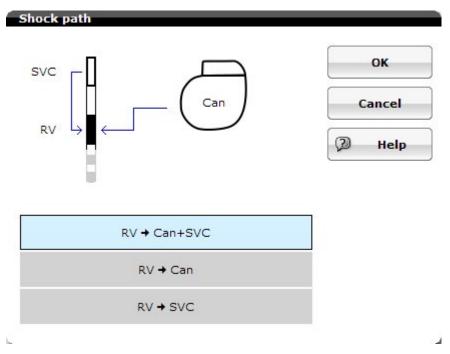
If the set shock path does not correspond to the implanted lead model, the required therapy cannot be delivered.

Make sure that the implanted lead model has two shock coils before setting one of the following values in the Shock path window:

 \Rightarrow RV \rightarrow Can+SVC

⇒ RV → SVC

The Shock path window



Therapy shock parameters: configuring zones separately

Navigation: Parameters \rightarrow Tachycardia \rightarrow Shock details

Configuring zones separately

Select [Configure zones separately] to enable you to set different values for each individual arrhythmia zone separately.

If different values have been set for each arrhythmia zone and you undo your selection, then the values of \mathtt{VF} will be entered for $\mathtt{VT1}$ and $\mathtt{VT2}$.

Parameters for post-shock pacing

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Post-shock pacing

Objective

After the termination of a ventricular arrhythmia by a therapy shock, the implanted device should not immediately begin pacing according to the permanent program, but should be able to respond to a possible temporary increase in threshold or to a higher required rate.

To do this you can program your own post-shock pacing. The duration of use and parameters of this program are temporary and can be set independently.

Pacing parameters

The pacing mode for the post-shock mode automatically arises out of the permanent program as follows:

Permanent program mode	Post-shock mode
DDD(R)	DDI
DDD-ADI(R)	DDI
DDI(R)	DDI
DDD-CLS	DDI

Permanent program mode	Post-shock mode
VVI-CLS	VVI
VDD(R)	VDI
VDI(R)	VDI
AAI(R)	DDI
VVI(R)	VVI
OFF	VVI

• A, RV:

Pulse amplitude: 7.5 VPulse width: 1.5 ms

LV:

Pulse amplitude: permanent programPulse width: permanent program

↑ WARNING

Changed pacing threshold: loss of capture

Defibrillation of the heart can temporarily increase the pacing threshold.

• Program the parameters for post-shock pacing with an adequate safety margin.

Surge guard - details

Function

If a tachyarrhythmia is accelerated by an ATP therapy into a higher arrhythmia zone and after the initial detection is redetected after a deceleration in that zone, then this ATP therapy is blocked for the remaining course of the episode.

ProgramConsult - selecting programs by indication	81
Pacing Modes	82
Resynchronization Therapy	88
Rate Adaptation	99
Pacing Parameters	110
iming Functions	111
Atrial and Ventricular Capture Control	133
Antitachycardia Functions	149
Patient Data Diagnostics and Home Monitoring	154

ProgramConsult - selecting programs by indication

Navigation: Parameters \rightarrow Program sets

Objective

The ProgramConsult function provides a number of programs with default parameters for the most common pacemaker indications.

By selecting a program suggestion for a specific indication, a number of default parameters are loaded which have shown to be effective for these indications.

- These parameters are displayed in blue in the program's tabs and windows.
- They are shown unchanged in black if the already set parameters have the same values as the programmed suggestions.

The parameters can be adjusted to the individual needs of the patient and transmitted directly to the device as a new permanent program.

Using ProgramConsult

Proceed as follows:

- 1. Select Parameters \rightarrow Program sets \rightarrow ProgramConsult.
- 2. Select a program with the applicable indication.
- 3. Adjust the parameters to the patient's needs.
- 4. Transmit the program to the implanted device by pressing [Program].

Pacing Modes

Mode (pacing mode)

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Mode



Asynchronous modes: no tachyarrhythmia protection

Asynchronous modes can only be set when tachyarrhythmia detection is switched off. Consequently, the device will not detect or treat any tachyarrhythmias.

Monitor the patient continuously and always keep an external defibrillator ready.

Single-chamber modes

AAI mode, VVI mode

Single-chamber modes of AAI and VVI are used for atrial or ventricular demand pacing. In each case, pacing and sensing only occur in either the atrium (AAI) or the ventricle (VVI).

The basic interval is started by a sensed or paced event. If an event occurs within the basic interval, pulse delivery is inhibited. Otherwise, pacing takes place at the end of the basic interval.

Dual-chamber modes

DDD mode

In the DDD mode, the basic interval starts either with an atrial sensed event As, an atrial paced event Ap, or a ventricular sensed event without a preceding atrial event (PVC = premature ventricular contraction).

If neither an atrial sensed event nor a PVC occur within the basic interval, atrial pacing takes place at the end of the basic interval and the basic interval and AV delay are restarted. However, if an atrial sensed event occurs within the basic interval, but outside the atrial refractory periods, atrial pacing is inhibited and the basic interval and the AV delay are restarted.

If no ventricular sensed event occurs during the AV delay, the device delivers a pacing pulse in the ventricle at the end of the AV delay. If a ventricular sensed event occurs during the AV delay, the ventricular pulse delivery is inhibited.

A ventricular sensed event without a previous atrial event (PVC) results in restart of the basic interval. The AV delay is not restarted in this case. Atrial and ventricular pulse delivery is inhibited.

DDI mode

In contrast to the DDD mode, the basic interval in DDI mode is not restarted by atrial sensed or paced events (P waves), but by ventricular sensed or paced events. The VA interval (basic interval minus the AV delay) is started together with the basic interval.

If no atrial or ventricular sensed event occurs during the VA interval, atrial pacing takes place at the end of the VA interval. The AV delay is restarted together with this pacing. If a sensed event then occurs, the atrial pacing delivery is inhibited. However, the AV delay does not start with this sensed event, but starts after the VA interval has elapsed. Therefore P waves do not trigger ventricular events in the DDI mode.

VDD mode

The VDD mode is derived from the DDD mode. The difference is that no atrial pacing takes place in the VDD mode. If the atrial sensed event does not take place, then the basic interval starts with a premature ventricular contraction or with the end of the preceding basic interval.

The AV block is the only indication for the VDD mode.

VDI mode

The VDI mode is derived from the VVI mode and enables the recording of atrial events. The VDI mode was originally designed for measuring retrograde conduction with the IEGM and/or the marker function. Retrograde conduction time can be determined directly in the programmer or in an additional ECG recorder as the length of time between a ventricular paced or sensed event and the subsequent atrial sensed event.

Triple-chamber modes

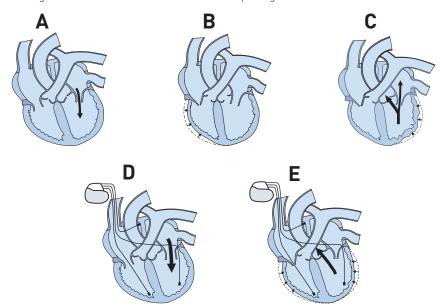
Triple-chamber devices

For triple-chamber devices, the NBG code is DDDRV. Triple-chamber pacing can be carried out using two leads in a single ventricle or in each of the two ventricles. Multisite ventricular pacing is the primary function of cardiac resynchronization therapy.

Both ventricles are paced synchronously. This prevents blood from being pumped back into the atrium through the mitral valve.

At the same time, the ventricle filling time and therefore the cardiac output is increased (see illustration).

The diagram shows how multisite ventricular pacing functions:



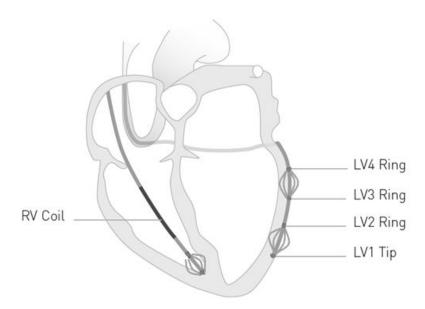
- A. Shortened diastoles result in incomplete left ventricular filling
- **B**. Delayed left ventricular contraction
- C. Septal dyskinesia and pumping blood back through the mitral valve
- D. Atriosequential biventricular pacing with extended diastole and increased left ventricular filling
- E. Synchronized ventricular contraction with increased cardiac output

The following ventricular pacing configurations are available for multisite ventricular pacing:

- BiV (pacing in both ventricles or in two locations within one ventricle)
- LV (pacing only in the left ventricle)
- RV (conventional single-chamber or dual-chamber pacing)

MultiPole Pacing: Devices of type HF-T QP can deliver 2 LV paces in the left ventricle and one pace in the right ventricle sequentially or synchronously. The pacing sites can be configured individually and offer the following options:

- 2 LV paces during each cardiac cycle
- 1 RV pace during each cardiac cycle
- 0-50 ms delay between the pacing sites LV and LV2
- Both LV paces require different polarities
- The following configurations are possible:
 - LV 2nd LV RV
 - RV LV 2nd LV



Note

Cardiac resynchronization in a triple-chamber device can be disabled by switching to RV pacing.

The ventricular pacing configuration BiV can be combined with dual-chamber and single-chamber modes with ventricular participation (DDD, VDD, DDI, VDI, VVI) and the ventricular pacing configuration LV can be combined with the atrial-controlled dual-chamber modes (DDD, VDD). The timing of the device is carried out in accordance with the rules of the configured single-chamber or dual-chamber modes. Only pulse delivery in the ventricles is additionally affected by the ventricular pacing configuration.

Note

The ventricular pacing configuration is to be programmed separately in the following programs and functions; it is not automatically adopted:

- a) Permanent program
- b) Mode switching
- c) Post-shock pacing

Summary of the functions and time intervals of the pacing modes

About this table

The table summarizes the functions and time intervals that apply to the various pacing modes. Not included are rate-adaptive parameters of the R modes (accelerometer) and parameters that can be programmed in all pacing modes.

The sensitivity can always be programmed during pulse inhibition and/or pulse triggering.

Functions and timing intervals of the different pacing modes

Parameter	Pacing modes							
	DDD	DDD- CLS	DDD- ADI	DDI	VDD	VDI	AAI	VVI
Basic rate	X	X	X	Х	Х	X	Х	X
Rate hysteresis	X		X	X	X	X	X	X
Rate scan/repetitive rate hysteresis	X		X	Х	X	X	Х	X
Upper rate	X	X	X		Х	X		
Pulse width/amplitude A	X	X	X	Х			Х	
Rate pulse width/amplitude	X	X	X	Х	Х	X		X
As inhibits Ap	X	X	X	X			X	
As triggers Ap								
As triggers Vp	X	X	X		Х			
Vs inhibits Vp	X	X	X	Х	Х	X		X
Vs triggers Vp								
Refractory period A	X	X	X	Х	Х	X	Х	
Refractory period V	X	X	X	X	X	X		X
Dynamic AV delay	X	X	X		X			
AV hysteresis	X	X			X			
AV scan/repetitive hysteresis	X	X			X			
AV safety delay	Х	X	X	Х				

Parameter	Pacing modes							
	DDD	DDD- CLS	DDD- ADI	DDI	VDD	VDI	AAI	VVI
Sense compensation	X	X	Х					
Ventricular blanking period	Х	X	X	X				
Wenckebach possible	X	Х	X		X			

Table legend:

- x = present
- A = atrium, atrial
- V = ventricle, ventricular
- Ap = atrial paced event
- As = atrial sensed event
- Vp = ventricular paced event
- Vs = ventricular sensed event

Rate-adaptive modes

Rate adaptation via CLS

The device achieves physiological rate adaptation with closed loop stimulation. The closed loop modes are functionally identical to the non-rate-adaptive modes, with the difference that the basic rate increases if the device senses patient stress or exertion. The closed loop modes are indicated by CLS.

Rate adaptation via accelerometer

Rate-adaptive modes are marked by an R (for rate) in the device code. The rate-adaptive modes function in the same way as the corresponding non-rate-adaptive modes, with the difference that the basic rate increases when patient exertion is sensed by the motion sensor.

Note

Take into account that with high rates in rate-adaptive modes (DDD-CLS, VVI-CLS, DDDR, DDIR, DDDR-ADIR, VDDR, VVIR, AAIR) it is possible that the atrial or ventricular refractory period can comprise a major portion of the basic interval, so that sensing of intrinsic events is limited or completely suspended.

Note

Automatic switching to DDI(R) or VDI(R) mode is performed by default when using mode switching.

Special modes

OFF mode

In the OFF pacing mode, all functions relevant to the pacemaker are deactivated in the permanent program. Sensing can only take place in the right ventricle, which is used for detection classification of the tachyarrhythmia therapy. If the OFF pacing mode is activated and ICD detection is programmed to OFF, the ICD is completely switched off.

V00 mode

In the V00 pacing mode, the pacing pulses are delivered asynchronously in the ventricle.

Note

Consider the risks associated with asynchronous ventricular pacing when programming the V00 mode.

No VT and VF detection are permitted in V00 mode.

D00 mode

Asynchronous AV sequential pulses are delivered in the D00 pacing mode.

Note

Consider the risks associated with asynchronous ventricular pacing when programming the $\ensuremath{\mathsf{D00}}$ mode.

No VT and VF detection are permitted in D00 mode.

Resynchronization Therapy

Settings for resynchronization therapy

Multisite or MultiPole left ventricular pacing polarity

In practice, the special and complex location of the left ventricular lead results in extracardiac pacing (e.g., phrenic nerve stimulation) more often than with right ventricular leads. Ideally, the LV lead is placed in a lateral or posterolateral coronary sinus vein and thus very close to the left-side phrenic nerve and to its area of stimulation. The problem of an undesired phrenic nerve stimulation can be eliminated by means of the programmable left ventricular pacing polarities without another surgical intervention. Different pacing polarities can be programmed with a bipolar or quadripolar LV lead, see the following pages.

In addition to the location of LV leads, passive fixation in the vein on the outside cardiac wall is an indication that LV leads often have poorer pacing thresholds than RV leads. Polarity paces can also be used in this case to avoid surgical intervention.

Note

Use of a bipolar or a quadripolar LV lead is required for the use of all pacing polarities of the multisite or MultiPole pacing.

Triggering and maximum trigger rate

Triggering in combination with cardiac resynchronization in the triple-chamber devices should ensure synchronous ventricular contraction in cases of nonspecific exertion (e.g., sinus tachycardia) as this makes an essential contribution to cardiac output for congestive heart failure patients.

A ventricular sensed event would cause inhibition of the stimulus in the ventricle by definition because the rules for the single-chamber and dual-chamber modes also apply to the triple-chamber modes. However, this would counteract cardiac resynchronization because it is based on synchronous pacing in the ventricle. Therefore triggering should cause forced left ventricular pacing after right ventricular sensing. The trigger pulse is processed as defined in the NBG code, but it is limited solely to the left ventricle and only in combination with one of the ventricular pacing configurations BiV or LV.

As a consequence of triggering, left ventricular pacing is delivered immediately following a right ventricular sensed event RVs (+ RPVC).

Triggering can be activated solely for right ventricular sensed events (RVs) or for a combination of right ventricular sensed events and right ventricular sensed extrasystoles (RVs + RPVC). Triggering can also be switched off entirely, in which case the device again functions in conventional DDD mode with a multisite ventricular pacing configuration.

Note

Even though premature ventricular contraction does not have a hemodynamic effect due to its special properties for resynchronization of the ventricle, there are some rare conditions (e.g., Chagas disease) that require the triggering of these events. Premature ventricular contractions do not normally have to be triggered.

Note

Triggering has to be set both for the permanent program and for mode switching. The setting from the permanent program is not automatically adopted.

In addition to the general option of switching off triggering, it is also possible to limit triggering for right ventricular sensed events using the maximum trigger rate. This parameter represents an upper limit for triggering, up to which the device triggers left ventricular stimuli based on right ventricular sensed events.

The maximum trigger rate can be set between 90 and 160 bpm. However, due to the greater affinity to the upper tracking rate (UTR), the maximum trigger rate can also be automatically programmed with the upper tracking rate using the setting UTR + 20 bpm.



Right ventricle triggering

In patients with intact AV conduction, intrinsic atrial tachycardia can be conducted into the right ventricle at a rate of up to 160 bpm. In such cases, deactivate triggering or reduce the maximum trigger rate.

LV T-wave protection

For protection against pacing in the vulnerable period of the left ventricle, triplechamber devices have a function that is controlled by left ventricular sensed events. This is intended to protect the left ventricle against triggered stimuli during the vulnerable period, which could be caused by a left ventricular extrasystole (LPVC). The LPVC is conducted into the right ventricle and used here as RVs to trigger left ventricular stimuli (see Triggering). The left ventricular pulse that is triggered immediately following the sensed RVs could then occur in the vulnerable period of the left ventricle.

The duration of the interval to protect against undesired pacing of the left ventricle is calculated based on the maximum trigger rate. The safety interval is started after each LVs.

Note

Left ventricular sensed events are only used for the function described above and for diagnostic purposes. It has no impact on timing in triplechamber devices.

Sensing polarity

The triple-chamber device offers different configurations for the left ventricular sensing function: In the unipolar configuration, the electrical signal is received between the left ventricular tip electrode and the device housing. The bipolar configuration, by contrast, measures signals between one bipole along the lead.

The quadripolar sensing polarity using a quadripolar lead provides the following setting options:

- $LV1 \rightarrow LV2$
- $LV1 \rightarrow can$
- $LV2 \rightarrow LV3$
- $LV2 \rightarrow can$
- $LV3 \rightarrow LV4$
- $LV3 \rightarrow can$
- $LV4 \rightarrow can$

VV delay

During biventricular pacing, either the right (RV) or the left ventricle (LV) can be set as the chamber that is paced first. This can be used to set interventricular conduction times to match the condition optimally. Interventricular conduction times between 0 and 100 ms are available only after ventricular pacing (LVp or RVp).

In the case of a right ventricular sensed event, conduction is carried out immediately. With the setting deactivated triggering or upon reaching the maximum trigger rate, inhibition is carried out. If LV T-wave protection is activated, a left ventricular sensed event would start the interval to protect the left ventricle and possibly prevent pacing in the left ventricle or, if LV T-wave protection is deactivated, there would be no effect.

Setting concept LV lead polarity: LV and 2nd LV stimulus

Navigation device HF-T: Parameters o Bradycardia/CRT o Pacing polarity o LV

Navigation device HF-T QP LV: Parameters o Bradycardia/CRT o LV/MultiPole pacing o Pacing polarity o LV

Navigation device HF-T QP 2nd LV: Parameters \to Bradycardia/CRT \to LV/MultiPole pacing \to Pacing polarity \to 2nd LV

Objective

The goal of left ventricular pacing and sensing is to do the following:

- Optimize hemodynamics
- Suppress phrenic nerve stimulation
- Reduce excessive left ventricular pacing thresholds
- The variety of possible settings allows you to set optimal values without having to reposition any leads.

Note

- Resynchronization therapy can be effective only with continuous multisite ventricular pacing. Patients cannot tolerate phrenic nerve stimulation.
- Phrenic nerve stimulation can be prevented by programming the lead configuration.

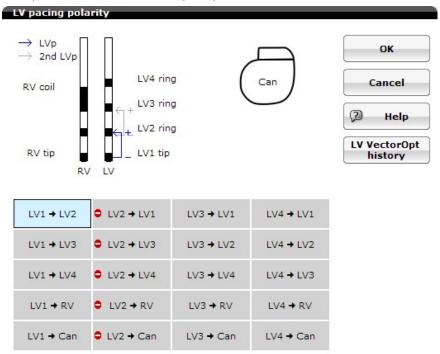
Lead polarity configurations

The following polarities for pacing and sensing are possible, depending on the type of lead being used (unipolar, bipolar or quadripolar):

Lead polarity	Number of polarities in LV				
	Pacing	Sensing			
UP	2	1			
ВР	5	2			
QP	20	7			

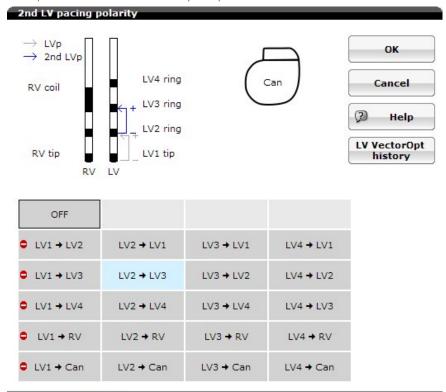
User interface

Example for device HF-T QP with quadripolar LV lead (LV)



Threshold: Not available PNS threshold: Not available

Example for device HF-T QP with quadripolar LV lead (2nd LV)



Threshold: Not available PNS threshold: Not available

Call and display LV pacing history

You can make the software display LV configuration and the measured values for the left ventricular pacing as a history.

The archive can be selected from the fields for LV pacing polarity. In triple-chamber devices this is possible both in the field for the LV pacing polarity and in the field for the 2nd LV pacing polarity.

Proceed as follows:

• Select the [LV VectorOpt history] option.

The archive shows the following:

- Polarity of the LV pacings
- Pacing threshold with details on pulse amplitude and pulse width
- Pacing threshold of the PNS pacing with details on the pulse amplitude and pulse width
- Interventricular conduction time RVs -> LVs
- Interventricular conduction time RVp -> LVs
- Lead impedance
- Remaining service time with respect to the selected vector. The time shortened for all displayed vectors is indicated here in comparison to the longest service time. For instance, vector 1 = longest, for vector 2 = -2 months. This is a relative estimation of the service time.
- Date of measurement

LV sensing polarity

For a description of the LV sensing polarity, see: Setting LV sensing polarity [Page 92]

Setting LV sensing polarity

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Sensing polarity

Setting LV sensing polarity

There are up to 7 setting possibilities for the LV sensing path depending on the type of LV lead used (see: Setting concept LV lead polarity: LV and 2nd LV stimulus [Page 90]).

Note

Please note that the LV sensing polarity can be programmed independently of the LV pacing polarity.

When using the CRT AutoAdapt and MultiPole Pacing functions, please note the following:

 Program the parameters of the left ventricular lead polarities LV1 to LV4 with the same settings for the LV sensing polarity and LV pacing polarity functions to ensure correct sensing and pacing.

Proceed as follows to set the left ventricular polarity:

- 1. Select a sensing polarity as a direct selection value (for example LV1 -> LV2) in the sensing polarity window.
- 2. Confirm with [OK].

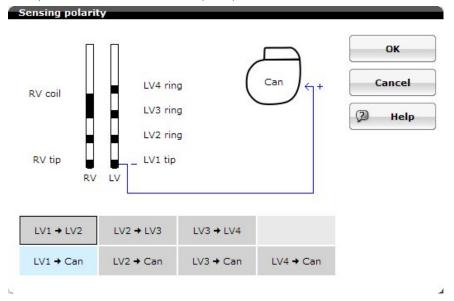
Result

The set path is displayed on the user interface in the following field:

$Parameters \rightarrow Bradycardia/CRT \rightarrow Sensing polarity$

User interface

Example of an HF-T-QP device with quadripolar LV lead



Setting ventricular pacing

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Ventricular pacing

Objective

Configure ventricular pacing for cardiac resynchronization therapy (CRT), etc.:

- Right ventricular (RV)
- Biventricular (BiV)
- Left ventricular (LV)
- Biventricular MultiPole Pacing (BiV-MPP)

Biventricular pacing

In the case of biventricular pacing, you can pace either the right or the left ventricle first.

The interventricular conduction time (VV delay) allows the biventricular pacing to be optimally set to the specific pacing requirement of the patient.

The CRT AutoAdapt function is available for optimum automatic adaptation of the CRT pacing.

The following parameters with the following functions can be set according to the indication and individual requirements of the patient:

Parameter	Function
CRT AutoAdapt	CRT AutoAdapt is a function that automatically and continuously adapts the CRT pacing. A prerequisite for use is that the patient has an intrinsic AV conduction. For further details see: CRT AutoAdapt [Page 95]
Triggering	Ensures that ventricular contractions are synchronous: RV, if sinus tachycardias occur In cases of premature ventricular contractions
LV T-wave protection	During the protection interval of the vulnerable phase for the left ventricle, no stimulus is delivered to that ventricle.
Maximum trigger rate	 Maximum rate to be used for resynchronization. The setting UTR + 20 derives the maximum trigger rate from the upper rate. The safety interval for the left ventricle is calculated from the maximum trigger rate (LV T-wave protection).
Initially paced chamber	The chamber to be paced first controls the primary pulse. VV delays can be set after Vp depending on RV or LV.
VV delay after Vp	Interventricular latency period:VV delay after Vp is configurable.

⚠ WARNING

LV-only pacing: risk for pacemaker-dependent patients

If lead dislodgement occurs, and the device is programmed to LV-only pacing, the effectiveness of ventricular pacing may be lost.

• LV-only pacing is contraindicated in pacemaker-dependent patients.

⚠ WARNING

LV-only pacing: loss of resynchronization or phrenic nerve stimulation

If lead dislodgement occurs, and the device is programmed to LV-only pacing, there is a risk of loss of resynchronization or phrenic nerve stimulation.

• Note corresponding symptoms in order to be able to take timely action.

★ WARNING

Triggering the ventricle: conduction of atrial tachycardias

For patients with intact AV conduction, intrinsic atrial tachycardias can be conducted to the ventricle to a maximum of 170 bpm.

In such cases, deactivate triggering or reduce the maximum trigger rate.

MultiPole Pacing

MultiPole Pacing is an additional pacing option in cardiac resynchronization therapy, with which 2 stimuli can be delivered to the left ventricle and 1 to the right ventricle during the cardiac cycle.

Note

MultiPole Pacing requires a large amount of energy and reduces the service time of the active device.

The following parameters with the following functions are set for MultiPole Pacing:

Parameter	Function
MultiPole pacing	The MultiPole Pacing settings with different pacing polarities of the 2nd LV stimulus can be found under: Parameters \rightarrow Bradycardia/CRT \rightarrow LV/MultiPole pacing \rightarrow Pacing polarity \rightarrow 2nd LV.
	For further details see: Setting concept LV lead polarity: LV and 2nd LV stimulus [Page 90]
LV-2nd LV delay	Latency period between LV stimulus and 2nd LV stimulus
Pacing sequence	Stimulation sequence as governed by the initially paced chamber.
	• LV - 2nd LV - RV
	• RV - LV - 2nd LV

CRT AutoAdapt

Navigation: Parameters o Bradycardia/CRT o Ventricular pacing o CRT AutoAdapt

Objective

The CRT AutoAdapt function automatically and continuously optimizes the CRT therapy settings of the device.

Ineffective CRT pacing is, among other things, due to suboptimal AV delay setting, because the intrinsic AV conductions change dynamically in the course of the clinical therapy and thus also the conditions for optimal AV delays.

CRT AutoAdapt automatically adjusts the AV delay and sets the ventricular pacing configuration to BiV or LV. The settings are based on intracardiac conduction times, which are measured every 60 seconds.

Note

Prerequisite for using CRT AutoAdapt: The patient has measurable intrinsic AV delays.

CRT AutoAdapt algorithm

CRT AutoAdapt has the following features:

- Frequent measurement of the intrinsic AV conduction. Measuring cycle: every 60 seconds.
- If the intrinsic AV conduction is interrupted, the measurement period will be continuously postponed up to 17 hours.
- The measurements of the intrinsic AV delays on the right and left side of the heart (A-RVs, A-LVs) are performed with device-specific measurement functions.
- CRT AutoAdapt can be used with MultiPole Pacing.
- CRT AutoAdapt only switches to solitary LV pacing if the LV capture control has been turned on.
- Measurement results and settings of the pacing configuration can be checked directly on the programmer during an in-office follow-up.

Requirements for the use of CRT AutoAdapt

The following conditions must be met for use:

- The patient has a measurable intrinsic AV delay.
- CRT AutoAdapt is switched on (ON or AVadapt).
- CRT AutoAdapt does not work during a VT/VF episode.
- For solitary LV pacing, the daily LV threshold measurement must be valid.
- The following pacing mode is set: DDD(R)/BiV.

Parameter of the automatic AV conduction tests

The following settings are used for the intrinsic conduction tests:

- BiV; VV delay = 0; Triggering = OFF; AV delay after pacing = 300 ms
- Automatic conduction test
 - AV delay on the right side (As-RVs)
 - AV delay on the left side (As-LVs)
 - Limit for AV delay measurement (As-RVs): 250 ms + sense compensation
- Pacing mode: DDD(R)/BiV

Test results and CRT AutoAdapt pacing settings:

The automatically adapted AV delay is 70% or at least -40 ms of the measured right-side intrinsic AV delay (A-RVs) to ensure reliable ventricular pacing. The percentage indicated above can be changed, if necessary, in the CRT AutoAdapt expert parameters.

Test result of comparison of AV delays (RV, LV)	Resulting pacing setting
A-RVs < A-LVs	LV pacing with dynamic AV delay
A-RVs = A-LVs	BiV pacing with dynamic AV delay
A-RVs > A-LVs	BiV pacing from the permanent program with fixed AV delay

Test results and CRT AutoAdapt pacing settings: AVadapt

For setting CRT AutoAdapt = AVadapt, the same AV optimization behavior applies as for setting CRT AutoAdapt = ON. The difference between setting CRT AutoAdapt = ON and CRT AutoAdapt = AVadapt is that no LV pacing with dynamic AV delay can be set with the CRT AutoAdapt = AVadapt setting.

CRT AutoAdapt parameters

In addition to activating the function with the ON and AVadapt setting options, the CRT AutoAdapt window also displays the following measured values and information:

- Last measured AV conductions
 - Last measured AV conduction Ap > RVs
 - Last measured AV conduction As > RVs
 - Last measured AV conduction Ap > LVs
 - Last measured AV conduction As > LVs
- Optimized AV delays
 - Optimized AV delay after pace
 - Optimized AV delay after sense
- Date and time of last optimization
- Status
 - adaptive BiV
 - adaptive LV only
 - non-adaptive BiV
 - suspended
- Note

During non-adaptive BiV pacing:

- Irregular rhythm
- High rate

During interrupted pacing mode:

- A/V episode runs
- Mode switching
- Post-mode switching
- Post-shock pacing

CRT AutoAdapt continues to run in the background during follow-up. The above-mentioned measured values and information initially show the status during the first interrogation. The values can be refreshed at any time through [Interrogate]. This is also used to test out the function when applying on the patient for the first time.

CRT AutoAdapt expert parameter

Click on the triangle in the lower part of the CRT AutoAdapt window in the line [Show CRT AutoAdapt expert parameters].

The values can now be modified for the following parameters to customize the AV parameters set by CRT AutoAdapt to specific requirements.

- Adaptive AV reduction;
 range of values: 0.5; 0.6; 0.7; 0.8; 0.9; standard value: 0.7
- Adaptive AV lower limit; range of values: 50 ... (10) ... 150 ms; standard value: 50 ms

Diagnostics CRT AutoAdapt expert parameter

In the CRT AutoAdapt window, click on **[CRT AutoAdapt diagnostics]** to view recordings on the effectiveness of CRT pacing, as well as adaptive AV delay.

Recorded parameter:

- Ventricular pacing status
- Adapted AV delay

Rate Adaptation

Pacing modes

Rate-adaptive modes

Rate adaptation principles

The device uses 2 independent principles for rate adaptation:

- Physiological rate adaptation via closed loop stimulation
- Rate adaptation using the accelerometer

An overview of rate adaptation

The programmable rate-adaptive modes can be categorized as follows:

Rate adaptation		
Closed loop stimulation	Accelerometer	
DDD-CLS	DDDR	
VVI-CLS	DDIR	
	DDDR-ADIR	
	VDDR	
	VVIR	
	VDIR	
	AAIR	

Mode-independent rate adaptations

Principles

The device uses 3 more functions for rate adaptation that are not controlled by measuring the physiological stress of the patient:

- Rate smoothing
- · Rate fading
- Rate stabilization (during mode change)

Sensor functions

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Sensor/Rate fading

Objective

Sensor-controlled rate adaptation adapts the pacing rate to changing metabolic requirements at rest and under stressful conditions.

Description

The pacing rate increases at the onset of exertion to the sensor determined rate. It slowly returns to the basic rate when exertion is no longer detected. Detection and inhibition remain active during sensor-controlled operation.

Note

Where pacing rates are high, the refractory period may take up a large share of the basic interval, which can lead to asynchronous pacing.

Each parameter in detail

See Sensor Functions – Details [Page 100]

Sensor functions - details

Navigation: Parameters \rightarrow Bradycardia/CRT \rightarrow Sensor/Rate fading

Maximum sensor rate

Regardless of the sensor's detected signal amplitude, the pacing rate will never exceed the programmed maximum sensor rate. The programmed value refers to the maximum pacing rate in sensor control and must be less than the upper rate.

Note

The shorter the selected AV delay, the higher the maximum sensor rates can become. The respective values are indicated by the programmer.

Sensor gain

The programmable sensor gain designates the factor by which the electric signal of the sensor is amplified. This allows the rate adaptation to be modified for individually variable signal strengths. The optimal setting is achieved when the desired maximum sensor rate is reached during maximum exertion. Before adjusting the sensor gain, the rate increase, rate decrease, and maximum sensor rate parameters must be checked for their suitability with respect to the individual patient.

Automatic sensor gain

The programmable sensor gain is supplemented by the automatic sensor gain function. Every day, the device checks whether 90% of the set maximum sensor rate has been reached for a certain total duration (for at least 90 s (cumulative) within one day).

If	Then
90% of the set maximum sensor rate is reached,	the sensor gain decreases by one increment.
90% of the set maximum sensor rate has not been reached within 7 days,	the sensor gain increases by one increment.

Sensor threshold

The minimum signal strength used for rate adaptation is determined using the programmable sensor threshold. Sensor signals below this threshold do not affect rate adaptation. With the sensor threshold, a stable rate can be achieved when the patient is at rest by ignoring low-amplitude signals that have no relevance for increased levels of physical exertion. If the pacing rate at rest is unstable or reaches values that are above the basic rate, the sensor threshold should be increased. On the other hand, the sensor threshold should be reduced if a sufficient rate adaptation is not observed with slight exertion. The sensor gain should be adjusted before setting the sensor threshold.

Rate increase

The programmed rate increase value determines the maximum speed at which the pacing rate rises if the sensor signal indicates increasing exertion. A setting of the rate increase of 2 bpm per cycle, for example, means that the rate increases from 60 bpm to 150 bpm in 45 cycles. The programmed rate increase applies only to the rate analyzed by the sensor.

Rate decrease

The programmed rate decrease value determines the maximum speed by which pacing is reduced if the sensor signal begins decreasing. A setting for rate decrease of 0.5 bpm per cycle, for example, means that a rate of 150 bpm will fall to 60 bpm within 180 cycles.

Note

In DDIR mode, the actual rate decrease is sometimes slower, depending partly on the programmed AV delay.

Sensor simulation

Even when a non-rate-adaptive mode is programmed, the sensor response is recorded without being effective. As a result, when rate adaptation is activated there will already be data according to which the sensor response can be evaluated in the histogram.

Rate fading - rate smoothing

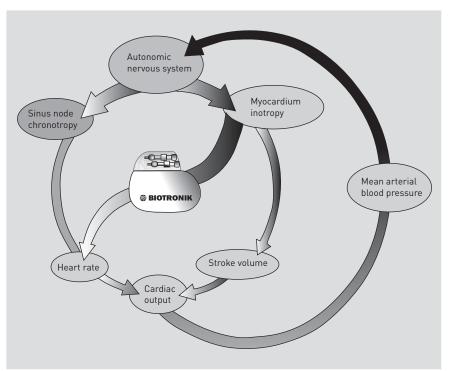
In all pacing modes, the rate smoothing function (rate fading) can, in cases of sudden rate decreases, lead to a controlled adjustment of the pacing mode of the device to the patient's intrinsic rhythm, to the programmed basic rate or to the sensor rate.

If rate smoothing is activated, the device calculates the backup rate, which is always active in the background. When a sudden decrease of the heart rate occurs, the device immediately begins to pace at the backup rate and regulates the process of rate decrease guided by the backup rate and the rate fading settings.

Physiological rate adaptation (CLS function)

Principle of closed loop stimulation

The contraction dynamics of the myocardium vary depending on the patient's exertion. The changes are characteristic and closed loop stimulation uses these to generate a physiological pacing rate specific to the patient. This also applies to the patient's mental stress.



The device evaluates the dynamics of the contraction of the myocardium (inotropy) in a short time period after the beginning of ventricular excitation. Impedance measurement is carried out with a ventricular lead and is primarily dependent on the specific conductivity of a small volume surrounding the lead tip.

The impedance changes are characteristic for the ventricular contraction procedure and directly proportional to the stress on the heart. The device calculates the required pacing rate using a reference measurement with a reference impedance curve recorded at rest. The CLS responds immediately at the beginning of stress by using contractility as input information for rate adaptation. Therefore, the combination with rate adaptation by accelerometer is not necessary.

Closed loop stimulation is self-calibrating and automatically adjusts to the patient's situation within just a few minutes. There is usually no need to manually fine-tune the system. Automatic fine-tuning is active during the entire service time of the device.

Among other things, pacing cycles with extended or shortened AV delays update the reference impedance curves at regular intervals.

However, some individual cases (e.g., if the patient is extremely active or extremely inactive) may require adjustment of the CLS.

Individual adjustment of CLS parameters

Overview

The following parameters can be individually adjusted in the ${\sf CLS} \to {\sf Hide} \; {\sf CLS}$ expert parameters window:

- CLS response
- CLS resting rate control
- Vp required

Vp required

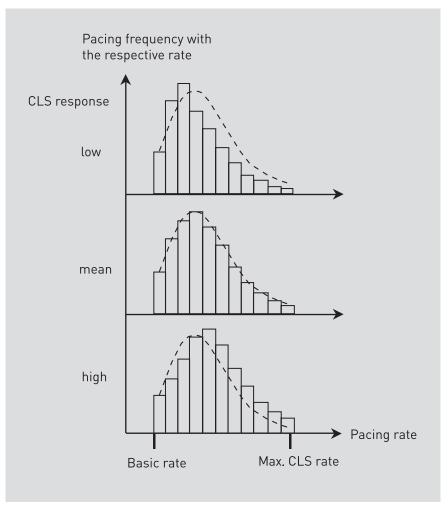
In the mode DDD-CLS, an AV hysteresis is set by default to support existing adequate intrinsic AV conduction. For patients with inadequate or non-existent intrinsic AV conduction, it may be necessary to deactivate the AV hysteresis. The Vp required parameter is activated for this.

CLS response

The factory settings for closed loop stimulation are made so as to ensure that the majority of patients receive optimum rate dynamics. Adjustment is not usually required.

However, the rate profile resulting from closed loop stimulation can vary greatly from patient to patient. In individual cases, the rate dynamics can be optimized if rate distribution is not adequate.

The CLS response parameter affects an internal device target rate, which depends on the preset basic and maximum closed loop rate parameters. The device internally controls rate adaptation so that 20% of the pacing events are always above the internal target rate. If the CLS response parameter is reprogrammed, increasing setting values result in rate distribution towards higher mean rates and lower setting values result in rate distribution with lower rates.



Resting rate control

This parameter limits the pacing rate attainable at rest to the programmable value of, e.g., 20 bpm above the set basic rate. This serves to suppress unspecific rate excursions at rest without limiting rate adaptation in cases of mental stress. This can be switched off if a high rate limit is not desired from the clinical perspective.

The exact value depends on the relationship between the basic rate and the maximum closed loop rate.

CLS safety feature

The device regularly checks the requirements for correct closed loop stimulation internally. If one of the requirements is not met, then closed loop stimulation is interrupted. The accelerometer takes on rate adaptation for the duration of the interruption. Once all requirements have been met, closed loop stimulation is automatically activated again. The following events interrupt closed loop stimulation:

- Automatic initialization of CLS
- Mode switching
- Ventricular fusion beats
- Inadequate impedance values
- Hardware and software errors

Rate adaptation using the accelerometer

Rate adaptation (R modes)

Objective

Sensor-controlled rate adaptation adapts the pacing rate to changing metabolic requirements at rest and under stress conditions. With increasing activity, the pacing rate rises to the rate determined by the sensor and then slowly drops back to the programmed basic rate when no further activity is detected.

This is implemented technically through an accelerometer integrated into the circuitry. Under physical activity, the accelerometer generates an electrical signal that is continually evaluated.

The following parameters characterize rate-adaptive pacing:

· Sensor gain

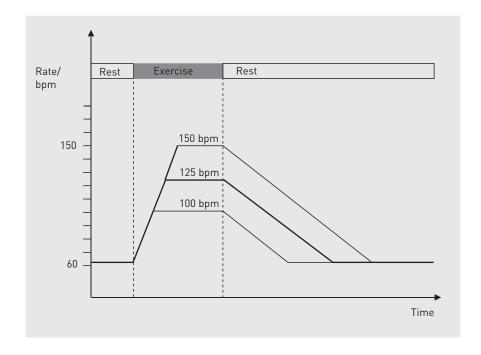
Factor that correlates a certain level of activity with a defined rate.

• Automatic sensor gain

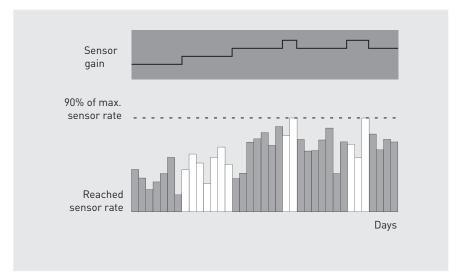
When automatic gain is switched on, the gain parameter is influenced as follows:

- If 90% of the maximum sensor rate is not reached for the duration of 1 hour within a week, gain is incremented by one step.
- If 90% of the maximum sensor rate is reached for 1 hour within 24 hours, gain is reduced by one step.

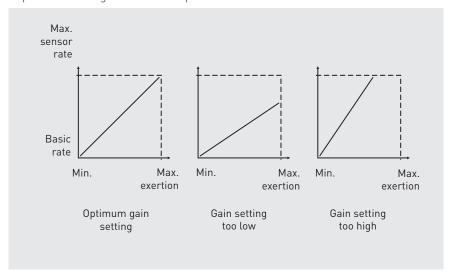
Maximum sensor rate for various settings during physical activity



Automatic adjustment of sensor gain with a 7:1 algorithm

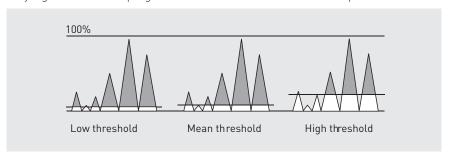


Impact of sensor gain on rate adaptation



The **Sensor threshold** defines the value for the minimum level of activity triggering a defined rate above the hysteresis rate.

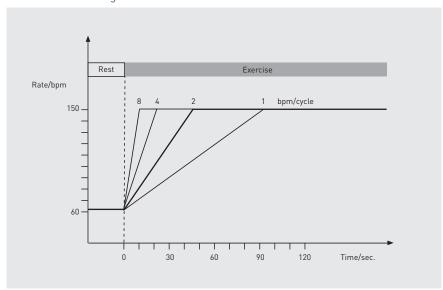
Only signals above the programmed threshold influence rate adaptation.



The **maximum sensor rate** defines the maximum pacing rate (bpm) permitted by the sensor. This parameter is also used as a criterion for the automatic gain function.

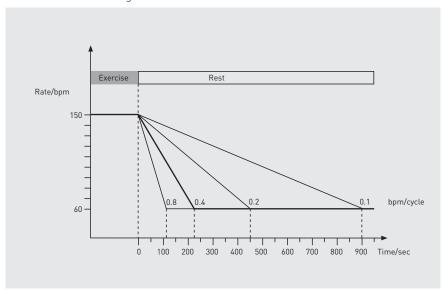
The **maximum rate increase** defines the maximum rate of increase in the pacing rate (bpm/cycle) required to follow the sensor rate.

Rate increase during exertion



The **maximum rate decrease** defines the maximum rate of decrease in the pacing rate (bpm/cycle) required to follow the sensor rate.

Rate decrease following exertion



Calculation of the pacing rate

Adaptation of the pacing rate to the new values is carried out using the maximum rate increase and maximum rate decrease parameters of the accelerometer, in order to prevent erratic rate changes.

Rate smoothing – rate fading – rate stabilization

Pacing modes

The device provides three functions that control an increase or decrease of the pacing rate in a way tolerable for the patient in case of sudden rate changes. The rate fading and rate stabilization functions are used with mode switching in the modes listed below if these functions were previously activated. The rate smoothing function is automatically active and cannot be deactivated:

DDD(R), DDD(R)-ADI(R), DDI(R), VDD(R), VDI(R), VVI(R), AAI(R)

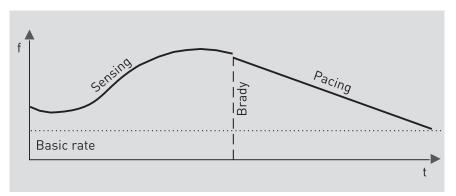
Rate smoothing

The following is a list of applications of rate smoothing using the same rate increase/decrease as rate fading in order to provide a tolerable transition between different pacing rates.

- Switching from basic rate → night rate → basic rate
- Beginning and end of mode switching
- At the end of post mode switching duration
- At the end of post-shock pacing

Rate fading

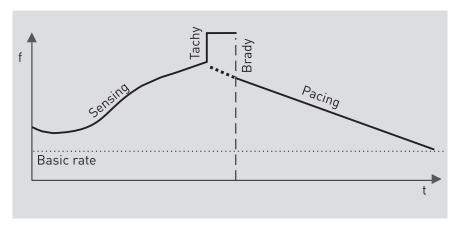
Rate fading results in improved adjustment of the device's pacing rate to the patient's intrinsic rhythm in case of sudden bradycardia.



After four consecutive As, the target rate for the backup rate is calculated from the current atrial rate minus 10 bpm. AES and Ap set the target rate to the value of the basic or sensor rate.

If rate fading is activated, the device calculates a backup rate, which is always active in the background. As soon as the heart rate decreases, the device paces with the backup rate. With a certain delay, the backup rate follows the heart rate according to the programmable rate increase (1; 2; 4; 8 bpm/cycle) and the programmed rate decrease (0.1; 0.2; 0.5; 1.0 bpm/cycle). These settings determine the sensitivity of the controlled rate fading.

Rate stabilization with mode switching

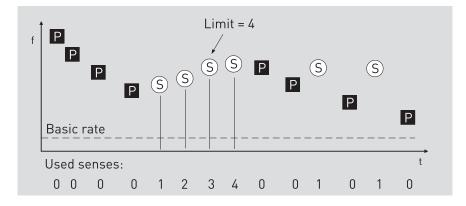


In cases of atrial tachycardia, which result in mode switching, the target rate is set to the sensor or basic rate. The current pacing rate in the ventricle results from the current value of the backup rate.

If rate stabilization is activated with mode switching, the device calculates the backup rate, which is always active in the background. As soon as the rate decreases, the device paces with the backup rate. With a certain delay, the backup rate follows the heart rate according to the programmable rate increase (1; 2; 4; 8 bpm/cycle) and the programmed rate decrease (0.1; 0.2; 0.5; 1.0 bpm/cycle). These settings determine the sensitivity of the controlled rate stabilization with mode switching.

If the pacing rate reaches the heart rate upon rate decrease, at least four consecutive intrinsic cycles above the pacing rate are required to adjust the pacing rate to the last intrinsic event.

This way, rate stabilization is continued during intermittent sensed events.



Four consecutive sensed events are required to activate the function. Individual sensed events have no impact.

Backup rate	Rate at which the device paces in the case of sudden rate decrease. This is 10 bpm lower than the heart rate and follows the target rate upwards at 1; 2; 4; 8 bpm per cycle or falls at 0.1; 0.2; 0.5; 1.0 bpm per cycle if the target rate is lower than the current backup rate.
Target rate	The target rate is either the current rate minus 10 bpm or the sensor/basic rate. The backup rate follows the target rate at the programmed rate increase or decrease.

Pacing Parameters

Setting pulse amplitude and pulse width

Navigation: Parameters \rightarrow Bradycardia/CRT

Objective Optimized pulse amplitude and pulse width values ensure effective and reliable

pacing. The lower these parameter values can be set, the longer the service time

of the device.

Safe and regular pulse The pulse amplitude and pulse width values are continuously maintained during amplitudes and widths

the entire service time of the device. This applies to pulse amplitude values up to

7.5 V. Thus the safety margin is maintained even when the battery voltage

decreases at the end of the device's service time.

Setting pulse amplitude and The pulse amplitude and the pulse width can be set independently for all pulse width

channels.

Evaluate the default parameter values and adjust them if necessary.

Timing Functions

Basic rate during the day and at night

Basic rate during the day

A sensed or paced event starts the basic interval. If a sensed event does not occur during the basic interval, the device emits a pulse at the end of the basic interval. A sensed event inside the basic interval and outside the set refractory period inhibits pacing and restarts the basic interval. Asynchronous modes such as V00 and D00 are excluded.

In the atrial-controlled modes, the basic interval is started by an atrial event. In the atrial-controlled dual-chamber modes, the basic interval is also started by a premature ventricular contraction.

In the ventricular-controlled modes, the basic interval is started by a ventricular event.

Night rate

If the night rate parameter is activated, the device paces at the set night rate during the night. This makes it possible to adapt the pacing rate to the patient's reduced metabolic needs during this time.

The night rate as well as the beginning and end of the night can be set.

At the beginning of the night period, the basic rate and the hysteresis rate are reduced to the night values.

If rate adaptation is enabled, the sensor threshold during the night is increased by one increment (less sensitive). This prevents undesirable rate increases – even in patients who do not sleep soundly.

After the night has ended, the device resumes the basic rate.

Note

Please take into consideration that the patient may travel to other time zones. If this is expected, the night duration should be programmed accordingly shorter or even deactivated.

Note

The internal clock of the device is automatically adjusted to the clock of the programmer at every interrogation. Ensure that the time displayed on the programmer is correct.

Rates and rate hystereses

Rate hysteresis

Promotion of intrinsic rhythm

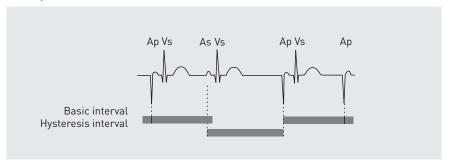
Rate hysteresis can be set to promote the patient's intrinsic rhythm. In this case, after a sensed event, the device not only waits for the duration of the basic interval for a new sensed event, but also for the duration of the longer hysteresis interval before pacing occurs.

The device tolerates an intrinsic rhythm whose rate lies below the basic rate. However, the intrinsic rate must be higher than the rate that corresponds to the hysteresis interval. If a sensed event does not occur within the hysteresis interval, a pacing pulse is delivered at the end of the hysteresis interval. The next interval then corresponds to that of the basic interval or the interval determined by the sensor.

Note

If rate hysteresis is to be used in the DDI mode, the AV delay must be programmed shorter than the intrinsic conduction time. Otherwise, the device paces at the hysteresis rate instead of the basic rate even in the absence of intrinsic activity.

Rate hysteresis

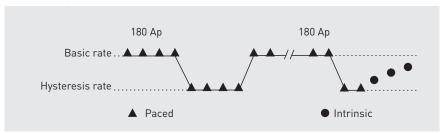


Rate scan hysteresis

This function is a sub-feature of rate hysteresis and promotes the intrinsic rhythm after long periods of pacing. The function is always switched on in combination with the repetitive rate hysteresis.

After 180 consecutive pacing cycles, the ICD reduces its rate to the hysteresis rate for 10 cycles with the purpose of either sensing an intrinsic event in this time and thus inhibiting its own effects, or continuing pacing at the basic rate after this event.

Rate scan hysteresis

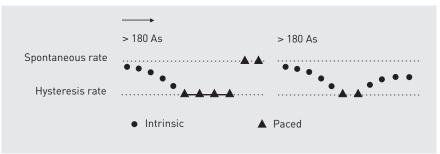


Repetitive rate hysteresis

This function is a sub-feature of rate hysteresis and is always switched on in combination with rate scan hysteresis.

If the intrinsic rhythm falls below the hysteresis rate or ceases entirely (e.g., due to post-extrasystolic pauses), the device first paces only at the hysteresis rate for 10 cycles. Pacing by the device is inhibited as soon as an intrinsic event is detected.

Repetitive rate hysteresis



Rate hystereses

Navigation: Parameters \rightarrow Bradycardia/CRT \rightarrow Basic rate

Objective

Hysteresis functions inhibit pacing in favor of the intrinsic rhythm of the heart.

Rate hysteresis

If the intrinsic rhythm is lower than the basic rate, but higher than the hysteresis rate, pacing is inhibited.

Repetitive hysteresis

Repetitive hysteresis contributes to the prevention of unnecessary pacing in cases in which conventional hysteresis can be overcome – by post-extrasystolic pausing, for example.

Scan hysteresis

Scan hysteresis helps the production of an intrinsic rhythm during longer phases of pacing:

- If scan hysteresis is enabled, the device regularly reduces the pacing rate to the hysteresis rate for 10 cycles after 180 successive pacing events in order to search for intrinsic events.
- If no intrinsic event is sensed during the scan intervals, pacing at the basic rate is resumed by the device (at the sensor rate with active rate adaptation).

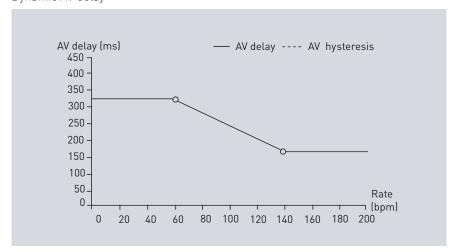
Functions of the AV Delay

Dynamic AV delay

The AV delay defines the interval between an atrial paced or sensed event and the ventricular pacing pulse. If the ICD is programmed to a dual-chamber mode, an intrinsic ventricular event falling within the AV delay will inhibit the ventricular pacing pulse. If not contraindicated, a longer AV delay can be selected to increase the probability of ventricular pulse inhibition.

An AV delay is dynamic when it varies depending on the intrinsic atrial rhythm. The dynamic AV delay provides an independent selection of AV delays for two rate points. The ICD calculates and sets the dynamic AV delay between these two points linearly. The incline of the AV delay curve can be positive or negative here, which provides the possibility of triggering long AV delays with slow rates and short AV delays with fast rates or vice-versa.

Dynamic AV delay

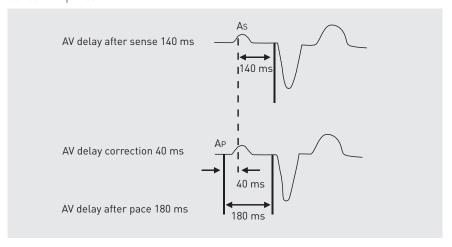


In addition to selecting the preset values (low, medium, or high) for the dynamic AV delay, the dynamic AV delays can be programmed individually or to a fixed AV delay.

Sense compensation

For hemodynamic reasons, it is desirable to maintain a constant period between an atrial and a ventricular contraction and to adjust it to physiologic conditions. For this purpose, sense compensation can be used to shorten the AV delay after an atrial sensed event.

Sense compensation



Setting AV delay

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow AV delay

Objective

Dynamic AV delay simulates natural AV conduction in various stress situations.

Description

The AV delay is the interval between an atrial event and the subsequent ventricular pace. If AV delay is programmed dynamically, it adjusts itself automatically using a rising pacing rate.

AV hystereses

A positive hysteresis extends the AV delay and negative hysteresis shortens it.

See: Setting AV hystereses [Page 117]

Sense compensation

Sense compensation shortens the AV delay after an atrial sensed event to improve the stability of the patient's hemodynamics, in accordance with the patient's specific physiological conditions.

Optimize AV delay

The AV delay can be individually adapted to the requirements of the patient using the AV optimization test:

• Optimized AV delays are determined on the basis of P-wave measurements. The test results are displayed and can be used for pacing and sensing.

See: Optimize AV delays with AV Opt test [Page 237]

Procedure

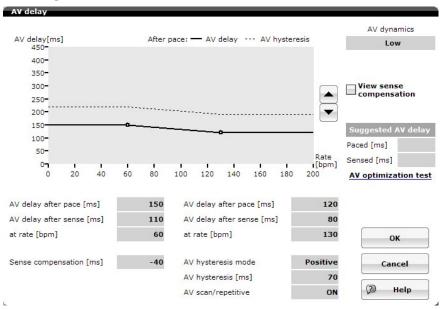
Proceed as follows:

- 1. Select AV delay.
- 2. Select one of the default settings in the AV dynamics field.

 The dynamics of the AV delay are interpolated in the selected rate range.
- 3. Where appropriate, modify the settings by selecting a numerical value, by changing settings with the arrow keys, or in the graph move the upper and lower rate point using the stylus. The setting is now considered individual.
- 4. To show sense compensation in the diagram, if applicable, activate the **[View sense compensation]** check box.
- 5. Select **[OK]** to accept the values.

User interface

AV delay

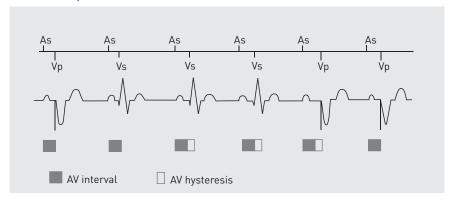


AV hysteresis Positive AV hysteresis

AV hysteresis can be programmed to promote spontaneous AV conduction.

In doing so, the AV delay is extended by a defined range of values after sensing an intrinsic ventricular event. The long AV delay remains intact as long as an intrinsic ventricular rhythm is measured. The short AV delay without extension by the hysteresis value follows after ventricular pacing.

Positive AV hysteresis

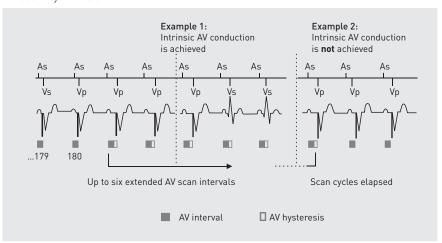


AV scan hysteresis

This function is a sub-function of positive AV hysteresis and promotes spontaneous AV conductions even during longer phases of pacing. The function is always switched on in combination with AV repetitive hysteresis.

After 180 consecutive pacing cycles, the ICD will extend the AV delay for five cycles to the time extended by the AV hysteresis. If the ICD detects spontaneous AV conduction during this time, pacing is withheld until it is needed again. Otherwise, the ICD switches to the short AV delay and repeats the described process after 180 consecutive pacing cycles.

AV scan hysteresis

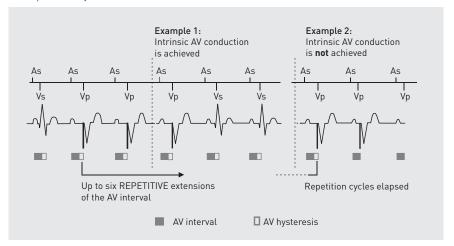


AV repetitive hysteresis

This function is a sub-function of positive AV hysteresis, thereby further improving the chances of successful spontaneous AV conduction. The function is always switched on in combination with AV scan hysteresis.

The extended AV delay after a ventricular paced event remains with the AV repetitive hysteresis for five cycles in addition to the AV hysteresis. If spontaneous AV conduction occurs during one of these cycles, the extended AV delay remains intact. If not, the ICD reverts to the short AV delay.

AV repetitive hysteresis

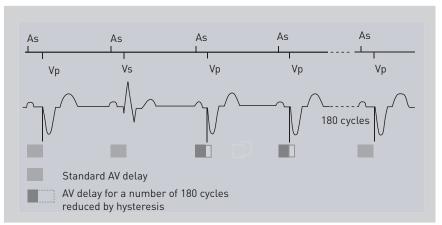


Negative AV hysteresis

This function is intended to suppress intrinsic excitation conduction and promote pacemaker stimulation in the ventricle. This is required for patients with hypertrophic obstructive cardiomyopathy (HOCM) for example or can be considered within the context of cardiac resynchronization therapy for congestive heart failure patients.

The function shortens the AV delay upon occurrence of a sensed ventricular event. The AV delay is shortened by the set value after sensing an intrinsic ventricular event. Following ventricular pacing with short AV delay, the permanently programmed AV delay takes effect without shortening by the hysteresis value.

Negative AV hysteresis



Setting AV hystereses

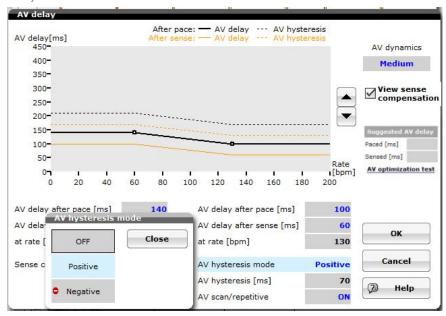
Navigation: Parameters ightarrow Bradycardia/CRT ightarrow AV delay

Objective

- A positive AV hysteresis aims to contain a patient's spontaneous AV conduction for as long as possible, thus ensuring that the contraction sequence is natural. All unnecessary pacing of the ventricle should be avoided.
- A negative AV hysteresis aims to encourage ventricular pacing and allow as little as possible conduction of the intrinsic atrial rhythm; e.g., in cases of hypertrophic obstructive cardiomyopathy (HOCM) or in support of resynchronization therapy.

User interface

AV hystereses



AV repetitive hysteresis

When AV repetitive hysteresis is activated, the AV delay is extended/shortened by the defined hysteresis value after sensing an intrinsic ventricular event.

• If a ventricular paced event occurs, the modified interval for AV delay remains unchanged, in contrast to the case of a normal AV hysteresis.

Positive

- If an intrinsic activity occurs during one of these repetitive cycles, the long AV
 delay remains intact. Only when the repetitive cycles have elapsed without
 spontaneous AV conduction does the pacemaker switch back to the short AV
 delay.
- The AV repetitive hysteresis reduces ventricular pacing, when an intrinsic ventricular event occurs within the extended AV delay.
- The AV repetitive hysteresis maintains the extended AV delay for 5 successive cycles.

Negative

• The repetitive cycles occur with the shortened AV delay. When the preset 180 cycles are completed, the programmed AV delay is restored (extended). An intrinsic ventricular event shortens the AV delay again.

AV scan hysteresis

In case of an AV scan hysteresis, after 180 successive cycles in which one paced event and no ventricular sensed event has taken place, the AV delay switches to the interval extended by the AV hysteresis.

- The long AV delay remains intact for a preset number of (5) cycles. If an intrinsic AV conduction occurs within these cycles, the AV hysteresis remains intact.
- The short AV delay interval resumes only when no ventricular event has been sensed within the number of cycles and instead every one of these cycles ends with a paced event. The counter starts to count successive paced cycles over again from zero. Intrinsic ventricular events (excluding PVC) reset the counter to zero.
- Hence, AV scan hysteresis reduces pacing in situations in which intrinsic conduction exists but does not fall within the programmed AV delay.

AV safety delay

Protection against pulse inhibition

If an atrial pace triggers ventricular oversensing through crosstalk, undesired pulse inhibition in the ventricle can result. Sensing of atrial pulse delivery in the ventricular channel during the AV delay can be incorrectly interpreted as an intrinsic ventricular event. Therefore, the AV safety delay (100 ms) is started after atrial pacing in the DDD(R) and DDI(R) modes.

If ventricular sensing (RVs) occurs after the cross blanking has elapsed but still within the AV safety delay, the ICD paces at the end of the AV safety delay in the ventricle. This ventricular stimulus after 100 ms (the regular AV delay could be longer) is a backup pulse. The backup pulse serves as protection from undesired impulse inhibition after crosstalk.

If the AV delay is shorter than the AV safety delay, pacing occurs at the end of the AV delay. This prevents ventricular pulse inhibition through ventricular sensing of atrial pacing (crosstalk). If AV sequential pacing is observed with an AV delay corresponding to the AV safety delay, this may be evidence of ventricular crosstalk.

Note

In triple-chamber devices, the pacing configuration BiV causes a backup pulse to be delivered first in the chamber that has been programmed as the chamber to be paced first (RV or LV). The programmed VV delay is automatically reset to 0 ms in the case of AV backup stimulation.

Refractory and blanking periods

Refractory and blanking periods

Refractory periods

Refractory periods serve to depict the physiological timing of the heart in the device, in which no pacing pulses are to be expected normally.

Sensed events that occur during the refractory period have no effect on device timing. Exceptions are mode switching and tachycardia detection. With these functions, sensed events within the refractory period are utilized for arrhythmia detection.

Blanking periods

Sensed events that occur during the blanking period have no effect on device timing.

Atrial refractory behavior

The **ARP** is the atrial refractory period after an atrial sensed event (225 ms + sense compensation) or stimulus (225 ms or AV delay, whichever is longer). ARPs are not programmable. They are automatically set.

An atrial, non-refractory sensed or paced event starts the atrial refractory period (ARP). It is not retriggerable by atrial sensed events. Atrial sensed events that occur within the atrial refractory period, but outside the blanking periods (atrial refractory sensed events, Ars) have no influence on device timing.

Post-ventricular atrial refractory period (PVARP)

The PVARP function prevents atrial sensing from being triggered directly after a ventricular event. This prevents a pacemaker-mediated tachycardia (PMT).

- In all P-synchronous modes, a PVARP starts in the case of the following events: RVp and/or LVp
- In all R-synchronous modes, a PVARP starts in the case of the following events: RVp/LVp, PVC, Vs

Auto PVARP

After ending a pacemaker-mediated tachycardia (PMT), PVARP and PVARP after PVC are automatically extended by 50 ms.

The limit for PVARP is:

- Value of the VA criterion + 50 ms
- Minimum automatic setting: 175 ms

If no pacemaker-mediated tachycardia (PMT) is detected within 7 days, the Auto PVARP function automatically reduces PVARP and PVARP after PVC by 50 ms. Once a value that does not trigger a PMT has been found, the PVARP is no longer automatically shortened

Ventricular refractory behavior

The **VRP** is the ventricular refractory period after a ventricular pacing and a ventricular sensed event.

It is not retriggerable by ventricular sensed events during the VRP. PVC starts a ventricular refractory period. The VRP after sensing is set to a fixed value of $200~\mathrm{ms}$.

A ventricular refractory period (VRP) after ventricular paced events is always exactly as long as the ventricular blanking period.

A ventricular stimulus starts the ventricular refractory period (VRP). No ventricular pulse is delivered during the ventricular refractory period. Triggered ventricular paces and safety paces can be delivered during this period. Sensed events outside the ventricular refractory period (Vs) have an impact on device timing. Ventricular sensed events within the ventricular refractory period (Vrs) do not affect device timing.

Ventricular refractory periods are not programmable.

Atrial blanking periods

If the atrial channel is blanked, all incoming atrial sensed events will be suppressed. They do not affect the rhythm and noise evaluation and device behavior. An atrial sensed event starts the blanking period in its own channel; it is not retriggered by a new atrial sensed event. An atrial stimulus starts the atrial blanking period. After a ventricular stimulus, the atrial channel is blanked for the duration of cross blanking.

Note

Additional atrial blanking periods can be an effective means of suppressing ventricular far-field sensing in the atrium (see far-field protection).

Ventricular blanking periods

If the ventricular channel is blanked, all incoming ventricular sensed events will be suppressed. They do not affect the rhythm and noise evaluation and device behavior.

A ventricular sensed event starts the blanking period in its own channel; it is not retriggered by a new ventricular sensed event. A ventricular pulse starts the ventricular blanking period. After an atrial stimulus, the ventricular channel is blanked for the duration of cross blanking.

PMT protection (description)

Overview

- Description of the PMT detection
 - Criteria of the detection algorithm
 - Terminating the PMT
- Setting PMT protection
- Details of PMT confirmation

Objective

PMT protection uses the basic algorithm to inhibit triggering of a pacemaker-mediated tachycardia (PMT).

In the atrial-controlled dual-chamber device modes (DDD, VDD), the device starts PMT protection after the following events:

- Ventricular stimulus
- Premature ventricular contractions

PMT detection

The principle of PMT detection is based on the presence of coupling between a ventricular stimulus and the following atrial sensed event during sinus rhythm. The detection algorithm is based on a constancy in the length of the VA interval (duration between Vp and subsequent As).

Criteria of the detection algorithm

Criterion	Description
1	The mean value of the last eight sequential Vp-As intervals is shorter than the programmed VA criterion.
2	The mean value of the Vp-As intervals is subtracted from each of the eight individual Vp-As intervals. The result is compared with an internal PMT stability criterion and evaluated with respect to a particular margin of fluctuation that can be tolerated. If stability (+/- 25 ms) exists, a confirmation phase follows.

Confirming and terminating the PMT

If	Then
these two criteria are met,	the device automatically changes the AV delay by a defined value.
the following Vp-As interval remains constant,	the PMT is considered to be confirmed.
the PMT is confirmed,	the algorithm for terminating the PMT is initiated with an automatic extension of the PVARP interval for the duration of a cardiac cycle.

Setting refractory periods, blanking periods, and PMT protection

Navigation: Parameters \rightarrow Bradycardia/CRT \rightarrow Refractory period/Blanking Objective

Blanking and refractory periods can prevent false inhibition of the device by interference potentials. The following interference potentials may inhibit the device:

- Retrograde conductions
- Far-field sensing
- Afterpotentials

Overview

The following parameters can be configured for PMT protection, refractory and blanking periods:

- PVARP, PVARP = AUTO, PVARP extension, PVARP after PVC
- Far-field protection after Vs, far-field protection after Vp
- PMT protection

PVARP - description of the parameters

The PVARP lengthens the atrial refractory period (ARP) after a ventricular event (PV = post-ventricular). The total atrial refractory period is divided into the atrial refractory period (ARP) and two other safety intervals – far-field blanking (FFB) and PVARP. A right ventricular extrasystole (RVES) triggers the prolonged PVARP.

- Automatic PVARP
 - In case of a confirmed pacemaker-mediated tachycardia (PMT), the post-ventricular atrial refractory period is automatically extended by 50 ms.
 - This value remains "frozen" and is not further reduced in the absence of PMTs.
 - If PMTs should occur again, then the PVARP is increased further.
- Automatic atrial refractory period
 - The atrial refractory period (ARP) is automatically coupled to the AV delay.
 - The ARP does not drop below 225 ms.
- Refractory periods

Events that occur during the refractory period and are sensed by the device have no effect on device timing. This does not include algorithms used for prevention in the case of atrial tachyarrhythmia (for example, automatic mode switching).

- Far-field protection
 - Far-field protection prevents atrial leads in dual-chamber modes from detecting events in the ventricle (far-field sensing) and interpreting them incorrectly as events in the atrial channel.
 - Events that are sensed in the far-field protection interval do not affect device timing.
 - Far-field protection always has a 16 ms time lead over the ventricular event.
 - When the parameter far-field protection after Vs is programmed to AUTO, the algorithm behaves as follows:

If the patient's heart rate is below the programmed VT rate, the value of the far-field blanking = 75 ms.

If the patient's heart rate is above the VT rate, the value of the far-field blanking = 25 ms. This algorithm reduces unnecessary shock deliveries by specifying the atrial sensing behavior.

The automatic change from 75 ms to 25 ms occurs when VT/VF events are first detected. Two consecutive events shorten the FFB.

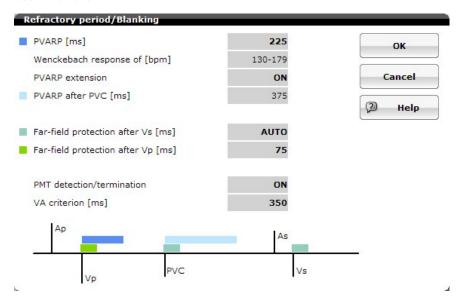
The VT/VF termination (short termination and episode termination) causes automatic change from 25 ms to 75 ms.

Events and safety intervals

The following events trigger the safety intervals:

- Atrial events start the ARP.
- All ventricular events start the far-field protection.
- Ventricular stimuli start the PVARP interval.
- Premature ventricular contractions (PVCs) increase the value of PVARP by 150 ms.

User interface



Purpose of PMT protection

Note

Dual-chamber devices: disproportionately high ventricular pacing rate

Retrograde conduction can lead to a disproportionately high ventricular pacing rate in the case of dual-chamber devices.

To avoid retrograde conduction, consider the following:

- Activate PMT protection.
- Program the VA criterion appropriately.

With its basic algorithm, PMT protection can interrupt the persistance of a pacemaker-mediated tachycardia (PMT).

When the parameter value PVARP = AUTO is set, where a PMT has been confirmed, the PVARP is extended automatically; see also: PVARP – description of the parameters [Page 123]

In the dual-chamber device's atrially controlled modes (DDD, VDD), the device will start PVARP after the following events:

- Ventricular stimulus
- Premature ventricular contractions

PMT detection

In the case of a sinus rhythm, there is normally no coupling between a ventricular stimulus and the subsequent atrial sensed event.

In the case of a PMT, however, there is a coupling between a Vp and a subsequent As (crosstalk).

The detection algorithm is based on a constancy in the length of the VA interval (duration between Vp and subsequent As).

Where a confirmed PMT has occurred, the device will attempt to interrupt it by extending the PVARP.

Ventricular pacing suppression

Ventricular pacing suppression – concept

Why should right ventricular pacing be avoided?

Right ventricular pacing evokes an asymmetrical contraction of the ventricle due to the unphysiological activation of the cardiac conduction system.

Various randomized studies performed with pacemaker and ICD patients have shown that frequent ventricular pacing is connected with an increased risk of congestive heart failure and atrial fibrillation as long-term effects.

Therefore, pacing should only be performed if it is clinically necessary.

Based on this increase in knowledge, it is widely accepted that pacemaker therapy should avoid unnecessary right ventricular pacing.

This particularly applies to patients with sick sinus syndrome (SSS) and/or intermittent AV block.

Which device type is suitable for which underlying disease?

Devices with AAI function are sufficient for patients with intact AV conduction.

However, dual-chamber devices are indicated in most cases for safety reasons if the patient develops an AV block, bradycardia-induced atrial fibrillation, or druginduced bradycardia.

According to the German heart registry, this happens in 83% of the cases. The device should be able to be programmed in such a way that unnecessary right ventricular pacing can be avoided.

Dual-chamber devices are always indicated for patients with AV block. For patients with intermittent AV block, right ventricular pacing should cease in phases of intrinsic AV conduction.

In cases of intermittent or permanent first-degree AV block, a decision has to be made between delayed atrioventricular conduction and pacing with a short AV delay, which is hemodynamically more effective.

Vp suppression: option for avoiding ventricular pacing

- In phases of intact AV conduction, pacing is performed in a mode similar to AAI
- In phases when there is no AV conduction, the mode is switched back to DDD pacing and the right ventricle is paced.

The Vp suppression function enables the device to toggle between these two modes according to the patient's needs.

Ventricular pacing suppression – functioning

Overview

The following topics are described within this segment:

- Activation of Vp suppression
- Mode of functioning
- Switching from DDD(R) to ADI(R)
- Switching criterion and Vs continuity search
- Vs continuity search triggered by a single Vs
- Vs continuity search triggered by a timing interval
- Intelligent search
- ADI(R) mode
- Switching from ADI(R) to DDD(R)
- Switching criterion: 2 s without Vs

- Switching criterion: 2 consecutive cycles without Vs
- Switching criterion: programmable number X out of 8 cycles without Vs
- Summary
- Vp suppression and mode switching
- Vp suppression and high rates
- Vp suppression interactions with other functions and actions

Activation of Vp suppression

The Vp suppression function is activated if the mode DDD-ADI or DDDR-ADIR is selected.

Mode of functioning

Vp suppression supports intrinsic AV conduction by pacing in the ventricle only if intrinsic AV conduction becomes unstable or stops.

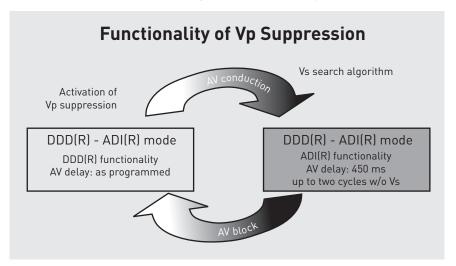
If there is intrinsic AV conduction, the function works in a mode similar to ADI(R).

If intrinsic AV conduction stops or becomes unstable, the function paces in DDD(R) mode with the programmed AV delay in the ventricle.

Automatic mode switching between these two modes provides for maximum intrinsic optimization without doing damage to the patient.

Scan algorithms with a programmed schedule test intrinsic AV conduction whereby the AV delay is extended to 450 ms.

The ADI(R) mode – according to the NBG pacemaker code – describes precisely what the device does in this status. Thus, as opposed to the AAI(R) mode, sensing is also possible in the ventricle in order to switch to the DDD(R) mode and pace in the ventricle in the case of ventricle pauses or unstable rhythms.



Switching from DDD(R) to ADI(R)

If Vp suppression is activated by switching on the DDD(R)-ADI(R) mode, the function initially works in DDD(R) mode, so that a ventricular pace is triggered at the end of the AV delay.

In DDD(R) mode, the device systematically scans to determine whether there is an intrinsic ventricular rhythm.

If no activity is sensed for 30 s within the AV delay, the function starts a continuous scan algorithm called the Vs continuity search.

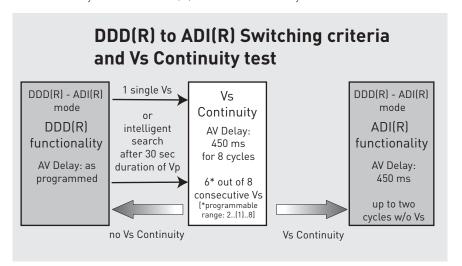
The search for an intrinsic ventricular rhythm can be triggered by 2 different events:

- Sensing of a single Vs event within the AV delay (also PVC)
- No sensing of Vs after 30 s (intelligent search)

Switching criterion and Vs continuity search

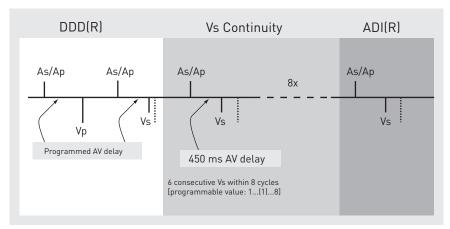
In order to prevent constant switching between DDD(R) and ADI(R), an additional test is performed to verify the stability of the intrinsic ventricular rhythm.

The device only switches to ADI(R) if a stable Vs activity is verified.



Vs continuity search triggered by a single Vs

If the device paces in the DDD(R)-ADI(R) mode according to the set AV delay and senses a single Vs within the AV delay, the Vs continuity test is started.



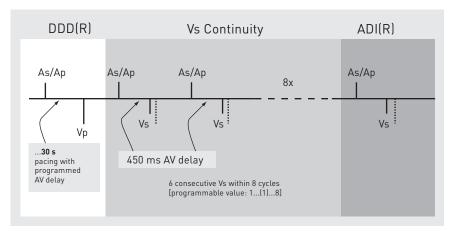
The search is successful if the set number of cycles has been sensed consecutively within 8 cycles. If no further Vs was sensed except for the initial Vs, the device paces for 8 cycles with an AV delay of 450 ms.

As a result, the device will work in the DDD(R) mode with the programmed AV delay until the next Vs continuity test.

If the search was successful and the number of programmed consecutive Vs was sensed, it switches to the ADI(R) mode.

Vs continuity search triggered by a timing interval

If the DDD(R)-ADI(R) mode has been set and the device paces with the programmed AV delay in the ventricle, the initial Vs continuity search begins immediately.



The Vs continuity search runs in the same way within the programmed AV delay as the search triggered by a single Vs.

The condition for switching to the ADI(R) mode is met if the programmed number of Vs is consecutively sensed within 8 cycles.

Intelligent search

The intelligent search serves to avoid frequent scan cycles for patients who have no intrinsic rhythm.

The reason for this is that some patients become symptomatic if the device paces with a long AV delay.

Every time the Vs continuity search is unsuccessful, the timing interval for starting the search is doubled until a limit of 128 min is reached. Then the Vp suppression function will only search every 20 h for intrinsic AV conduction. The scan interval is set to 20 h instead of every 24 h so that the search is initialized at different times of day. The search is carried out at different times of day and night in a 6-day cycle.

The Vp suppression function does not deactivate itself entirely on its own.

Intelligent search time schedule

$$30 \text{ s} \rightarrow 1 \text{ min} \rightarrow 2 \text{ min} \rightarrow 4 \text{ min} \rightarrow \dots \rightarrow 128 \text{ min} \rightarrow 20 \text{ h}$$

ADI(R) mode

The device always works in ADI(R) mode if there is a stable intrinsic rhythm.

If the device works in ADI(R) mode according to NBG nomenclature, pacing is only performed in the atrium (A). Sensing takes place in both chambers (D), but atrial pacing is inhibited (I) if the intrinsic rhythm is higher than the basic rate or the rate specified by the sensor (R).

While working in ADI(R) mode, no ventricular pacing is carried out. If no ventricular sensing occurs within 2 cardiac cycles or within 2 s, it switches to DDD(R) mode.

While the device is working in the ADI(R) mode, sensing is performed in the atrium and ventricle. The AV delay is 450 ms and is not followed by a ventricular stimulus.

Switching from ADI(R) to DDD(R)

If an intrinsic ventricular rhythm is no longer sensed, it switches to DDD(R) mode.

In order to safely account for all situations, there are 4 different criteria which result in switching and they all work independently:

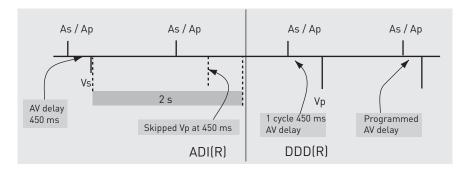
- No Vs for 2 s
- 2 consecutive cycles without Vs
- Pacing support for X out of 8 cycles without Vs (programmable number, default setting: 3 out of 8)
- 15 switches per hour permanently switch to DDD(R) until 24:00 h of the same day.

The criterion that is met first triggers the switch. Regardless of the criterion, switching is AV-synchronous. The ventricle is always paced either using the programmed AV delay or with the AV delay of 450 ms depending on the situation and especially depending on the rate.

Switching criterion: 2 s without Vs

In the example shown below, the 2-second criterion is met first. The 2-second timer always starts at the ventricular sensed event. The ventricular pause is greater than 2 s because the ventricular stimulus is AV-synchronous. In this example, the ventricular pause is about 3 s. Due to the fact that the rate is low (1500 ms), the 2-second criterion is met earlier than the 2-cycles-without-Vs criterion.

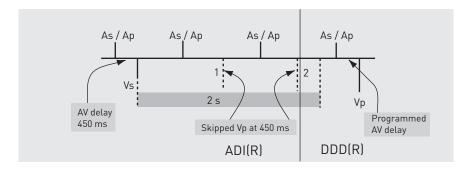
Example: ventricular pause at 40 bpm



Switching criterion: 2 consecutive cycles without Vs

In the example shown below, the 2-cycles-without-Vs criterion is met earlier than the 2-second criterion because the cycle length is 857 ms (70 bpm).

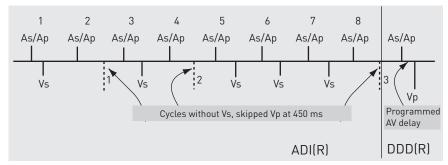
Example: ventricular pause at 70 bpm



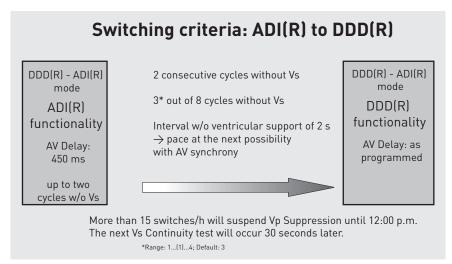
Switching criterion: programmable number X out of 8 cycles without Vs

In order to avoid irregular ventricular rhythms while in ADI(R) mode, only a programmable number of cycles is permissible without an intrinsic event. The default setting is 3 out of 8 cycles. If this criterion is met, it switches to DDD(R) mode.

Example: 3 out of 8 cycles without Vs



Summary



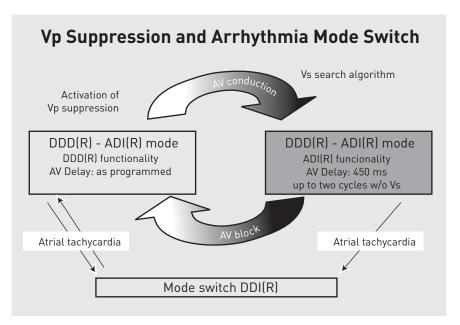
Vp suppression and mode switching

Mode switching is available in the background regardless of the current Vp suppression mode function in order to protect the patient against high ventricular rates. The function is deactivated for the duration of mode switching.

Whenever the mode switching criterion is met, the algorithm switches to the DDI(R) mode regardless of the current functioning of the DDD(R)-ADI(R) mode.

The algorithm remains in DDI(R) mode until the resynchronization criterion is met.

Subsequent to resynchronization from within mode switching, the algorithm always switches to DDD(R) and not to ADI(R) mode to work with defined conditions after a tachycardia.



Vp suppression and high rates

Vp suppression is not connected to specific rate limits like, for example, capture

In the case of high rates, the AV delay would be longer than the VA interval if the AV delay is set to a maximum of 450 ms.

Therefore, the AV delay of 450 ms is reduced depending on the rate to avoid unfavorable hemodynamic situations in the case of high rates.

The exact AV delay dependent on the rate when Vp suppression is activated can be viewed in the diagram of the dynamic AV delay function.

The maximum AV delay is still 450 ms at 100 bpm and is reduced incrementally, reaching a base of 300 ms at 140 bpm, which remains set even at higher rates.

Vp suppression interactions with other functions and actions

As already mentioned above, there are functions with a higher priority than Vp suppression.

The Vp suppression function is interrupted if a function with higher priority starts. After automatic reactivation of Vp suppression, the function always initially works in DDD(R) mode regardless of which mode was active when the Vp suppression was interrupted.

The following algorithms, partial functions, and actions interrupt the Vp suppression function:

- Pacing threshold search of atrial and ventricular capture control
- Mode switching
- PMT detection
- Long-term deactivation when ERI is reached

Setting ventricular pacing suppression

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Vp suppression

Objective

The ventricular pacing suppression function serves to promote the intrinsic ventricular rhythm with AV conduction.

Description

The Vp suppression function supports intrinsic AV conduction. The function can only be set in DDD(R)-ADI(R) mode. In cases of intrinsic conduction, the device works in a mode similar to AAI.

The device switches back to the DDD(R) mode under the following conditions:

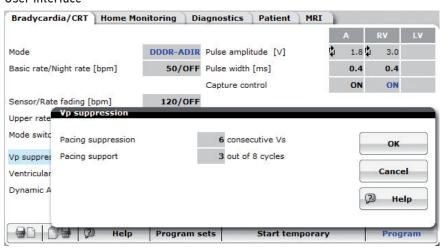
- 2 consecutive cycles without Vs
- X (1-4) of 8 intervals without ventricular support
- Interval without ventricular support for 2 s
- More than 15 conversions per hour deactivate the function for 20 h

Activate the function

Proceed as follows:

- 1. Select Parameters \rightarrow Bradycardia/CRT \rightarrow Mode.
- 2. Select the mode DDD-ADI or DDDR-ADIR. The Vp suppression function is now activated and shows the value ON in the Bradycardia/CRT window.

User interface



Effect

Over the long term, right-ventricular pacing has been shown to cause asymmetrical ventricular contraction due to the unphysiological cardiac conduction. In the long term, the ventricular pacing suppression serves to prevent loss of ventricle synchronization and development of congestive heart failure.

Atrial and Ventricular Capture Control

Atrial capture control

Atrial capture control - concept

Overview

- Objective of atrial capture control
- Function
- Advantages

Objective of atrial capture control

Lead aging, changes to the medication, lead dislodgement and pathological changes can result in changes to the pacing threshold.

Automatic algorithms permit follow-ups to be carried out as efficiently as possible. Automatic measurement of the ventricular threshold and the corresponding automatic adaptation of the ventricular pulse amplitude are functions that have already been used for many years in clinical practice.

This type of automatic algorithm is thus advantageous for measurement of the atrial threshold and the corresponding adaptation of the atrial amplitudes.

Function

The dual-chamber and triple-chamber devices of this device family have an algorithm for atrial capture control that is based on periodic observation and differentiation of atrial signals. The algorithm automatically measures the atrial pacing threshold at a defined time and adapts the pulse amplitude when needed.

Advantages

The following advantages arise from the use of atrial capture control:

Home Monitoring-supported follow-up:

Follow-up can be performed as a Home Monitoring-supported follow-up. One of the requirements for this is presence of the atrial capture control function.

Safety

The atrial amplitude is automatically adapted to increased atrial pacing thresholds, so that atrial exit blocks are avoided.

• Longevity:

The lowest atrial pulse amplitude value is determined by atrial capture control. It is automatically adapted to the current atrial pacing threshold in each case and a safety margin is added. Low values for the atrial pulse amplitude increase the service time of the device.

Automatic pacing threshold measurement

Overview

- Testing principle
- Determining the intrinsic rate and performing overdrive pacing
- Searching for the pacing threshold
- Confirming the pacing threshold
- Automatic capture control
- Programming suggestions

Testing principle

When measuring the atrial threshold, the pulse amplitude is reduced until pacing in the heart no longer triggers a response. As soon as there is no atrial capture response, the intrinsic atrial rhythm takes over and generates a sensing marker, which can be produced using possible retrograde conduction if there is no intrinsic atrial rhythm.

Therefore, the atrial threshold can also be identified in the case of sinus arrest (no intrinsic atrial rhythm) by means of retrograde conduction.

Determining the intrinsic rhythm and performing overdrive pacing

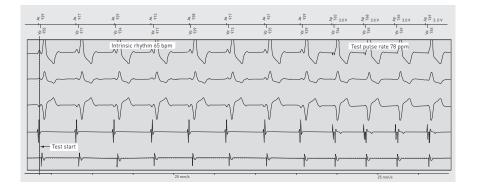
The atrium is paced in order to be able to identify the loss of capture response at a certain amplitude.

Therefore, the intrinsic rhythm is subjected to overdrive pacing amounting to 20% to ensure the atrium is being paced artificially. The intrinsic rhythm is identified using the average rate of the last 4 cycles in each case.

Conditions for overdrive pacing

If	Then
the average atrial rate is higher than the programmed pacing rate,	the atrial pacing threshold test is carried out at a rate which corresponds to the average intrinsic rhythm + 20%.
the average atrial rate is lower than the programmed pacing rate,	the atrial pacing threshold test is carried out at the pacing rate + 20%.
the average atrial rate lies above 108 beats per minute,	the test cannot be carried out at the present time and the atrial pulse amplitude remains at the current value.

Intrinsic rhythm 65 bpm + 20% = test pulse rate of 78 bpm



Searching for the pacing threshold

Pacing mode and AV delay during the test

DDI mode:

Pacing in DDI mode prevents tracking of retrograde conducted P waves, which can occur if the atrial capture response is lost during the pacing threshold test.

In DDD mode, retrograde conducted P waves can trigger pacemaker-mediated tachycardia. Therefore, the test is carried out in DDI mode.

• AV delay = 50 ms

After the AV delay of 50 ms, ventricular pacing is carried out, starting an atrial blanking with the far-field blanking (FFB) value.

Pacing threshold search using amplitude reduction

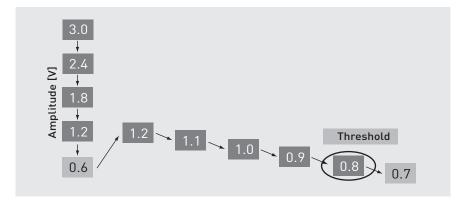
- The pacing threshold search begins at the programmed start amplitude (default setting: 3.5 V). The amplitude is reduced here in 0.6 V increments, until 2 intrinsic atrial events are sensed within 5 cycles (2 out of 5).
- After the first loss of capture response (2 out of 5), the device switches back to the amplitude at which the last capture response took place, in order to perform a more detailed search.
- The test amplitude is decreased in increments of 0.1 V until the device detects a loss of 2 out of 5 possible capture responses for the second time.

This completes the pacing threshold search.

Below 0.6 V, the search is always performed in 0.1 V increments.

The criterion 2 out of 5 was selected because, statistically, at least 2 events within 5 cycles can be sensed outside the far-field protection interval.

Test example: **start amplitude of 3.0 V**; amplitude reduction: 0.6 V increments; loss of capture response at 0.6 V; beginning of detailed search at 1.2 V; amplitude reduction: 0.1 V increments; loss of capture response at 0.7 V; **pacing threshold at 0.8 \text{ V}**.



Test amplitude per test pulse, analysis algorithm, and synchronization pulse

- Each test amplitude is delivered and analyzed 5 times with the same pacing energy for the duration of 5 cycles.
- After two sensed events within 5 cycles, the test sequence is likewise terminated prematurely, because ineffective pacing has occurred and the value has fallen below the pacing threshold.
- After each test pulse sequence with the same pacing energy, a synchronization pulse is delivered to ensure that the AV synchrony is restored after possible loss of pacing.

For technical reasons, the synchronization pulse is even delivered without a loss of capture response.

If no capture response occurs, the synchronization pulse has a pacing energy 0.6 V greater than the unsuccessful test pulse.

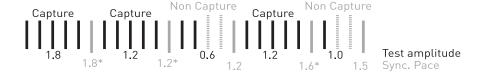
If a capture response occurs, the synchronization pulse has the same pacing energy as the test pulse.

In the test sequence with smaller increments (0.1 V), the pacing energy of the synchronization pulse is increased by 0.5 V.

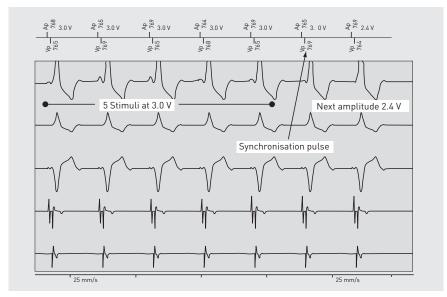
• Premature ventricular contractions have no impact on the test.

Test sequence	Amplitude of the synchronization pulse
Decrease in increments of 0.6 V with capture response	Pacing energy the same as test amplitude
Decrease in increments of 0.6 V without capture response	Pacing energy the same as test amplitude + 0.6 V
Decrease in increments of 0.1 V with and without capture response	Pacing energy the same as test amplitude + 0.5 V

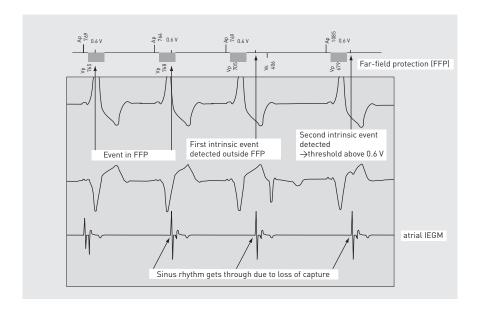
Diagram of the test and synchronization pulses with capture response (capture) and with loss of capture response (non-capture)



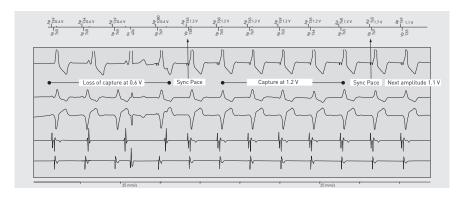
Example: synchronization pulse, 5 stimuli at 3 V and a synchronization pulse



Example: loss of capture response at 0.6 V; only atrial markers outside the programmed far-field protection value are evaluated ${\sf v}$



Example: beginning of the detailed search in 0.1 V increments, switching from 0.6 V to 0.1 V increments of decrementation



Confirming the pacing threshold

The threshold determined at the beginning is confirmed as follows:

• 1st step:

Pacing pulses of 0.3 V above the pacing threshold are delivered within a testing period of 5 atrioventricular pacing intervals.

2nd step:

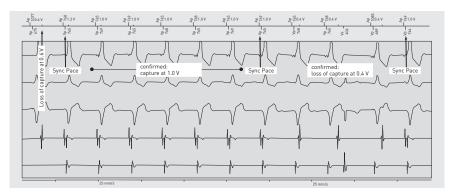
Another test cycle of 5 atrioventricular pacing intervals is carried out at 0.3 V below the pacing threshold.

• The pacing threshold is considered verified if a capture response is identified in the first step and loss of the capture response is confirmed in the second step.

Note

If the pacing threshold is $\leqslant 0.3$ V, pacing markers of 0 V are set in the IFGM

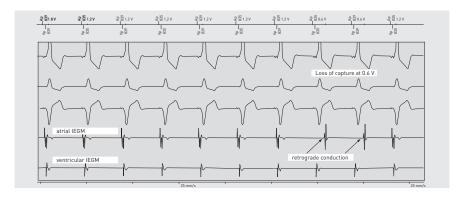
Example verification test: capture response at 0.7 V (= pacing threshold), loss of capture response at 0.6 V, (pacing threshold +/-0.3 V)



Pacing threshold measurement using retrograde conduction in the case of sinus arrest

- Atrial capture control also works if there is no atrial intrinsic rhythm.
- Retrograde conducted P waves, which are caused by ventricular pulses if there are no intrinsic atrial events, suffice for analysis.

Example: sinus arrest with retrograde conduction time of 220 ms



Automatic capture control

- The atrial pulse amplitude is adapted by adding the programmed safety margin (default setting 1.0 V, adjustable) to the measured pacing threshold.
- If no atrial pacing threshold test could be carried out (e.g., at an intrinsic rhythm > 108 bpm), the current atrial amplitude remains valid.
- If atrial capture control is deactivated, the atrial amplitude is calculated by adding the test output amplitude and the safety margin. Default setting: 3.0 V + 1.0 V = 4.0 V.

Note

If atrial capture control is deactivated, an error message is displayed in the Follow-up window and an event message is generated for BIOTRONIK Home Monitoring.

Unsuccessful measurements of atrial capture control are shown in the Home Monitoring statistics as gaps.

Programming suggestions

- The value of the "Threshold test start" parameter does not influence the success of the test (as opposed to ventricular capture control), but decrementing makes it several seconds faster.
- The test is repeated daily at the programmed time.

Note

Make sure there is a sufficient difference between the threshold and the value of the threshold test start parameter, so that pacing threshold changes can be monitored following implantation.

Ventricular capture control

Ventricular capture control – concept

- Components of the algorithm
- Characteristics
- Manual/automatic determination of the pacing threshold
- Terms

Objective

During implantation and follow-up, the necessary pulse amplitude required to depolarize the myocardial tissue is usually measured. This minimum pulse amplitude is identified as the pacing threshold. The pulse amplitude is set twice as

high as the measured pacing threshold by default. The purpose of ventricular capture control is to automatically adjust the pulse amplitude in case of a change in the pacing threshold.

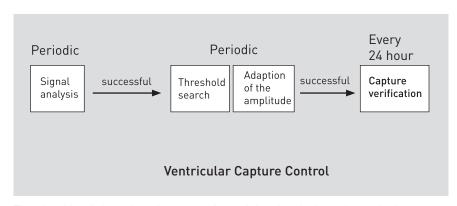
Components of the algorithm

The algorithm is comprised of 3 components:

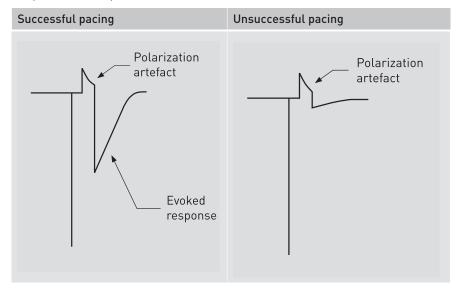
- Signal analysis
- Measurement of the pacing threshold with amplitude setting
- Verification of capture response

All components run periodically. If you activate the ventricular capture control function with ON, all 3 components are run through one after another.

Overview of the algorithm's components



The algorithm is based on the comparison of the signals from the evoked response and the polarization artifact.



Characteristics

The function comprises of the following characteristics:

- The function periodically measures the pacing threshold, automatically adjusts the pulse amplitude, and offers a programmable safety margin.
- The differences in the signal morphology and the evoked response and the
 polarization artifact are used to differentiate between effective and ineffective
 pacing.

Manual/automatic determination

- As the manual method of determining the pacing threshold occurs at long intervals (e.g., every 12 months), a large safety margin must be selected in order to ensure effective pacing.
- An automatic method which checks the efficiency of pacing and periodically
 determines the pacing threshold (every 24 hours) can manage with a smaller
 safety margin, since the pulse amplitude is adjusted to the demand. A smaller
 safety margin may lead to less power consumption and an extended service
 time of the device.

Terms

The following table lists and describes all terms that are used in connection with ventricular capture control:

Term	Description
Evoked response	The evoked response is an intracardiac signal which arises through the excitation of the myocardial tissue. The evoked response is independent from the pulse amplitude and the pacing threshold.
Polarization artifact	A polarization artifact is noise which arises between the lead and the myocardial tissue after delivery of the pacing pulse. The polarization artifact is depen- dent on the pulse amplitude, the structure of the lead tip, and the manner of the implantation.
Signal analysis	Signal analysis is a component of the function which periodically determines whether the evoked response has been correctly recognized and whether the polarization artifact's amplitudes are small enough. If the signal analysis determines that the signal is not useable, then the other components of the function cannot be activated.
Pacing threshold search	A component of the function which periodically determines the pacing threshold. The pacing threshold search can only be performed after a successful signal analysis.
Verification of capture response	A component of the function which classifies a stimulus as effective or ineffective.
Ineffective stimulus	A single ineffective, ventricular stimulus without depolarization (non-capture).
Safety margin	The difference between the pacing threshold and the programmed pulse amplitude is referred to as the safety margin.

Term	Description
Loss of depolarization	The function detects a loss of capture if a series of ventricular stimuli at different AV delays could not depolarize the tissue. In this case, 2 out of 3 consecutive stimuli were not effective.
Threshold test start	The set amplitude at which signal analysis and pacing threshold measurement start. The signal analysis is also carried out for every amplitude.
Pacing pulse (backup stimulation)	Pacing pulse with increased energy following an ineffective stimulus.

Signal analysis

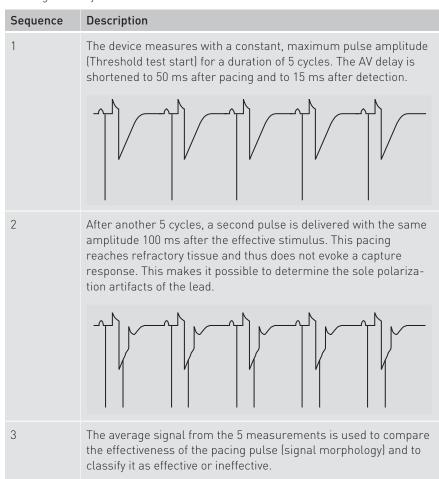
Objective

This sub-function analyzes the signal quality of the ventricular evoked capture response when the stimulus is effective and the polarization artifacts when the stimulus is ineffective.

The function ensures that only undisturbed and suitable signals are evaluated. The signal analysis function works up to a ventricular rate of 110 bpm.

How signal analysis works

The signal analysis sub-function works as follows:

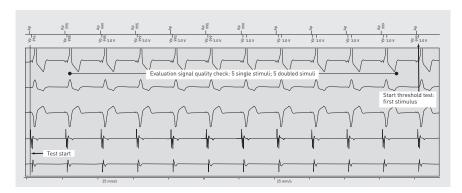


Note

If the signal quality is classified as insufficient, the device temporarily and automatically switches to backup stimulation until a successful measurement can be conducted.

The automatic pacing threshold search only functions at a constant pulse duration of $0.4\ \mathrm{ms}.$

Example: checking signal quality, analysis of evoked responses



Possible scenarios during signal analysis

If	Then
after initial activation signal analysis is completed successfully, but subsequently completed without success,	the pulse amplitude is set to a safe value. This value consists of the most recently measured pacing threshold + a maximum safety margin of 1.2 V if the measured value is greater than half of the start amplitude. If the measured value is less than half of the start amplitude, the value of the start amplitude is set. Signal analysis is conducted again at the next programmed time.

Automatic pacing threshold measurement

Objective

The pacing threshold measurement sub-function enables the pacing threshold with the resulting stimulus to be automatically determined. The ventricular threshold is periodically measured and the pulse amplitude is adjusted if necessary.

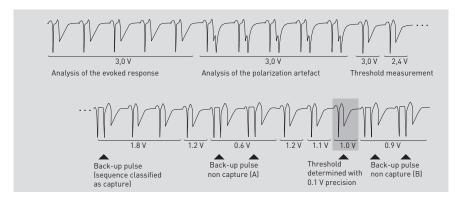
Prerequisite

Only after the signal quality has successfully been checked can the pacing threshold measurement and capture control functions be executed.

How the pacing threshold measurement works

The threshold is determined as follows:

Sequence	Description
1	After successful verification of the signal quality, the pulse amplitude is incrementally decreased with each pace.
	• The amplitude is reduced, first in larger increments (0.6 V), then in smaller increments (0.1 V).
	Each amplitude is tested with 1 stimulus.
	• The AV delay is shortened to 50 ms after pacing and to 15 ms after detection.
2	The incremental decrease of the pulse amplitude continues until a loss of stimulus response (ineffective stimulus) is measured. The last effective pulse amplitude that is measured is accepted and saved as the pacing threshold value.
3	A safety pulse with an increased pulse width energy of 0.6 V and 1 ms is delivered after each ineffective ventricular stimulus. This leads to continuous effective pacing.

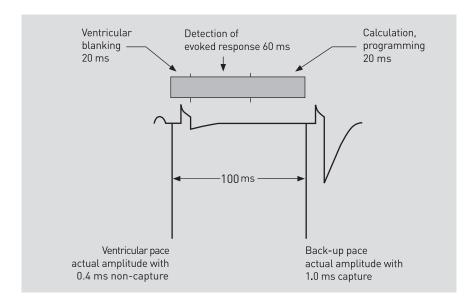


Backup pulse (backup stimulation)

The algorithm checks the effectiveness of every single ventricular stimulus during the threshold test. If an ineffective stimulus is detected, a backup pulse with more energy will be delivered 100 ms after this event. The energy of this stimulus is increased in that the pulse width is increased to 1.0 ms and the pulse amplitude is increased by $0.6\ V$.

Thus, the energy of the backup pulse is higher than the energy of the previous ineffective stimulus.

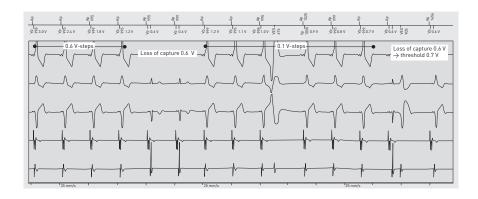
Diagram of the signal analysis when the stimulus is not effective



Automatic determination of the pacing threshold

If	Then
a single ineffective stimulus is detected during the first pulse amplitude decrement (0.6 V),	the pulse amplitude is set to the previous value and is then reduced by 0.1 V in order to determine the pacing threshold.
a single ineffective stimulus is detected during the second pulse amplitude decrement (0.1 V),	the preceding measured value is preselected as possible pacing threshold.
an ineffective stimulus is detected again,	up to 2 more stimuli are delivered with the same pulse amplitude.
2 out of 3 stimuli are ineffective,	the preceding measured value is adopted as the pacing threshold.
	The pulse amplitude is then set to the pacing threshold plus the programmable safety margin.

Example: the pacing threshold test was carried out in less than 20 seconds



Settings

The standard value for the start of the threshold test is 3.5 V and 2.5 with ATM. The pulse width is fixed at 0.4 ms and cannot be changed.

The scan mode is carried out at night just prior to the time of Home Monitoring transmission. This serves to minimize the impact that a highly fluctuating intrinsic rate has on the algorithm.

Setting capture control

Navigation: Parameters \rightarrow Bradycardia/CRT \rightarrow Capture control

↑ WARNING

Pacing may be ineffective if capture control is programmed to OFF or ATM

When capture control is programmed to OFF or ATM, the pulse amplitude is not automatically adjusted. If the pacing threshold increases intermediately under these conditions, pacing may be ineffective.

If the setting is programmed to OFF or ATM, ensure that there is an adequate safety margin when programming the pulse amplitude.

Setting parameters

Proceed as follows:

- 1. Select [Threshold test start] to set the initial value of the pacing threshold measurement.
- Select [Min. amplitude] to prevent the minimum amplitude from falling below a particular value.
- 3. Select [Safety margin] to adjust the safety margin. After successfully making automatic threshold measurements, if capture control = ON, the pulse amplitude is made up of the pacing threshold plus a safety margin.
- 4. Confirm your entries by pressing [OK].

Capture control for triplechamber devices

Capture control for triple-chamber devices works as follows:

Option	Explanation
Activation of capture control for both ventricles	The pacing threshold is determined first for the right ventricle and then for the left ventricle.
Fixing of the right ventricular pacing threshold	Ventricular pacing is temporarily set to right ventricular.
Fixing of the left ventricular pacing threshold	This happens under biventricular pacing where the left ventricle is first paced and the VV delay is set to 50 ms.
	Immediately after measuring the pacing threshold, permanent programmed ventricular pacing is set.

Display capture control status

Display	Description
OK	The capture control or ATM function is activated and operates without errors.

Display	Description
Disabled	Atrial and ventricular capture control are deactivated when the replacement indication ERI is reached or when lead impedance is outside the permitted range of values [200 to 3000 Ω].
Pending	The device could not yet determine a valid pacing threshold. If the measurement fails, the test is repeated after 30 minutes.

Ventricular and atrial capture control – programmable parameters

Parameter overview

Parameter	Range of values and explanations
Capture control	ON; OFF; ATM (monitoring only)
Minimum ampli- tude (atrial)	0.5 (0.25) 4 V The minimum amplitude and threshold test start (maximum atrial amplitude) parameters prevent a certain value of the atrial amplitude from being exceeded or undershot during the threshold search.
Threshold test start (maximum ventricular and atrial amplitude)	2.5 (0.5) 5 V
Minimum ventric- ular amplitude	1 (0.25) 4 V The minimum ventricular amplitude and threshold test start (maximum ventricular amplitude) parameters prevent a certain value of the ventricular amplitude from being exceeded or undershot during the threshold search.
Safety margins of the ventricular and atrial pulse ampli- tudes	Atrial safety margin: 0.5, 1.0, 1.2 V Ventricular safety margin: 1.0, 1.2 V The value of the pulse amplitudes, which is set by the function, is made up of the most recently measured pacing threshold plus the configured safety margin or the programmed initial amplitude + 1.2 V for the ventricle and 1 V for the atrium if the pacing threshold is higher than the initial amplitude (Threshold test start).

Function options

The following options are available for the capture control function:

Options	Explanations
Capture control	ON; OFF; ATM (monitoring only)

Options	Explanations
ON option	This option activates all sub-functions: The pacing threshold is monitored and recorded, and the pacing energy is periodically adapted. This is done with the following:
	Signal analysis (ventricle only)
	Automatic pacing threshold search
	Verification of capture response (ventricle only)
OFF option	This setting deactivates the entire capture control function.
Automatic threshold moni- toring (ATM) option	The pacing threshold is monitored and recorded at periodic time intervals. This is done with the following:
	Signal analysis (ventricle only)
	Automatic pacing threshold search
	Accordingly, no periodic adaptation of the pulse amplitude is performed.

When selecting the ATM or OFF options, make sure that a sufficient safety margin is selected when setting the pulse amplitude since there is no automatic tracking of the pulse amplitude for these options.

Atrial and ventricular capture control comparison

A comparison of differences between atrial and ventricular capture control

Atrial capture control	Ventricular capture control
The pacing threshold is determined using sensing markers.	The pacing threshold is determined by beat-to-beat measurement of evoked responses.
The reduction of the start amplitude of the pacing threshold test (Threshold test start) has no impact on the test result and makes the test faster.	The reduction of the start amplitude of the pacing threshold test (Threshold test start) from 3.5 V to 2.5 V increases the chances of success because the polarization artifacts are smaller in the leads. In addition to this, it makes the test faster.

Antitachycardia Functions

Behavior upon reaching the upper rate

Upper rate

In the atrial-controlled dual-chamber modes, the upper rate (UTR) determines the maximum ventricular rate triggered by P waves.

The upper rate must be set to a value tolerable by the patient for an extended period of time. The upper rate determines the minimum interval between a sensed or paced event and the subsequent ventricular paced event.

A reduction of the pacing interval to correspond to that of the upper rate may also be initiated at rest (e.g., upon sensing atrial extrasystoles, myopotentials, or other interferences). Therefore, programming of a low upper rate may be indicated for patients with increased vulnerability.

Wenckebach or 2:1

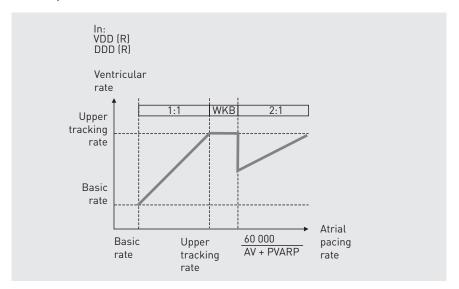
In the DDD(R) and VDD(R) modes, either Wenckebach response or 2:1 response is available depending on the programming of the AV delay, the PVARP, and the upper tracking interval.

Wenckebach response

• If the end of the AV delay falls in the upper tracking interval, ventricular pacing occurs at the end of the upper tracking interval.

2:1 response

• The high-rate atrial event occurs in the ARP, the FFB, or the PVARP. The AV delay is not started.



Special characteristics of the Wenckebach response

As part of the Wenckebach response, the device switches to ventricular timing in addition to atrial timing. A VA interval starts after a ventricular event (Vs, Vp) to avoid extension of the Wenckebach response due to atrial timing.

The timing in the device ensures that the Vp following the VA interval and the atrial stimulus can be emitted at the end of the AV delay. This enables a defined exit from the Wenckebach response at any time.

In the Wenckebach response, the device counts the number of consecutive Wenckebach cycles. If more than four Wenckebach cycles are detected, a shortened VA interval is started after Vp to guarantee the constancy of the ventricular rate.

The short VA interval in this instance is calculated from the ventricular interval of the upper rate minus the AV delay (or the AV safety delay). Once the Wenckebach response has come to an end, the device counter is reset.

Upper rate in the atrium

The upper rate in the atrium is intended to prevent atrial pacing from being carried out during the vulnerable period after an atrial sensed event during the post-ventricular atrial refractory period. This function is intended to assure that the next atrial stimulus is delivered outside of the heart's natural atrial refractory period.

Therefore, an upper rate is started in the atrium with values of 175, 200, or 240 bpm following an AsPVARP.

The atrial intervals have the following values with four possible settings:

- OFF
- 175 bpm = 342 ms
- 200 bpm = 300 ms
- 240 bpm = 250 ms

The next Ap can only be delivered after the atrial interval has passed.

This means that the atrial stimulus is delayed especially in cases in which sensor rates are high.

To guarantee the stability of the ventricular rate as best as possible, the AV delay can be shortened to the AV safety delay (at the most) when the basic interval is extended.

Note

If mode switching is activated, no atrial stimulus takes place in DDI mode with activated atrial upper rate at the end of the sensor or basic interval.

Upper rate

Navigation: Parameters \rightarrow Bradycardia/CRT \rightarrow Upper rate

Description

In all of the triggered pacing modes, the upper rate limits the pacing rate triggered by atrial sensing.

The settings help prevent the conduction of atrial tachycardias to the ventricle.



Triggering the ventricle: conduction of atrial tachycardias

Intrinsic atrial tachycardias can be transmitted to the ventricle from the device at a rate of up to 170 bpm.

- Reduce the upper rate response.
- Adjust the mode switching parameters.
- Program a ventricular-controlled mode (DDI, WI, VDI, or similar).

Device response

Note

The response of the implanted device at the upper rate (Wenckebach (WKB) or 2:1) is pre-set via a combination of several parameters including AV delay and PVARP. They cannot be set directly.

- Wenckebach response occurs when the intrinsic rhythm exceeds the upper rate.
- 2:1 response occurs when the intrinsic rhythm exceeds the rate resulting from the following: 60,000 divided by AV delay plus PVARP.

Displaying results

The display in the Wenckebach response of field (from n to m bpm) is the rate range in which the implanted device exhibits the Wenckebach response.

Atrial upper rate

The upper rate in the atrium should prevent atrial pacing from occurring in the vulnerable period of the atrium after an atrial sensed event during PVARP. The upper rate in the atrium should therefore ensure that the next atrial stimulus is delivered outside the natural atrial refractory period of the heart.

Mode switching - concept

Objective

The conduction of high atrial rates and atrial tachycardias to the ventricle is effectively suppressed with a device algorithm.

This function is especially suited for patients with irregular atrial signals (atrial flutter, atrial fibrillation), thus preventing conduction of the high atrial rate.

Description

When a tachycardia episode occurs, the device automatically switches from an atrial-controlled to a ventricular-controlled mode.

Sensing is based on the continuing evaluation of the last 8 atrial intervals. When X out of 8 intervals reveal an atrial rate that is above the programmed intervention rate, the onset criterion is fulfilled and mode switching automatically follows.

Atrial-controlled mode	Ventricular-controlled mode after mode switching
DDD(R), DDD-CLS, DDD(R)-ADI(R)	DDI(R)
VDD(R)	VDI(R)

The device offers algorithms that effectively suppress the conduction of high atrial rates and atrial tachycardias into the ventricle:

Mode switching with X/Z-out-of-8 algorithm

Resynchronization

The device runs in the programmed non-atrial mode until the resolution criterion (Z-out-of-8) is satisfied.

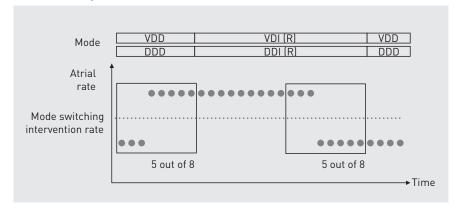
When Z out of 8 intervals lie below the programmed intervention rate, the atrial tachycardia is considered to be over, and the pacemaker automatically switches back to the originally programmed atrial-controlled mode.

The X or Z counter is reset to zero after every completed switching.

The X-out-of-8 criterion prevents, for example, unnecessary mode switching in cases of atrial extrasystoles or unstable atrial signals.

Furthermore, this algorithm can be employed to determine the speed at which a de- and resynchronization with ventricular depolarization takes place. The intervention rate is programmable.

Mode switching



Post-mode switching: rate and duration

In order to avoid reentry of atrial tachyarrhythmias after mode switching, dual-chamber and triple-chamber devices provide the option of pacing at a higher basic rate following resynchronization of mode switching.

The required parameters are as follows:

- Post mode switching rate
- Post mode switching duration

The ICD then generally uses the permanent program parameters for the post mode switching duration. Only the basic rate parameter corresponds to the set post mode switching rate.

Rate stabilization with mode switching

The rate stabilization parameter during mode switching uses the same algorithm as the rate fading parameter for increasing and decreasing the pacing rate relative to the intrinsic rhythm, see Rate smoothing – rate fading – rate stabilization [Page 107].

Mode switching

Navigation: Parameters ightarrow Bradycardia/CRT ightarrow Mode switching

Objective

The conduction of high atrial rates and atrial tachycardias to the ventricle is prevented through the use of mode switching, for example, from DDD to DDI on the basis of X/Z-out-of-8 algorithm.

Description

- An atrial tachycardia is considered detected where the X-out-of-8 onset criterion is fulfilled. The 8 currently most recent atrial intervals are evaluated for detection purposes.
- During detection the device switches into ventricularly controlled mode. This mode remains active until the resolution criterion (Z-out-of-8) is fulfilled.
- If Z out of 8 intervals are below the programmed intervention rate, the device automatically switches off into the originally programmed atrially controlled mode.

Meaning of parameters The mode switching parameters have the following meanings:

Parameter	Meaning
Intervention rate	Rate at which an atrial tachycardia is detected
Mode	Ventricular-controlled mode the device switches to
Mode switching: Ven. pacing	Configuration of ventricular pacing for mode switching Set CRT parameters: see Setting ventricular pacing [Page 93]
Change of basic rate	Rate for the duration of mode switching
Post ModeSw rate	Rate at which pacing is required after mode switching ends. This rate is higher than the basic rate and should therefore prevent any relapse of the previous atrial arrhythmias.
Post ModeSw duration	Duration of the post mode switching rate
Onset criterion	Total atrial intervals above the intervention rate (X- out-of-8): leads to mode switching
Resolution criterion	Total atrial intervals below the intervention rate (Z- out-of-8): terminates mode switching
Rate stabilization during mode switching	 This prevents any rapid fall in the ventricular rate: To configure the required ventricular rate, the sensed atrial rate is not used. Instead, the mean sensed ventricular rate minus 10 bpm is used as the pacing rate. If no ventricular rate is sensed, then the basic rate is used for mode switching.

Patient Data, Diagnostics, and Home Monitoring

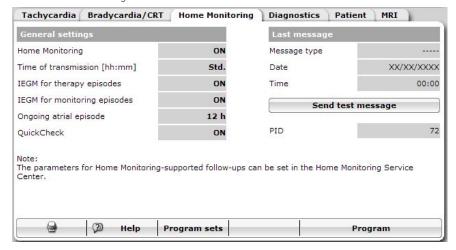
Setting Home Monitoring

Navigation: Parameters \rightarrow Home Monitoring

Objective In the Home Monitoring tab you can make the settings for data transmission

for the Home Monitoring function.

User interface The Home Monitoring window



General settings group box

The following parameters, among others, can be set in the ${\tt General}\,$ settings group box:

Parameter	Description
Time of transmis- sion	Time of day at which the message from the device to the CardioMessenger and from there to the BIOTRONIK Home Monitoring Service Center is sent. Std. = to a default time in the early hours of the morning – which will depend on the serial number of the device.
IEGM for therapy episodes	Determine whether the IEGM of a therapy episode should be transmitted to the Home Monitoring Service Center.
IEGM for moni- toring episodes	Determine whether the IEGMs of the monitoring episodes should be transmitted to the Home Monitoring Service Center. Monitoring episodes are episodes that are not treated with therapy, e.g. SVT, atrial episodes, or VT monitoring episodes.
Ongoing atrial episode	Determine whether an atrial tachycardia should be considered a sustained atrial episode, and, if so, after how much time. If the system has classified an episode as sustained, this information is transmitted to the Home Monitoring Service Center with an event message.
QuickCheck	Activate QuickCheck to send a follow-up data request from the Home Monitoring Service Center to the device. The request is triggered in the Home Monitoring Service Center. The prerequisite is that QuickCheck has been programmed to ON in the device. More details can be found in the technical manual and in the help of the Home Monitoring Service Center.

Last message group box

The following data, among others, can be found in the Last message group box:

Parameter	Description
[Send test message]	Checks the data transmission function.
PID	PID is the ID number for the device and is required to initialize Home Monitoring at the BIOTRONIK HMSC.

Setting diagnostic functions

${\bf Navigation: Parameters} \rightarrow {\bf Diagnostics}$

Objective

Make your settings for the various parameters for statistics and IEGM recordings in the $\tt Diagnostics$ tab.

Recordings

Among the parameters to be set in the Recordings group box are:

Parameter	Description
For AT/AF	Determine whether AT/AF episodes are to be recorded.
	The Advanced ON parameter value extends the time window for medical history.
For SVT	Determine in this field whether episodes classified as SVT are to be recorded.
For nsT	In this field, define whether or not non-sustained tachycardia (nsTs) should be counted and represented in IEGMs even when they do not fulfill the VT or VF detection criterion. For more information on nsT see: Non-sustained tachycardia (nsT) [Page 157]
For CRT pacing interrupt	Determine in this field whether interruptions in CRT pacing are to be represented in IEGMs.
Periodic recording [days]	If Home Monitoring = OFF (Setting Home Monitoring [Page 154]), you can use this field to set the cycle duration of periodic IEGM recordings. The recordings are displayed under: Recording episodes → Episodes .
IEGM configuration	For triple-chamber devices, set the channels for recordings. FF indicates the far-field derivation between the RV shock coil and the housing.

Statistics

In the Statistics group field, set the following parameters:

Parameter	Description
Start resting period and Resting period duration	The resting period is a daily time period in which the minimum intrinsic heart rate is recorded as the resting rate. The results can be seen under: $\textbf{Diagnostics} \rightarrow \textbf{HF monitor}$.
AV delay adj. sensing test	 In the pacing modes DDD(R) or VDD(R), an AV delay can be fixed for the automatic P/R wave measurement in order to be able to sense intrinsic signals.
	OFF: The AV delay is assumed from the permanent program for the duration of the automatic P/R measurement.

Setting thoracic impedance

See Thoracic impedance [Page 156]

Thoracic impedance

Navigation: Parameters \rightarrow Diagnostics \rightarrow Thoracic impedance (TI)

Objective

Thoracic impedance measurements may be useful for patients with a risk of decompensated heart failure.

Usually decompensated heart failure is accompanied by edemas, which can be detected effectively via a reduction in thoracic impedance. The devices in this product family can measure thoracic impedance and transmit this information to the BIOTRONIK Service Center via Home Monitoring. In addition, the impedance trend can also be displayed on the programmer: Display HF monitor statistics [Page 197].

Details Thoracic impedance measurement – details [Page 157]

Thoracic impedance measurement - details

Navigation: Parameters ightarrow Diagnostics ightarrow Thoracic impedance (TI)

Technical implementation of impedance measurement

- The function is synchronized with R-waves and is based on a shock impedance measurement with sub-threshold stimuli.
- The measurement is made between the housing and the distal shock coil.
- The average daily impedance measurement values are stored in the device.
- Via the daily transmission made using Home Monitoring, the data are sent to the BIOTRONIK Home Monitoring Service Center, where they are displayed.
- The impedance measurements are displayed as thoracic impedance trend. Display HF monitor statistics [Page 197]

Non-sustained tachycardia (nsT)

Navigation: Parameters ightarrow Diagnostics ightarrow Recording episodes ightarrow For nsT

Details

- Non-sustained tachycardia (nsT) consist of a total number of VT intervals that are shorter than the value programmed for the detection counter, and which therefore do not generate a detection.
- The nsT detection counter takes in all intervals that fall within one of the programmed tachyarrhythmia zones.
- An nsT is detected when in case of short termination (5 out of 5 non-tachycardia intervals) the nsT detection counter is greater than or equal to 1.
- Any detected nsT triggers an IEGM recording and is counted by the nsT detection counter.
- The total number of nsTs that have occurred during the monitoring interval is displayed as a trend.
- In this trend a distinction is made between slow and fast nsTs. For this purpose, a running mean value is created from 4 successive intervals. If the shortest mean value is less than 220 ms, then the associated nsT is considered a fast nsT and otherwise as a slow nsT.
- Counter and IEGM are transmitted to the BIOTRONIK Home Monitoring Service Center
- When the For nsT parameter is set to OFF, then IEGM recording and the associated counters and statistics will also be switched off.
- The nsT detection counter will be reset on detection (of VT, VF, SVT, VT1 monitoring) and not incremented during the episode.

Patient and device data

Navigation: Parameters \rightarrow Patient

Objective

The following can be done in this tab:

- In case of a new implantation:
 - Entering the patient data and storing them in the device
- In case of a follow-up:
 - View the patient data interrogated by the device, correct errors if necessary, and print out for the report.
- In case of a device change:
 - Import the data from the prior device (for example, name, date of birth, and information on the leads) into the new device.

This data is used for unique patient identification and the allocation of follow-ups stored in the programmer. It has no impact on the therapeutic or diagnostic functions of the device.

Save data in the implanted device

Select **[Program]** in order to save this data permanently in the implanted device and to make it available for follow-up care.

Importing data

Proceed as follows:

- 1. Select [Import].
- 2. Select the patient data that you want to import.
- 3. Select [OK].

Note

The serial number of the previous device is also imported. It is sent to the Home Monitoring Service Center (HMSC) with a message from the new device.

If the patient's previous device was registered with the Home Monitoring Service Center, the HMSC recognizes the device change and shows this to the HMSC user.

Introduction	160
Criteria for the Use of Home Monitoring	162
Home Monitoring Parameters	166
Types of device messages	167
EGM-Online HD	169

Introduction

With BIOTRONIK's Home Monitoring function, patients can be treated even more effectively. All Home Monitoring devices are equipped with a small transmitter and are designated with the letter "T" (VR-T, VR-T DX, DR-T, HF-T).

All functions and features of the basic device, such as pacing and sensing functions, preset parameters, or memory functions, are unaffected by the Home Monitoring function.

When using BIOTRONIK Home Monitoring, the information transmitted from the device can be viewed in the Home Monitoring Service Center and printed there as a status report (PDF file). This keeps you permanently informed of your patient's cardiac status.

A transmitter receives messages from the device and transmits them to the Home Monitoring Service Center. At the Center, the data are processed and are made available via a secure Internet connection.

The Home Monitoring function can be used for the entire service time of the device or for shorter periods, such as several weeks or months.

The most important components of Home Monitoring are the device, the transmitter, and the Home Monitoring Service Center.

Device

The power of the device's transmitter is very low, so that the patient's health is not affected in any way. The resulting small transmission range requires the use of a special transmitter to forward the device data to the BIOTRONIK Service Center.

The patient's device data are sent to the transmitter at regular intervals. With Home Monitoring, the distance between the device and the transmitter should not be less than 20 centimeters (7 inches) and not more than two meters (6 feet).

The device can send three different types of messages:

- Test message (triggered by the programmer)
- Trend message (daily message and Home Monitoring-supported follow-up)
- Event message

In addition, periodically recorded IEGMs can be transmitted at configurable times for Home Monitoring-supported follow-up:

• Appointments for Home Monitoring-supported follow-ups can be scheduled via the HMSC.

Further information: Setting Home Monitoring [Page 154], Home Monitoring-supported follow-up [Page 163].

Transmitter

The transmitter CardioMessenger® SMART functions like a cellular phone and transmits the messages received from the device via the cellular phone network to the Home Monitoring Service Center. The battery of the CardioMessenger® SMART enables battery-operated usage for up to 24 hours. The CardioMessenger® SMART can also be used with the included charging station.

Home Monitoring Service Center

At the Home Monitoring Service Center, the device messages transmitted by the transmitter are analyzed. The analysis criteria are specific to the particular device and can additionally be individually customized for each patient. The results of the

analysis are presented as monitoring findings on the secure internet platform. They can trigger notifications about the receipt of the device message which are sent to the attending physician via SMS or e-mail.

Internet platform

The BIOTRONIK Home Monitoring Service Center is the internet platform where patients' current findings are presented clearly and are accessibly. The detail view contains specifics about the findings as well as the medical history for every patient.

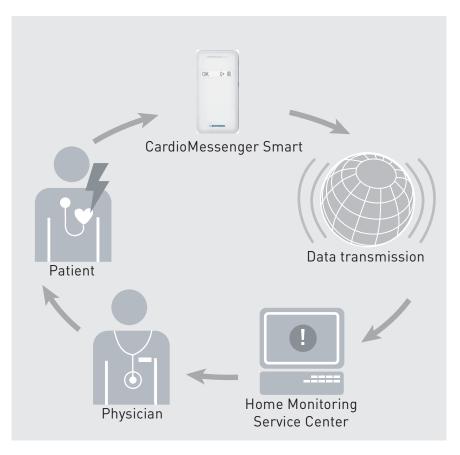
Programmer

You must activate the BIOTRONIK Home Monitoring function in the programmer and register the device with the BIOTRONIK Home Monitoring Service Center.

Further information about activating Home Monitoring on the programmer can be found here: Setting Home Monitoring [Page 154].

For information about registering Home Monitoring, see the technical manual for the BIOTRONIK Home Monitoring Service Center. For information about registering a device, see the online help for the Home Monitoring Service Center.

Home Monitoring concept



Criteria for the Use of Home Monitoring

Intended use

The general intended medical use is to make diagnostic information available to physicians. The Home Monitoring Service Center is a diagnostic tool. It can be consulted for decisions on further therapeutic actions. The therapeutic effect of devices that transmit data is not affected because the Home Monitoring Service Center has no direct effect on the device. Patient review via Home Monitoring has no effect on the therapy of concomitant cardiovascular diseases. This must still be performed according to guidelines.

The specific intended medical use is to make data available for the following purposes:

- · Diagnostics of rhythmologic functions
- Analysis of the effectiveness of therapies delivered by the device
- Monitoring of the technical status of the device and the lead(s)
- Assessment of further therapeutic measures, especially regarding follow-ups

Prerequisites

The technical prerequisites for access to the functions are described in the manual for the BIOTRONIK Home Monitoring Service Center.

Indications

The approved indications and contraindications for ICDs are identical, regardless of whether or not the Home Monitoring function is available. There is no absolute indication for the use of the Home Monitoring Service Center.

However, every patient with an indication for an ICD could benefit from using Home Monitoring and its individualized therapy options. The Home Monitoring Service Center can be used as a diagnostic tool for all patients who have a BIOTRONIK implanted device with Home Monitoring function and who have been equipped with a corresponding transmitter by their physician. The indication for using the Home Monitoring Service Center can include, but is not limited to the following:

- The patient must be monitored in the postoperative phase.
- The patient has a history of paroxysmal or intermittent atrial arrhythmias.
- The patient has an exceptionally high incidence of ventricular tachycardias.
- The patient has marginal sensing thresholds and/or pacing thresholds. Lead impedances are outside of the normal range.
- The patient's medication has been changed.
- The patient resides in a remote location.
- The patient has transportation issues.
- The device is nearing the end of its battery service time (ERI or EOS).

Contraindications

There are no contraindications for the use of the Home Monitoring Service Center as a diagnostic tool because it has no effect on the diagnostic or therapeutic functionality of the device. However, proper use of Home Monitoring requires the

complete cooperation of the patient. A further prerequisite is that the physician has access to the Home Monitoring Service Center. The Home Monitoring system is not recommended for use in the following situations:

- The patient is unable to correctly operate the system due to physical and/or mental conditions.
- There is no cellular phone network roaming partner of T-Mobile available in the patient's vicinity.
- The clinic or practice has no internet access that is regularly maintained.
- The physician is unable to use the internet or there is no personnel qualified to analyze the collected Home Monitoring data.
- The clinic or practice is unable to contact the patient if therapeutic measures are required.

Home Monitoring-supported follow-up

Monitoring using the Home Monitoring function is not intended to replace regular in-office appointments with the physician required for other medical reasons.

Home Monitoring-supported follow-up can be used to functionally replace inoffice follow-up under the following conditions:

- The patient was informed that the physician must be contacted if symptoms worsen or if new symptoms arise despite the use of the Home Monitoring function.
- Device messages are transmitted regularly.
- The physician decides whether the data transmitted via Home Monitoring with regard to the patient's clinical condition, as well as the technical state of the device system, are sufficient. If not, an in-office follow-up needs to be performed.

Possible early detection due to information gained via Home Monitoring may necessitate an additional in-office follow-up. For example, the data may indicate at an early stage lead problems or a foreseeable end of service time (ERI). Furthermore, the data could provide information about previously unrecognized arrhythmias or necessary modification of the therapy by reprogramming the device.

For devices whose programmed parameters cannot be displayed or adequately displayed in the Home Monitoring Service Center, documentation of the programming should be used as a reference.

Follow-up intervals

Follow-ups must be performed at regular, agreed upon intervals.

- Following the lead ingrowth phase (approximately 3 months after implantation), the first follow-up must be carried out by the physician using the programmer (in-office follow-up).
- The next in-office follow-up should be performed annually and no later than 12 months after the last in-office follow-up.

Extraordinary Home Monitoring-supported follow-up with QuickCheck

For the latest ICD product generations of the 7 series, the QuickCheck function is available for unscheduled transmission of Home Monitoring follow-up data.

The following section "Device interrogation with QuickCheck" refers to settings you configure in the Home Monitoring Service Center.

Device Interrogation with QuickCheck

The QuickCheck function is available for the latest ICD product generations.

The QuickCheck function allows sending a request for Home Monitoring follow-up data to the device. Usually the request will be answered within 15 minutes. A current data set is then immediately available.

QuickCheck is used in the following situations:

- The patient contacts his doctor. Using the additional data, the doctor would find out about the condition of the patient.
- The doctor needs current, additional data for other reasons, and does not want to wait to receive data transmitted at the next scheduled Home Monitoring-supported follow-up.

The [Request] button to request for additional data is located on the [Patient profile] / [QuickCheck] tab.

After the request, the following process will run:

- The Home Monitoring Service Center sends the request to the CardioMessenger. Prerequisite: The CardioMessenger is switched on and ready to receive. It is located preferably at a place where it can also be seen during transmission in the night; usually it is the bedside table of the patient.
- The CardioMessenger sends the request to the device. Prerequisite: The patient is in the immediate vicinity of the CardioMessenger. For example, the patient may sit on their bed next to the bedside table.
- The device compiles the data usually required in a Home Monitoringsupported follow-up and sends the data to the Home Monitoring Service Center via the CardioMessenger.
- The Home Monitoring Service Center informs the doctor about the receipt of data.

Scope of functions of Home Monitoring

Monitoring of system integrity:

- Battery status, battery voltage
- Detection and therapy activation

Monitoring of lead integrity:

- Impedance in the atrium and ventricle
- Shock impedance

Bradycardia and tachycardia rhythm and therapy monitoring:

- Sensed event and paced event counter
- Detected episodes
- Delivered therapies
- Success of ATPs and shocks

QuickCheck

 You can directly send a follow-up data request from the Home Monitoring Service Center to the device using the QuickCheck function. How to activate the QuickCheck function can be found here: Setting Home Monitoring [Page 154], General settings group box [Page 154].

The QuickCheck function is only available for 7 series ICDs.

Warnings and precautions

Recognized safety warnings and precautions for ICDs are applicable and are independent of Home Monitoring. However, there are specific precautions for Home Monitoring.

Please follow the specific warnings and precautions for Home Monitoring in the BIOTRONIK Home Monitoring Service Center manual and the patient device manual.

Home Monitoring Parameters

Parameters: description and settings

The meaning and setting of the Home Monitoring parameters can be found under: Setting Home Monitoring [Page 154]

Types of device messages

Devices with the Home Monitoring function send device messages at fixed times or after certain events have occurred. Message transmission can be triggered as follows:

- Trend message
 - The time of day (daily) triggers the message.
- Event message
 - The event triggers the message.
- Message with periodic IEGM for Home Monitoring-supported follow-up

Trend message

In the programmer, you can configure the time at which the daily device message is transmitted to the transmitter. The standard setting is a time during which the patient is sleeping because the patient will then be near the transmitter.

This setting usually should not be changed.

The length of the time interval (monitoring interval) is not programmable, but is preset to daily. A data set is generated in the device for each monitoring interval.

Event message

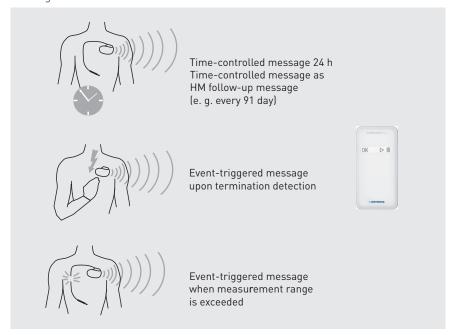
When the device detects certain cardiac and technical events, an event message is sent to the transmitter. The triggering events are adjusted to the specific device. You can go to the Home Monitoring Service Center on the internet to partially configure whether these events should trigger a notification and to which address the notifications should be sent via e-mail or SMS.

Events can trigger monitoring findings. For many events, you can select whether a red, yellow, or no finding is triggered. Color coding is applied to the findings in the Home Monitoring Service Center (internet platform). Some events (e.g., ERI) are always coded red. Notifications are sent if communication channels have been stored (e-mail, SMS) and if the event is coded accordingly. A notification is always sent for a red monitoring finding. With yellow monitoring findings, it depends on whether the HMSC user has set whether to receive a notification for this particular type of event.

Message with periodic IEGM for Home Monitoring-supported follow-up

This message type sends a periodically recorded IEGM and additional data from the device so that a Home Monitoring-supported follow-up can be performed. The point in time for this message is set either in the Home Monitoring Service Center or on the programmer's interface.

Message transmission



QuickCheck message

For the latest ICD product generations of the 7 series, the QuickCheck function is available for unscheduled transmission of Home Monitoring follow-up data, see Device Interrogation with QuickCheck [Page 164].

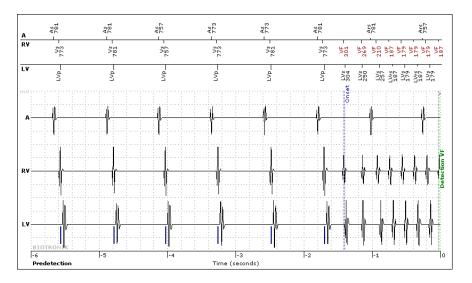
IEGM-Online HD

Depending on the device type, the IEGM sent by Home Monitoring consists of the following:

- Episode details
- Right atrial marker channel
- Right ventricular marker channel
- Left ventricular marker channel
- Right atrial morphology
- Right ventricular morphology
- Left ventricular morphology
- Far-field (FF) ECG as a leadless ECG instead of an external ECG (recording between the housing and the shock coil) together with RA and RV morphology or RV and LV morphology
- Transmission of up to 4 IEGMs daily (up to 2 IEGMs each for monitoring and therapy episodes with prolonged recording of the medical history)

Up to three channels are transmitted depending on the selection.

IEGM and marker channel



2.6 Recordings

Objective	171
Recordings, Basics	172
Memory Management – Details	173
Evaluating Episodes	174
Evaluating IEGM Episodes	177
Episode List, IEGM Marker Texts	179
Episode List, Evaluating Details	181
Evaluating the Shock List	182
Evaluating the Counter	184
ATP Statistics	187

Objective

The Recordings function is a long-term memory that supports the therapy monitoring of ICDs with the following features:

- Storage of tachycardia events with differing origins, with IEGM recording and marker channels
- Storage of periodic IEGMs and marker channels
- Visualization of the complete shock history:
 - Shock energies and impedances
 - Charge time of all charging cycles
- Numerical list of all detections and therapies since the implantation and last follow-up
- The ATP statistics consist of recordings of delivered ATP attempts classified as successful or unsuccessful. If the ATP optimization parameter is active, the therapy sequence is re-sorted according to successful effectiveness. Accelerating ATP attempts are blocked if the ATP optimization parameter was activated. Blocked ATP therapy sequences can be unblocked in this window.

There is a message in the Follow-up window if no ATP attempt is available in a VT zone anymore due to blocking.

Recordings, Basics

Navigation: Recordings \rightarrow Episodes.

Interrogation and display

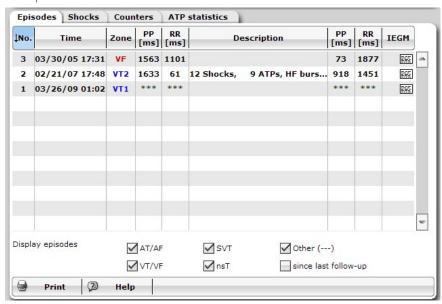
When you select [Recordings], the Episodes tab will display the initially obtained episode list.

Highlighted events

Episodes or IEGMs which have not yet been opened or read are indicated in bold type in the Episodes tab.

User interface

The Episodes tab



Memory management

The recordings are summarized in a single list, which is populated from 5 separate memory segments with the following events:

- VT and VF episodes with therapy
- AT and AF episodes with therapy
- VT1 monitoring, SVT, AF and AT monitoring
- Periodic IEGM, technical recordings
- nsT

For more information see: Memory Management – Details [Page 173]

Memory/memory segment: When the maximum capacity is reached, the oldest entry is overwritten with the newest.

Memory Management - Details

Memory segment capacity

The total memory capacity is spread among the segments as follows:

Memory segment	Number of episodes	Duration (min)
VT and VF episodes with therapy	60	40
AT and AF episodes with therapy	10	4
VT1, AT, AF monitoring, SVT	20	8
Periodic IEGM, technical recordings	40	6
nsT	20	2

Technical recordings

- Between two follow-ups, the following events (only the first in case of several) trigger a recording:
 - Atr. pacing impedance out of range
 - RV amplitude low (= less than 1.5 x minimum threshold)
 - RV pacing impedance out of range
 - LV pacing impedance out of range
 - Shock impedance out of range
 - Atr. threshold test unsuccessful
 - RV threshold test unsuccessful
 - LV threshold test unsuccessful
 - Start RV pacing: applies only at basic rate, but not where there is a rate increase due to rate adaptation or where rate fading is occurring
 - RV lead monitoring
 - > 30 short intervals within 24 h
 - Ongoing high ventricular rate: mean ventricular rate within 24h > 100 bpm (HVR)
- The following event (only the first in case of several) for the day triggers a recording:
 - CRT pacing interrupt: loss of BiV pacing (triple-champer devices) due to maximum ventricular trigger rate

Evaluating Episodes

Navigation: Recordings \rightarrow Episodes

Sorting the displayed data

- Default setting: The entries are in chronological order. The most recently saved entry is displayed at the top of the table.
- Sort the listed entries either in ascending or descending order by clicking on the field showing the relevant column heading. An arrow next to the column header indicates the direction of sorting.

Filtering the display

Filter the episode display with the help of the check boxes in the table footer.

Information relating to episodes

Taken individually, the entries in the Episodes tab mean the following:

Column header	Description
No.	Ordinal number of the episodes in the order of occurrence
Time	Date and time of detection
Zone	Arrhythmia zone which was identified during initial detection

Column header	Description	
PP [ms] (before/after therapy)	PP interval in milliseconds based on the sliding mean value of the last four PP intervals	
RR [ms] (before/after therapy)	RR interval in milliseconds based on the sliding mean value of the last four RR intervals	
Description	 Episode: Monitoring: no therapy was set for the respective zone Periodic recording: IEGM recording for Home Monitoring Regular episode with therapies: n Shocks: number of shocks n ATP: number of ATPs OFF: magnet was applied during episode Details on technical recordings Between two follow-ups, the following events (only the first in case of several) trigger a recording: Atr. pacing imp. out of range RV amplitude low	

Column header	Symbol	Description
IEGM		An IEGM has been saved for the episode: Click on the icon to display the IEGM, and the episode will be retrieved; see also: Evaluating IEGM Episodes [Page 177].
		Details have been saved for the episode: Click on the icon to display the details; see also: Episode List, Evaluating Details [Page 181].

Evaluating IEGM Episodes

Navigation: Recordings \rightarrow Episodes \rightarrow IEGM

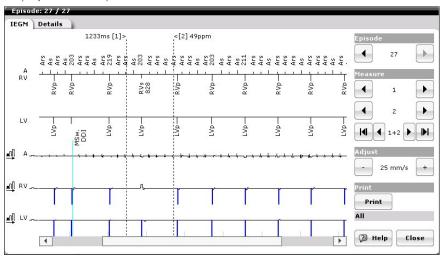
Displaying IEGM episodes

Proceed as follows:

Step	Action
1	Select the IEGM symbol in the Episodes tab:

User interface

Display of IEGM – episodes



Legend

The IEGM shows the following information for an analysis:

Event	Marker channel	IEGM
Initial detection, redetection	Type of detectionDetected arrhythmia zone	Vertical, dotted, green bar through all IEGM channels
Charging phase of capacitors	-	Solid, horizontal black bar above the IEGM channels
Shock	Energy valueImpedance value	Vertical red bar in the respective IEGM channel

Event	Marker channel	IEGM
Paced event	 Marker Pacing and ATP type with interval size in ms 	Blue bar in the lower half of the IEGM channel (also ATP)
Sensed event (used for timing)	Marker that is half as long as other barsInterval size	_
Refractory sensed event (not used for timing)	 Marker that is one quarter as long as other bars Interval size 	-

Marker texts

For an explanation, see Episode List, IEGM Marker Texts [Page 179]

Episode List, IEGM Marker Texts

Marker text legend

The following information is displayed for an evaluation:

Group	Abbreviation	Marker
Atrium	As	Atrial sensed event
	Ars	Atrial refractory sense
	As (PVARP)	Atrial sensed event in PVARP
	Ар	Atrial paced event
	AT	Detection of atrial tachycardia
Right ventricle	RVs	Right ventricular sensed event
	RVrs	Right ventricular refractory sensed event
	RVp	Right ventricular paced event
	PVC	Premature ventricular contraction
Left ventricle	LVs	Left ventricular sensed event
	LVp	Left ventricular paced event
VT/VF	VT1	VT1 episode
	VT2	VT2 episode
	VF	VF episode
	AFib, AFlut, SinusT	SVT episode
	 Det. VT1 Det. VT2 Det. VF Det. SVT Rdt. VT1 Rdt. VT2 Rdt. VF 	VT/VF episode: • Detection • Redetection
	Term	Termination of an episode
ATP therapy	• Burst • Ramp	ATP type

Group	Abbreviation	Marker
Mode	Perm. + mode	Mode of permanent program
	MSw + mode	Mode after mode switching
	PSh + mode	Mode of post-shock program
ECG/IEGM	FF	Far-field ECG/IEGM
	A	Atrium
	RV	Right ventricle
	LV	Left ventricle

Episode List, Evaluating Details

Navigation: Recordings \rightarrow Episodes

Displaying episode details

Proceed as follows:

Step	Action
1	In the episode list, select the symbol:
	(See: Evaluating Episodes [Page 174]).

Evaluating episode details

The tab shows the following information for an evaluation:

Episode	Description of episode
Zone	Arrhythmia zone
Measured Onset in V	Difference in percentage between the RR interval leading to detection and the last RR mean value (calculated from the four preceding RR intervals)
Measured stability in V	Fluctuations of the last four tachycardia intervals
MorphMatch counter	Percentage of events with VT morphology out of all evaluated events in this episode
Redetections	Number of redetections in the arrhythmia zones
ATP	Number of delivered ATPs
Shocks	Number of delivered shocks
Max. energy	Maximum energy charged for therapy shocks
ATP One Shot	Number of ATPs delivered in VF
Detection	Time of detection
Termination	Time of termination
Duration	Duration of episode (between detection and termination)
Remark	 Induced: arrhythmia triggered manually canceled: episode canceled by magnet application Explanation of the classification of an SVT Reference to errors detected in the IEGM recording Details on technical triggers

Evaluating the Shock List

Navigation: Recordings \rightarrow Shocks

Evaluating the shock list

Proceed as follows:

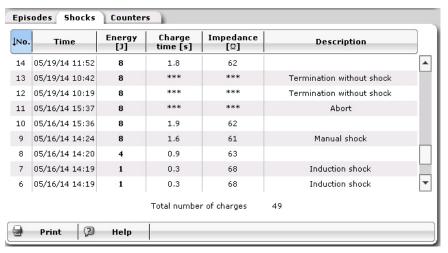
1. Select the Shocks tab.

Sorting the displayed data

- Default setting: The entries are in chronological order. The most recently saved entry is displayed at the top of the table.
- Sort the listed entries either in ascending or descending order by clicking on the field showing the relevant column heading. An arrow next to the column header indicates the direction of sorting.

User interface

The Shocks tab



Shock list

The displays in the shock list mean the following:

Column header	Description
No.	Ordinal number of the shocks and charges in the order of delivery
Time	Date and time of delivery
Energy	Programmed energy (in Joules)

Column header	Description
Charge time	Capacitor charge time (in seconds)
Impedance	 Shock impedance measured during shock delivery (in Ω) If the measured impedance is greater than 150 Ω or less than 25 Ω, the system indicates: > 150 < 25 *** indicates one of the following: Impedance invalid Reform Charge canceled, e.g., due to termination
Description	 Termination without shock: spontaneous termination detected upon shock confirmation Manual shock: shock was triggered manually (during an electrophysiological examination) Induction: Shock: shock was delivered for tachycardiac induction (during an electrophysiological examination) Emergency shock: emergency shock delivered Automatic cap reform: capacitors automatically charged for maintenance Manual reform: capacitors manually charged for maintenance Reversed: shock delivered with reverse polarity Abort: shock delivered or reforming aborted

Total number of charges

The total number of charges is indicated in the table footer: ${\tt Total}\$ number of charges.

Evaluating the Counter

 ${\bf Navigation: Recordings } \rightarrow {\bf Counters}$

Objective

Use the Counters tab to get an overview of the frequency and numerical $% \left(1\right) =\left(1\right) \left(1\right) \left($ distribution of the various detections and therapies.

Description

The table shows counters for all detections and the rapies separately for the time $% \left(1\right) =\left(1\right) \left(1\right) =\left(1\right) \left(1$ periods $\ensuremath{\mathsf{Detections}}$ since last follow-up and $\ensuremath{\mathsf{Detections}}$ since implantation.

Meanings

The information displayed in the Detections since last follow-up and Detections since implantation fields as well as in the Therapy since last follow-up and Therapy since implantation fields have the following meaning:

Field	Classification
Zone	Arrhythmia detected in: Atr. mon.: atrial tachycardias without therapy Atr. ther.: atrial tachycardias SVT: supraventricular tachycardias without therapy VT1 mon.: ventricular tachycardias in VT1 without therapy VT1 ther.: ventricular tachycardias in VT1 VT2: ventricular tachycardias in VT2 VF: ventricular fibrillation
SVT details	 SVT diagnosed as: AFlut: atrial flutter AFib: atrial fibrillation SinusT: sinus tachycardias 1:1: conductions at a ratio of 1:1
Therapy since last follow-up and Therapy since implantation	Delivered therapies: • ATP in AT/AF • HF burst in AT/AF • ATP in VT • ATP One Shot • Shock Therapy success: • Successful: with therapy success • Unsuccessful: without therapy success • Delivered: total

ATP Statistics

Navigation: Recordings \rightarrow ATP statistics

Objective

Use the ATP statistics tab to display an overview of the therapy success or failure of the delivered ATP attempts.

Description

The table shows recordings of all ATP1 and ATP2 therapy attempts delivered in the VT1 and VT2 therapy zones.

The recordings are sorted and listed in the order of their therapeutic success.

Note

If the ATP optimization therapy parameter is programmed to ON, the display follows the specifications of the ATP optimization parameter. This parameter sets successful ATP therapies for the next therapy delivery ahead in the order and withholds therapy attempts, that caused acceleration of a tachyarrhthmia. This ATP delivery sequence is maintained until the next in-office follow-up.

See also: ATP optimization – details [Page 68]

The recordings are deleted as soon as the ATP parameters are reprogrammed.

Meanings

The displays in the fields have the following meaning:

Field	Classification
Zone	ATP delivered in: • [VT1] • [VT2]
ATP	Displays the ATP type
Sequence	Delivered ATP therapies are assigned numbers corresponding to their order of success if ATP optimization is active. If ATP optimization is activated, blocked therapy sequences are marked as "blocked".

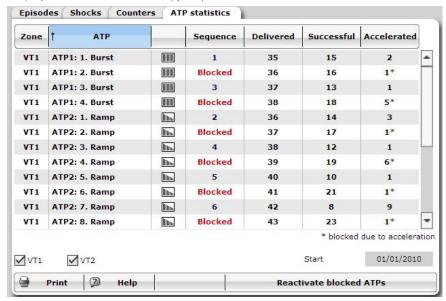
Field	Classification
Delivered	Number of therapy deliveries of the respective ATP attempt
Successful	Classification: successful therapy deliveries of the respective ATP attempt
Accelerated	Classification: Acceleration of the VT with the respective ATP attempt If ATP optimization is activated, the counters of blocked therapy sequences are marked with *. Counters that are not marked have either been recorded with deactivated ATP optimization, or have been reactivated during follow-up.

Reactivating blocked ATPs

Select the **[Reactivate blocked ATPs]** button to reactivate the ATP therapies that are blocked by ATP optimization.

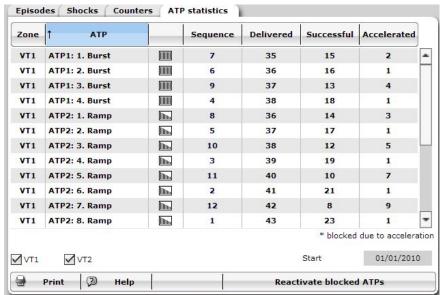
User interface: ATP optimization activated

Display with blocked ATP therapy sequences



User interface: ATP optimization deactivated

Display with unblocked ATP therapy sequences



General Considerations	191
Statistics Classes	192
Evaluating Statistics	195

General Considerations

Common features of the statistics

All statistics share the following features:

- Interrogate statistics
 - The statistics memories are read when the device is initially interrogated.
- Start statistics
 - When statistics are restarted, this deletes all statistics memories in the device. However, data transmitted to the programmer beforehand remain saved there until the end of the session.
- Start and duration
 - Long-term trends have a maximum recording duration of 240 days. The first recorded data is then overwritten. The start date in all long-term trend graphs can be read on the left side. Histograms are automatically restarted with each new interrogation of the programmer. The histogram duration is displayed in the window title on Follow-up → Details.
- Auxiliary line function
 - An auxiliary line function is provided in the statistics windows to help interpret trends and histograms. Along the displayed auxiliary line, the absolute and percentage values of the respective statistics are displayed for the selected time or histogram class.

Recording duration of the statistics

The displayed recording duration of statistics can include the following time period:

The time span between the start of recording and the time of interrogation

Some event counter data is recorded for the entire statistics recording period.

General notes regarding all trend statistics

The axes of the trend statistics are automatically scaled by the programmer.

The legends of the trend statistics and the histograms are automatically annotated depending on the device and the configured functions.

 $48\mbox{-hour}$ recordings are always up-to-date recordings of the past $48\mbox{ hours}$:

• The oldest data is overwritten after 48 hours.

Statistics Classes

The numerous statistics functions that save the data and the special events occurring between follow-ups in the device are assigned to various statistics classes according to content.

Objective

To transmit the data saved in the device to the programmer in order to evaluate it and to use it in optimizing diagnostics and therapy.

Description

- The counters for statistics functions are activated after transmitting a program.
- These statistics are suspended when a ventricular tachycardia episode occurs.

Transmitting statistics

All statistical data are automatically transmitted to the programmer and saved on it upon first interrogation.

Selecting statistics for diagnostics

Navigation: Diagnostics

Overview

The following actions can be performed with the Diagnostics function:

- Interrogating statistics:
 - Statistics are always interrogated during initial interrogation of the device.
- Displaying statistics
- Selecting statistics
- Evaluating statistics
- Update statistics by reinterrogation of the device
- Delete statistics by restarting

Interrogating statistics

On first interrogation from the start screen, all statistical data on the device (except data from the More diagnostics tab) are transmitted to and saved on the programmer.

Selecting statistics

Select a statistic as follows:

- 1. Select [Diagnostics] to call the function. The various classes of statistics available are shown under the associated tabs in the Diagnostics window:
 - Timing
 - Atrial arrhythmia
 - HF-Monitor (long-term trends for the diagnostics for cardiac resynchronization therapy)
 - Short-term trends of the last 48 h
 - More statistics for diagnostics
- 2. Select the statistics class that you want to look at, for example, Timing. All corresponding statistics are displayed in a window as histograms and trends.

Selecting and displaying other statistics

Select the other statistics as follows:

- Select Diagnostics

 More diagnostics to access the function.
 The various statistics summarized in the More diagnostics tab are shown in the group box with the same name.
- 2. Press one of the buttons, for example, Pulse amplitudes. The corresponding histogram or the trend is displayed.
- 3. Touch the buttons to switch between the various functions of the statistics. The corresponding data is displayed.
- 4. Tap on the magnifying glass icon in the graph to see the magnified image of the contents.

Update statistics by device reinterrogation

The statistical data is updated when it is reinterrogated. This reinterrogation will replace the device values previously displayed on the programmer with the current device values.

- 1. Select [End], to return to the start screen and confirm your action with [OK].
- 2. When telemetry contact (RF or programming head application) has been established, the device is reinterrogated and the statistics are updated. The updated data is displayed in the Diagnostics window.

Delete statistics by restarting

To completely delete available statistics from the device, proceed as follows:

1. Select [Start statistics] to initialize all counters of the statistics (reset to 0). The current display is not deleted by pressing the [Start statistics] button. The new statistical data is first shown when the device is reinterrogated.

Note

Trends are not deleted after follow-up The oldest recordings are overwritten after 240 days.

Histograms and counters are restarted after each follow-up. The restart takes place at the set Home Monitoring time, even if Home Monitoring has not been activated.

Using the statistics

Navigation: Diagnostics

Displaying the statistics

The statistics feature shows recorded data such as events, event sequences, and classifications as follows:

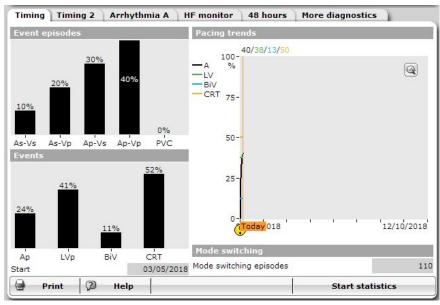
- Graphical display as histogram
- Numerical (absolute) quantity
- Occurrence expressed as a percentage
- Graphical display as trend curve

Using the histograms

A vertical auxiliary line and, on some statistics, two additional arrow keys allow you to navigate (to the right and to the left) through certain histograms. The corresponding values of the histogram are displayed at the location of the auxiliary line. Proceed as follows:

Туре	Action
1	Press on an area of the histogram on the screen. A vertical auxiliary line will appear, displaying the respective values.
2	Some statistics can also be navigated using arrow keys. Press the arrow keys [>>] and [<<]. The auxiliary line is moved gradually.
3	Tap on the magnifying glass icon in the graph to see the magnified image of the contents.

Example Timing tab with statistics



Evaluating Statistics

Displaying Timing Statistics

Navigation: Diagnostics o Timing

Navigation: Diagnostics \rightarrow Timing 2

Overview

- The following trends and histograms are available for the timing statistics:
 - Event episode and events; see also **Follow-up** → **Details**: Event episodes
 - Pacing trends as long-term trends for 240 days;
 see also Follow-up → Details: Long-term trends
- The following trends and histograms are available for the timing2-statistics:
 - Rate histograms
 - AV histograms

When a statistic function is selected, the statistic function opened last is displayed. This applies to the entire follow-up of a device.

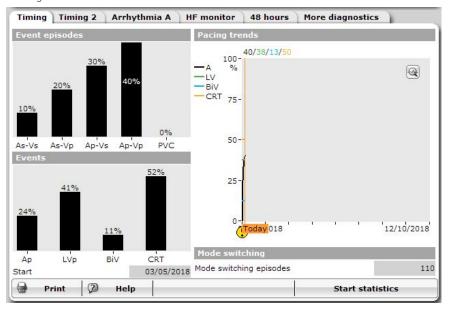
Note

Trends are not deleted after follow-up The oldest recordings are overwritten after 240 days.

Histograms and counters are restarted after each follow-up. The restart takes place at the set Home Monitoring time, even if Home Monitoring has not been activated.

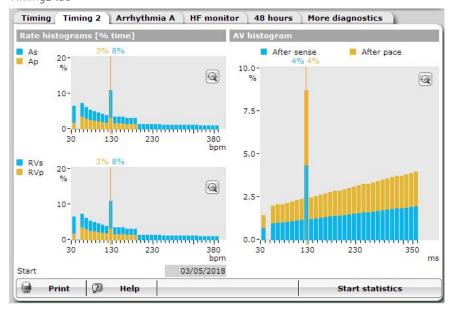
Displaying timing statistics

Timing tab



Displaying timing2 statistics

Timing2 tab



Displaying atrial arrhythmia statistics

Navigation: Diagnostics ightarrow Arrhythmia A

Overview

The following statistics are available for atrial arrhythmias:

- Arrhythmia burden
 - Total number of episodes since starting the statistics
 - Accumulated arrhythmia burden expressed as a percentage since starting the statistics
 - Duration and temporal distribution of the tachyarrhythmia episodes within the last follow-up period
 - Number of atrial tachyarrhythmia episodes per day
 - AT/AF activity duration trend per day in %
- Ventricular reaction
 - Histogram of rates with percentages of pacing and detection
 - Maximum and mean rate trend

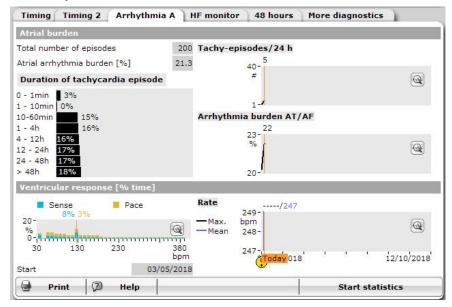
The recording duration usually begins with the initial start of the statistics after implantation. When the Statistics function is restarted during a follow-up – by pressing [Start statistics] – all previous statistical data is deleted and recordings are restarted from the beginning.

Note

Histograms and counters are restarted after each follow-up of the device. The restart takes place at the set Home Monitoring time, even if Home Monitoring has not been activated.

User interface Atrial

Atrial arrhythmia tab



Display HF monitor statistics

Navigation: Diagnostics \rightarrow HF monitor

Overview

The following HF monitor statistics are displayed as a long-term trend:

- Mean heart rate
- Mean heart rate at rest
- Variability of the mean heart rate
- Patient activity
- Thoracic Impedance

Activating HF monitor statistics

For more information see: Setting diagnostic functions [Page 155]

Displaying HF monitor statistics

Note the following details of the HF monitor statistics:

Mean heart rate

The mean heart rate per day is specified as follows:

- Display of the mean heart rate at rest per day in bpm.
- Recording as a long-term trend for a maximum of 240 days, each consisting of 24 hours, with a resolution of 1 bpm within a recording range of 30-250 bpm. The trend is then updated, beginning with the oldest value.
- Recording of Vs, Vp and Vrs (ventricular event sensed in the refractory period).
- Ventricular heart rate at rest

The ventricular heart rate at rest is recorded for the duration of the set resting period and indicated as follows:

- Display of the mean ventricular heart rate at rest in bpm. Mean values are calculated by dividing the set resting period into 10-minute intervals.
 The minimum averaged value of the 10-minute intervals per day is shown.
- Recording as a long-term trend for a maximum of 240 days, with a resolution of 1 bpm in a recording range of 30-250 bpm; after that, the trend is updated beginning with the oldest value.
- Recording of Vs, Vp and Vrs (ventricular event sensed in the refractory period).
- For each separate trend the display shows the mean values on all days for which valid values are present.
- Variability of the mean heart rate

The variability of the heart rate is recorded in bpm according to the SDANN algorithm, as a long-term trend for up to 240 days with a resolution of one day.

The corresponding heart rate is measured in the atrium (multi-chamber devices and DX).

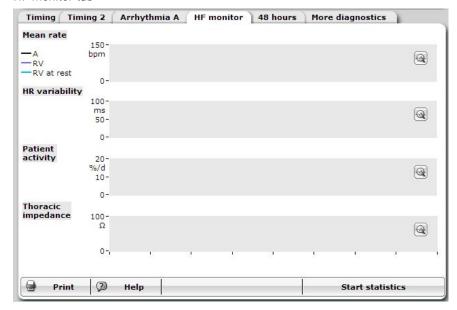
Patient activity

Patient activity is measured as the time during which the device's motion sensor delivers a rate higher than the device's basic rate. The resolution for patient activity is 2 s. The data is converted into % per day. For example, 2.4 h of patient activity are indicated as 10%/day in the trend.

- There has been activity wherever the current sensor signals are greater than or equal to the sensor threshold.
- A daily value of 0%/day means that no patient activity was detected. 24 h
 means that the device detected activity continuously throughout the day.
- Thoracic Impedance
 - The thoracic impedance measurements are displayed as a thoracic impedance trend and can thus be evaluated diagnostically on the programmer.

User interface

HF monitor tab



Statistics for the last 48 hours

Navigation: Diagnostics ightarrow 48 hours

Objective

These statistics provide important data recorded in the last 48 hours.

This makes it possible evaluate a summary of important data from the individual statistics (timing, atrial arrhythmia) at a glance.

The following statistics are displayed in the form of short-term trends:

- Rate trend (see also: $Diagnostics \rightarrow Timing$)
- Atrial burden (see also: **Diagnostics** → **Arrhythmia A**)
- Percentage of pacing (see also: $Diagnostics \rightarrow Timing$)

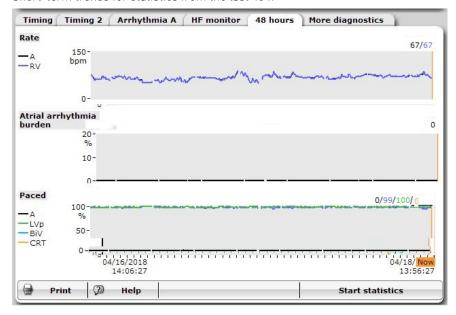
Note

The short-term trends continuously store the data from the last 48 hours. The oldest data is then overwritten.

The parameters are recorded every 10 minutes.

User interface

Short-term trends for statistics from the last 48 h



Displaying other statistics

Navigation: Diagnostics \rightarrow More diagnostics

Overview

The following statistics are displayed with histograms and trends in the Statistics group box:

- Event counters:
 - As, As (PVARP), Ars, Ap
 - RVs, RVrs, RVp, VES
 - LVs, LVrs, LVp
- Pulse amplitudes with threshold trends (A, RV, LV, LV2)
- Rate trend with percentages of pacing sensing A, RV; pacing: A, LV, BiV, CRT
- Sensor rate: percentage
- PVC/h: long-term trend
- Short intervals/nsT counter:
 - Counter of short intervals
 - nsT counter
 - The development of both counters is shown as a trend graph.

- LV-RV event sequences
 - Biventricular pacing
 - RVp without LVp: RVp events where the LV-T wave protection function (i.e., left ventricular sensing) prevents the delivery of a triggered LV pace.
 - RVs triggered LVp
 - RVs without LVp: RVs events where the LV-T wave protection function (i.e., left ventricular sensing) prevents the delivery of a triggered LV pace.
 - LVp exclusive (LV-only configuration): left ventricular paced events when the ventricular pacing mode is set to left-ventricular only pacing.
 - LVp exclusive inhibited (LV T-wave protection): LVp events inhibited due to LV T-wave protection when the ventricular pacing mode is set to leftventricular only pacing.
 - PVC triggered LVp
 - PVC without LVp: PVC events where the LV T-wave protection function (i.e., left ventricular sensing) prevents the delivery of a triggered LV pace.
- Extended RV lead measurement: The extended RV lead measurement allows
 a detailed assessment of the status of the entire RV lead. This is based on the
 periodic impedance measurement of all conductors, for which a daily mean
 value of 24 stored measured values is displayed,

The measurement paths in detail:

- RV coil => can
- RV coil => RV tip
- RV ring => can
- RV ring => RV tip
- SVC coil => can
- SVC coil => RV coil
- The zero line represents a 16-day mean value from the previous measurements as a reference, so that the daily relative deviations of the impedances from the reference value can be easily identified.
- In addition, the measured values of the shock impedances are displayed:
 RV => can (RV coil => can)/RV => SVC (RV coil => SVC coil)
- CRT AutoAdapt

The recordings are used to assess the efficacy of the automatically set CRT pacing parameters.

- Ventricular pacing status: LV adaptive; BiV programmed; BiV adaptive
- Adaptive AV delay: After pacing; After sensing

Sensor statistics, details

The recording of the sensor rate does not depend on whether the respective pacing rate was active or whether pacing did not occur due to intrinsic events.

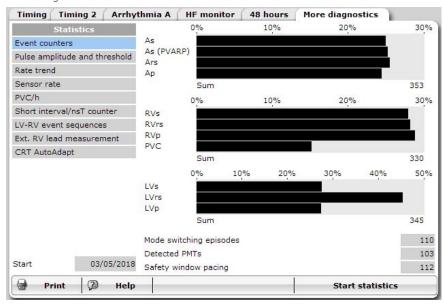
The sensor rate thus also shows how the device would have paced had pacing not been inhibited.

- The frequency with which the sensor rate occurs in certain rate ranges is recorded. The rate range between < 40 and > 180 bpm is subdivided into 16 equidistant rate classes.
- The graph shows the percentages of the individual classes in the form of a bar chart as well as the total number of events.

Note

The sensor histogram is displayed whether or not a rate-adaptive pacing mode has been set.

User interface More diagnostics tab



2.8 System Functions

Overview

The tab with the name of the interrogated implanted device contains the specific default settings and functions for the relevant device:

- Synchronizing system times
- Reading ICD data
- Turning on wandless telemetry
- Measuring the battery voltage
- Firmware version
- Connection type of the header: DF-1 or DF4

System Functions

Tab with Device Name

Navigation: More \rightarrow [Name of the device]

Synchronizing the time

Where necessary, synchronize the system time for the implanted device with the time as set in the programmer.

Wandless telemetry reduces the service time of the device

Wandless telemetry impacts battery longevity of the device, in comparison to PGH telemetry.

- Do not establish unnecessary wandless telemetry.
- Check the battery capacity of the device at regular intervals.

Selecting RF or PGH telemetry

- Always apply the programming head before setting the telemetry type.
- The selected telemetry type becomes active after two seconds.

★ WARNING

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH: Raise the programming head by at least 30 cm; the device will switch automatically to the permanent program.
- In the case of wandless telemetry: Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

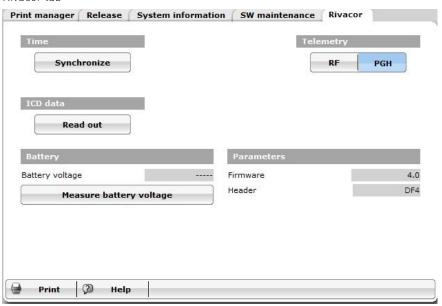
Reading ICD data (memory dump)

- Transfer the entire contents of the data storage of the device to the programmer for analysis.
- The data are saved on the programmer. From there they can be transferred onto an external storage medium (USB stick).
- The saved data can only be evaluated by BIOTRONIK employees.

System Functions

User interface: example

Rivacor tab



Measuring the battery voltage

Note

After shock delivery or capacitor reforming the battery will need some time (battery recovery time) to develop a new residual voltage. This process will modify the measured value.

For this reason, battery voltage should be measured only at least 24 hours after the last shock delivery or capacitor reforming. Check the entries in: Recordings → Shocks.

Printing

By pressing [Print] you will obtain the following printed information:

- Battery voltage
- Battery ID
- Details on the Parameters group box

2.9 Follow-Up

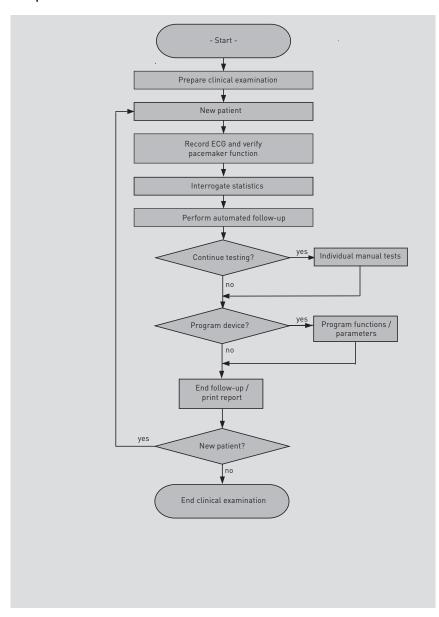
Preparing for Follow-Up	207
Follow-Up Assistant	214
Performing Manual Follow-Up	223

Preparing for Follow-Up

Performing a patient follow-up	207
Setting a follow-up sequence	210
Function of the tests	211
Configuring default parameters for tests	211
Function of the adjustable parameters	212

Performing a patient follow-up

Recommended sequence for follow-up



Overview

Recommended sequence of steps for patient follow-up:

Sequence	Description
1	Interrogate the device.
2	Record and evaluate the ECG.
3	Check the pacing function of the device.
4	 Evaluate the status of the device and the Follow-up window. As needed: Evaluate diagnostics. Evaluate recordings and episodes.
5	Automatically perform standard tests or alternatively: initiate all the follow-up tests manually.
6	Customize the program functions and parameters (depending on the follow-up results).
7	Transmit the permanent program to the device.
8	Print (print report) and document follow-up data.
9	Finish the follow-up for this patient.

Interrogating the device

Proceed as follows:

- 1. Place the programming head of the programmer directly above the patient's device and establish RF or PGH telemetry. When using RF telemetry, you can remove the programming head after two seconds.
- 2. Make sure that telemetry contact with the device has been established. When telemetry contact has been established, the following processes are performed automatically:
 - Identification of the device
 - Interrogating the current (permanent) device program
 - Transmitting all data stored in the device to the programmer

Recording and evaluating the ECG

Proceed as follows:

- Connect the patient to the ECG cables in the usual manner. As an alternative, you can also use the far-field ECG function, in which the ECG is acquired wirelessly between the shock coil and housing.
- 2. Record the ECG and print it as needed.
- 3. Evaluate the ECG.

Checking the pacing function of the device

Proceed as follows:

1. Check the pacing function of the device.

Checking the device

After transmission of the device data, the Follow-up window is displayed on the programmer. Proceed as follows:

- 1. The events that occurred are displayed in a list with the statistics symbol on the Follow-up page in the Episodes group box.
- 2. Select the event by clicking on it. Then the statistics class, to which the displayed event belongs, is displayed. The statistics contain detailed information on the corresponding results.

Starting follow-up tests automatically

Follow-up tests can be started automatically (by selecting the [Repeat all tests] button). The follow-up tests selected in the follow-up preferences are highlighted. Proceed as follows:

- 1. Start the tests. The sequence of the tests depends on the options offered by the device: either completely automated running in the background or partially automated as a follow-up assistant.
 - The values measured in the individual tests are displayed in the Test results group box.
- 2. Print the contents of the Follow-up window.

Running follow-up tests manually

In addition to the standard tests that are automatically started, all follow-up tests can also be executed manually. Proceed as follows:

- Select one of the tests for follow-up, start the tests, and perform the measurements
- 2. As needed, select other tests and functions.
- 3. Evaluate the tests.

Adapting the program parameters

If the tests and measurements indicate the need to adjust program functions and parameter values, then it is necessary to change the current program and transmit it to the device. Proceed as follows:

- 1. Change the necessary parameter values and activate or deactivate the relevant program functions.
- 2. Transmit the new program to the device so that your chosen settings can take effect. This can also be done temporarily for test purposes.
- 3. Transmit the new program as a permanent program to the device by selecting [Send]. Successful transmission is confirmed by a message.

Printing follow-up data

Proceed as follows:

- 1. Select [More]. The Print manager window opens.
- 2. Print the report of the entire follow-up.

Completing the follow-up

Proceed as follows:

- 1. Stop the follow-up session and RF telemetry by clicking on [End].
- 2. The patient may now leave the follow-up session.
- Interrogate the device of your next patient.
 The follow-up for the next patient is ready.
- 4. Proceed in the same manner as described above.

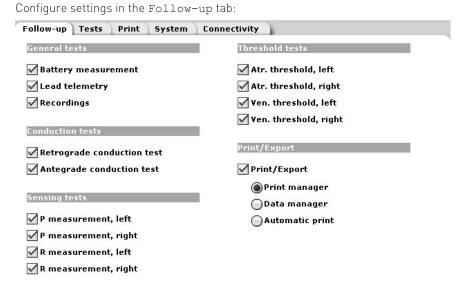
Setting a follow-up sequence

Navigation Preferences \rightarrow Follow-up

Objective Defining defau

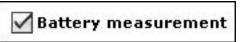
Defining default settings for the follow-up sequence helps simplify implementation and supports the customer-specific process. This is possible because the customer-specific settings take effect immediately when performing the different follow-up tests and functions. This eliminates the need to configure the individual tests separately in each follow-up.

User interface Configure settings in the F



Setting the sequence

The respective check boxes are used to configure which measurements and tests are performed automatically during follow-up:



The respective radio buttons are used to configure how the follow-up results are automatically output.



Note

The selected option for issuing follow-up results only works if Print/Export is selected.

Information pertaining to the respective function of the tests

Function of the adjustable parameters [Page 212]

Function of the tests

Function of the tests

The tests have the following functions:

Test	Function
Battery measurement	Measures the remaining voltage of the device battery
Lead telemetry	Measures impedance to assess lead integrity
Recordings	Read recorded data
Retrograde test	Measures the duration of the stimulus conduction from ventricle > atrium
Antegrade test	Measures the duration of the stimulus conduction from atrium > ventricle
P measurement, left	Measures sensing in left atrium
P measurement, right	Measures sensing in right atrium
R measurement, left	Measures sensing in left ventricle
R measurement, right	Measures sensing in right ventricle
Atr. pacing threshold, left	Measures pacing threshold in left atrium
Atr. pacing threshold, right	Measures pacing threshold in right atrium
Ven. pacing threshold, left	Measures pacing threshold in left ventricle
Ven. pacing threshold, right	Measures pacing threshold in right ventricle

Function of the adjustable parameters [Page 212]

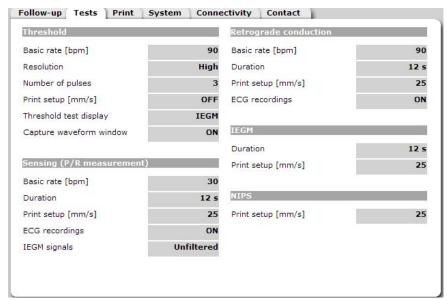
Configuring default parameters for tests

 $\mathsf{Preferences} \to \mathsf{Tests}$

Objective To simplify follow-ups using system default settings.

User interface

The Tests tab:



Sequence

Set

Sequence	Description
1	Select parameter
2	Select value from window

The selected value is immediately applied and is set as the default setting for the next system startup.

Further details

Information about the parameters in detail: Function of the adjustable parameters [Page 212]

Function of the adjustable parameters

Function of the parameters

Parameter	Function
Basic rate	The rate at which the device delivers pulses in the absence of sensed intrinsic events or if the sensing function is deactivated. To run the test effectively, the pacing rate of the threshold test must be higher than the patient's intrinsic rhythm.
Resolution	Range of values: Low, Medium, High.
Number of pulses	The parameter determines the number of test pulses triggered. When activated, this function ensures that the patient will remain without pacing for no longer than the set number of test pulses after falling below the pacing threshold. After each of the programmed number of test pulses, the device automatically returns to a safe start amplitude.

Parameter	Function
Report	The parameter controls automatic printing of ECG and IEGM as well as the paper speed while performing the respective tests.
Display threshold test	Displays the ECG or IEGM.
Display threshold test	Show or hide zoom sections for test pulses in the ECG window.
Duration	Period in which certain implanted devices use IEGM for measurement.
ECG recordings	It is possible to record the last 60 seconds of the ongoing IEGM, save it as a file and then archive it using the Freeze function. Markers and surface ECGs are also stored together with the IEGM.
IEGM signals	Range of values: Filtered, Unfiltered.

Follow-Up Assistant

Objective	214
Follow-Up Window	214
Legend for the Follow-Up Window	215
Display Events	215
Meaning of Event Messages	216
Trends: Pacing Thresholds, P and R Wave Amplitudes – Details	218
Archiving Follow-Up Results	218
Evaluate Trends in Measured Values	219
Impedance Trends – Details	220
Details of Diagnostics	221

Objective

The follow-up assistant helps the user to conduct follow-ups effectively. The system can execute the following actions from the dialog:

- Provide an overview of patient and device status
- Display episodes and events from previous follow-up periods and open the relevant linked window by clicking
- Display test results and trends
- Display important diagnostic information and details
- Start tests
- Navigate to the MRI program
- Print a follow-up report

Follow-Up Window

Navigation: Follow-up

Objective

The most important interrogated data and measured values are summarized in groups in the Follow-up window.

Abbreviations and symbols

See Legend for the Follow-Up Window [Page 215]

Prerequisites Note

The following requirements must be met for an automatic follow-up:

- Telemetry contact between the device and programmer must be established.
- The programmer indicates successful device interrogation by displaying the message: Interrogation was successful.
- Ensure that there is enough printer paper in the paper tray of the programmer (if you want to use the programmer's internal printer).

The pacing threshold test is automatically performed at a specific time of day if capture control has been activated.

Repeat all tests You can repeat the follow-up test sequence at any time, for example, if measured

values do not appear plausible: Select [Repeat all tests].

Start up tests individually You can start up tests individually by clicking on the appropriate measured value.

The system then switches to the tab for the relevant test: Select [Start] from

there.

Test results: trends See Evaluate Trends in Measured Values [Page 219]

Diagnostics: details See Details of Diagnostics [Page 221]

Legend for the Follow-Up Window

Navigation: Follow-up

Battery charging status The various abbreviations mean the following:

Abbrevia- tion	Meaning
BOS	Beginning of Service: • > 90% charge
ERI	Elective Replacement Indication (i.e., RRT: Recommended Replacement Time): • Indicates that the device must be replaced
EOS	End of Service: • Service life of the device has ended

★ WARNING

Battery charging status = EOS: patient not being treated

If the battery status is EOS (end of service), the active device is out of service and cannot provide any therapy.

• Replace the device immediately.

Symbols The symbol has the following meaning:

Symbol	Meaning
\$	Values have been automatically measured and updated in the last 24 hours.

Display Events

Navigation: Follow-up

Display The Follow-up window shows the events that have been saved in the device since the last follow-up.

Detail of user interface

Episodes

New episodes VF/VT/others

11/----/----

Display event details Click on the event being displayed to review its details.

Event messages See Meaning of Event Messages [Page 216]

Meaning of Event Messages

Navigation: Follow-up

⚠ WARNING

Battery charging status = EOS: patient not being treated

If the battery status is EOS (end of service), the active device is out of service and cannot provide any therapy.

Replace the device immediately.

Event messages

Note

The following table shows all possible event messages and explains their meaning. The precise messages shown will depend on the device type.

Priori- ty	Event text	Meaning
1	EOS occurred	End of Service Service life of the device has ended
2	Device error	Error of the device has occurred. Contact BIOTRONIK.
3	Elev. power consumpt. Code %d	Elevated power consumption has occurred. It is recommended to contact BIOTRONIK. The indicated numerical code can help in the analysis. Check impedances and leads.
4	Shocks in backup mode	Backup mode is operated with a restriction in the VF zone of 171 bpm, or 350 ms, which may under some circumstances deviate from the originally programmed restriction in the zone.

Priori- ty	Event text	Meaning
5	Low shock impedance detected. Shock path integrity can no longer be guaranteed. Please contact BIOTRONIK.	Low shock impedance was detected. The integrity (reliability) of the shock path can no longer be ensured. Contact BIOTRONIK.
6	Check shock impedance	Critical concern regarding measured shock impedance. Check the lead and modify if necessary.
7	Check pacing imped- ance	Critical concern regarding measured pacing impedance. Check the lead(s) and revise if necessary.
8	ERI occurred	Elective Replacement Indication Indicates device must be replaced
9	Very low RV sense amplitudes	Critical concern regarding signal amplitude. Check the leads and reposition if necessary.
10	Ineffective max. energy shock	Maximum energy shock had no effect. Check DFT.
11	Episode with multiple shocks	Critical episode. Check recordings and modify programming if necessary.
12	Ven. episode with ven. acceleration	Critical episode. Check recordings and modify programming if necessary.
13	All ATPs in VT1 disabled by ATP opti- mization All ATPs in VT2 disabled by ATP opti- mization	All ATP therapies in the indicated VT zones have been blocked by activated ATP optimization due to heart rhythm acceleration. Check ATP statistics.
14	Ven. episode with atr. acceleration	Critical episode. Check recordings and modify programming if necessary.
15	Ven. episode (> 1 min)	Ventricular episode lasted longer than 1 minute.
16	Ven. episode (> 3 in 24 h)	More than three ventricular episodes occurred within 24 h.

Priori- ty	Event text	Meaning
17	Atr. therapies blocked due to VT/VF	An atrial therapy may have increased the ventricular rate in a VT or VF zone. AT therapies have then been deactivated. During follow-up: Decide on the reactivation of AT therapies.
18	SVT episode (> 10 min)	Supraventricular episode lasted longer than 10 minutes.
19	Atr. therapies blocked due to Afib > 48h	Atrial fibrillation took longer than 48 h and increased the risk of cerebrovascular stroke significantly. AT therapies have then been deactivated. During follow-up: Decide on the reactivation of AT therapies.
20	> 48 h Afib since start of statistics	Sustained atrial episode > 48 h detected since start of statistics.
21	Shipment mode active	The manufacturer has set the device to shipment mode to conserve energy. Deactivate shipment mode before completing the implantation procedure.

Trends: Pacing Thresholds, P and R Wave Amplitudes - Details

Navigation: Follow-up \rightarrow TrendView

Pacing threshold trends

Enable the function for recording threshold trends here:

• Parameters \rightarrow Bradycardia/CRT \rightarrow Capture control \rightarrow ON or \rightarrow ATM (monitoring only).

Trends in P and R wave amplitudes

Note

If no value can be obtained, for example, due to permanent pacing, then no value is entered for that day.

- All trends record amplitudes from 0.2 to 20 mV.
- The P and R wave amplitudes are only displayed in the trend if sensing has been switched on for the relevant channel.

Archiving Follow-Up Results

Navigation: Follow-up ightarrow Last follow-up

Objective

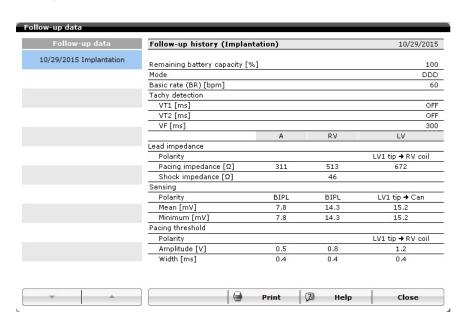
The archive offers you a structured overview of the chronological development of lead measurement values and the left ventricular polarity set for triple-chamber devices since implantation.

In addition, the data is shown for:

- Remaining battery capacity
- Pacing modes
- Basic rate

- Arrhythmia zones
- The values determined upon implantation and the 11 subsequent follow-ups are displayed.
- When 11 follow-ups have been recorded, the system overwrites the oldest record beginning with the first follow-up. However, the data set recorded at implantation remains saved.

User interface



Evaluate Trends in Measured Values

Navigation: Follow-up \rightarrow Trends

Display trends

The Trends function provides you with a structured overview of important measured values, which are displayed as graphic trends since the last follow-up.

- Pacing thresholds
- P/R amplitudes
- Pacing impedance in the atrium and ventricle
- P/R amplitudes

You can use the Trends function to navigate and to take a focused look at particular individual events.

Events from the event list are displayed directly beneath the auxiliary line in the **[Trends]** window with a comment and the date.

- Data for trends are saved continuously. Trends are not deleted after followup. The oldest recordings are overwritten after 240 days.
 - If required, initialize the restart for long-term trends here: ${f Diagnostics}
 ightarrow {f Start statistics}.$

Events icons

The icons have the following meanings:

Icon	Meaning
•	Event with details on data, time, and type
	Event plus icon;
800/ 858	Display details: click on the area shown in color
01.06.2008 MS-Holter	

Arrow keys for navigation

The arrow keys have the following functions:

Icon	Functions
0 0	Arrow keys with event icon: navigate to the left or right to the next event
4 >	Simple arrow keys: move the cursor to the right or left from one day to the next one

Zoom function in TrendView

The magnifying glass has the following function:

Icon	Functions
Q	The magnifying glass symbol above the curve of the individual trend histogram calls the individual window of the trend histogram and magnifies the display. This makes the data more visible in detail.

Related topics

See Impedance Trends – Details [Page 220]

See Trends: Pacing Thresholds, P and R Wave Amplitudes – Details [Page 218]

Impedance Trends - Details

Navigation: Follow-up \rightarrow TrendView

Time window and resolution

The following trends are displayed for up to 240 days with a preset resolution of 24 $\,\mathrm{h}$:

- Atrial impedance trend
- Right ventricular impedance trend
- Left ventricular impedance trend
- Shock impedance trend

Details

- Pacing and shock impedances are measured every 112 seconds. The measurement cannot be switched off.
- A mean value is calculated and stored from these measured values every hour.
- The displayed daily value is the mean value of 24 stored measured values.
 This daily value is used for illustration in Follow-up → TrendView and
 Diagnostics → More diagnostics → Ext. RV lead measurement.
- Shock impedance measurements are always carried out below the threshold.
- Measurement ranges:
 - Sensing/pacing RA/RV/LV: 200 3000 Ω
 - Shock path: $25 150 \Omega$
- If a measurement result is outside the measurement range, additional tests are carried out for this range:
 - Measurement path bipolar: If 2 out of 3 measurements are outside the measurement range, the impedance measurement is switched off.
 - Measurement path unipolar, advanced bipolar (combinations with the RV coil) and shock path: If the measurement is outside the measurement range, the impedance measurement is repeated after 1.5 hours. If 2 out of 3 measurements are outside the measurement range, the impedance measurement is switched off.
- Recording is interrupted briefly 2 minutes before the following time:
 - Message transmission for Home Monitoring
- The data is sent daily to the Home Monitoring Service Center if Home Monitoring is enabled.

Details of Diagnostics

Navigation: Follow-up ightarrow Diagnostics ightarrow Details

Objective

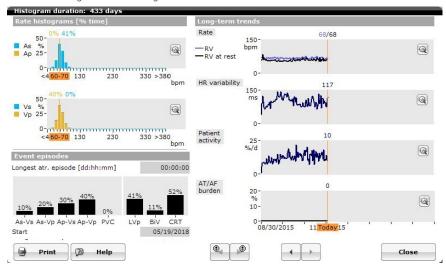
In the Follow-up window in the Diagnostics group box you can display selected statistical data for diagnostic purposes all together in a single window. Here, you can evaluate the most important data from the individual statistics at a glance.

Note

The long-term trends store the data continuously. This is unlike all other statistics histograms, which are re-initialised each time the device is interrogated.

User interface

Details of diagnostics; histograms and trends



Zoom function in diagrams

The magnifying glass has the following function:

Icon	Functions
(a)	The magnifying glass symbol in the diagrams calls the individual window of the diagram and magnifies the display. This makes the data more visible in detail.

Display details

In the Follow-up window in the Diagnostics group box, select: [Details].

Performing Manual Follow-Up

Test functions at a glance	223
Impedance Test	225
Sensing Test	227
Threshold Test	228
Determining the Defibrillation Threshold (DFT Test)	231
AV Opt Test	237
LV VectorOpt	239
NIPS – Non-Invasive Programmed Stimulation	241
Retrograde Conduction Test	246

Test functions at a glance

Electrophysiological tests

You can use the electrophysiological tests to determine and test effective detection and therapy parameters.

During the course of the various tests, the intrinsic events of the patient and the detection of the ICD can be monitored continually via IEGM and marker texts.

Impedance test of pacing

The pacing impedance measurement is used to determine the electrical resistance of the lead system. This value serves to check the condition (e.g., in case of lead fracture) and position of the lead for effective pacing.

Automatic:

- Pacing impedances are measured every 112 s. The measurement cannot be switched off.
- A mean value is calculated and stored from these measured values every
 hour.
- The displayed daily value is the mean value of 24 stored measured values. This daily value is used for illustration in Follow-up → TrendView.
- Measurement ranges:
 - Sensing/pacing RA/RV/LV: 200 3000 Ω

Manual:

The pacing impedance can also be measured manually in each follow-up using the programmer's test function. The programmer shows the current measured value of the last measurement cycle in each case.

Sensing test

The sensing test determines the current P and R amplitudes of the intrinsic events in all active channels. This lead position information provides the requirements for further tests.

Automatic:

The device automatically measures the P and R amplitudes in each active channel (A, RV, LV).

Valid results of automatic measurement of unfiltered amplitudes (P wave: 0.5 to 8 mV; R amplitude: 2 to 20 mV) are presented in the sensing statistics and transmitted via Home Monitoring. In the case of invalid measurement values, an event is sent during daily message transmission via Home Monitoring. In biventricular and left ventricular mode, the right ventricular sensed events are not triggered. This allows only intrinsic events to be considered for the sensing test.

Manual:

P/R amplitudes can also be measured manually in each follow-up using the programmer's test function. 6 sensed events are evaluated in the manual and automatic sensing test. The display is updated with every new measured value. The programmer indicates if no sensed events occur.

Threshold test

The threshold test determines the lowest pacing energy needed to pace the heart in all active channels. In the course of the threshold test, the pulse amplitude is reduced until a stimulus no longer triggers a response from the heart. The lowest value tested that effectively paces is the threshold. Low values for the pulse amplitudes increase the device's service time.

DFT test

The defibrillation threshold is the least required shock energy to successfully terminate a tachyarrhythmia.

The DFT test is used to determine the patient's defibrillation threshold.

During the DFT test, a temporary program is started for VF therapy that can be configured with different detection and therapy parameters than the permanent program.

Programmed bursts or T wave synchronized shocks are delivered for inducing VT or VF. These are then treated via manually or automatically delivered therapies (ATP or shock). If necessary, you can specifically deliver an emergency shock at maximum energy.

Painless shock impedance test

Measurement of shock impedance determines the electrical resistance between the shock coil and housing. This value serves to check the condition (e.g., in case of lead fracture) of the lead for effective shock therapy.

Automatic painless shock impedance measurement:

- Shock impedances are measured every 112 s. The measurement cannot be disabled
- A mean value is calculated and stored hourly from these measured values.
- The displayed daily value is the mean value of 24 stored measured values.
 This daily value is used for illustration in Follow-up → TrendView and
 Diagnostics → More diagnostics → Ext. RV lead measurement.
- The shock impedance measurement is carried out below the threshold.
- Measurement ranges:
 - Shock path: 25 $150~\Omega$

Manual:

Shock impedance can also be measured manually in each follow-up using the programmer's test function. The programmer shows the current measured value of the last measurement cycle in each case.

AV Opt Test

This test is helpful for optimizing the AV delay. Optimized AV delays are determined on the basis of P-wave measurements. These values are displayed for pacing and sensing and can be applied directly to the Dynamic AV delay parameter.

LV VectorOpt

It is possible to test LV polarities and their parameters in the LV $\mbox{VectorOpt}$ tab, and to transfer these settings directly into the permanent program.

Test of retrograde conduction times

Determining and evaluating retrograde conduction times forms a foundation for setting timing parameters that affect sensing and pacing between the right atrium and the right ventricle as well as between the right and left ventricle. Change the timing parameters in order to prevent pacemaker-mediated tachychardias and to optimize patient hemodynamics.

Impedance Test

Objective

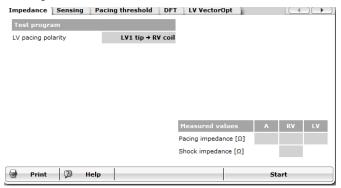
- The impedance test measures the following conductor resistances of the implanted leads:
 - Pacing impedance
 - Shock impedance
- The measured values serve to check the leads (for example, in case of lead fracture) and to evaluate the lead position.

Automatic impedance measurement

- Pacing and shock impedances are measured every 112 seconds. The measurement cannot be switched off.
- A mean value is calculated and stored from these measured values every hour.
- The displayed daily value is the mean value of 24 stored measured values.
 This daily value is used for illustration in Follow-up → TrendView and
 Diagnostics → More diagnostics → Ext. RV lead measurement.
- Shock impedance measurements are always carried out below the threshold.
- Measurement ranges:
 - Sensing/pacing RA/RV/LV: 200 3000 Ω
 - Shock path: 25 150 Ω
- If a measurement result is outside the measurement range, additional tests are carried out for this range:
 - Measurement path bipolar: If 2 out of 3 measurements are outside the measurement range, the impedance measurement is switched off.
 - Measurement path unipolar, advanced bipolar (combinations with the RV coil) and shock path: If the measurement is outside the measurement range, the impedance measurement is repeated after 1.5 hours. If 2 out of 3 measurements are outside the measurement range, the impedance measurement is switched off.
- Recording is interrupted briefly 2 minutes before the following time:
 - Message transmission for Home Monitoring
- The data is sent daily to the Home Monitoring Service Center if Home Monitoring is enabled.

User interface

The Impedance tab



Measuring impedance

Navigation: Tests \rightarrow Impedance



Unfavorable lead position: limited sensing and pacing performance

Inappropriate lead position in the heart impairs the lead properties and restricts sensing and pacing.

Measure the impedance of the leads to evaluate their position and, if necessary, to contribute to appropriate functionality by repositioning.

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH: Raise the programming head by at least 30 cm; the device will switch automatically to the permanent program.
- In the case of wandless telemetry: Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

Measuring impedances

1. Evaluate the default parameter values for the test program and adjust them if necessary.

Select [Start].

The following processing actions are executed by the system:

- Measuring shock impedance
- Measuring pacing impedance
- Displaying measured values

Evaluate the results and reposition the leads if necessary.

Sensing Test

Performing the sensing test

Navigation: Tests \rightarrow Sensing

Objective

The sensing test has the following clinical benefits:

- Evaluation of the position of the leads
- Check of prerequisites for additional electrophysiological tests
- Determination of optimal sensitivity for the device

↑ WARNING

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH:
 Raise the programming head by at least 30 cm; the device will switch
 automatically to the permanent program.
- In the case of wandless telemetry:

 Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

Performing the sensing test

To perform the sensing test, proceed as follows:

Step	Action	Remark
1	Evaluate the default parameter values for the test program and adjust them if necessary.	
2	Select Basic rate and reduce the basic rate to a value less than the intrinsic rhythm.	 Display of measured values: Current measured value: to the right of the IEGM Mean measured values: in the Measured values group box
3	Evaluate the mean measured values.	Optimization options: Reposition the leads. Change the parameter values.

When the test is completed, the permanent program is automatically reactivated.

Performing the intrinsic rhythm test

Step	Action	Remark
1	Select [Intrinsic rhythm] and hold down the button.	 The intrinsic rhythm test starts: Backup pacing is deactivated. The P and R amplitudes are measured and displayed.
2	End the intrinsic rhythm test by releasing the [Intrinsic rhythm] button.	The permanent program is active again.

Details

Sensing test - details [Page 228]

Sensing test - details

Navigation: Tests \rightarrow Sensing

Measurement of P/R amplitudes

During manual sensing tests, an evaluation is made either once for each channel for 5 seconds or for a maximum of 6 detected events. The display is updated with every new measured value. In manual sensing tests, if no sensed event occurs then the programmer will show a corresponding message.

Results

Depending on the test mode and the set parameters, the sensing test provides the following results:

- Display of minimum, mean and maximum signal amplitudes of the P/R waves in every chamber
- Display of mean rate if atrial sensed events occur

Threshold Test

Performing the threshold test

Navigation: Tests \rightarrow Pacing threshold

Objective

The threshold test determines the lowest value of pacing energy needed to pace the heart. Low values for pulse width and pulse amplitudes increase the service time of the device.

In the course of the threshold test, the pulse amplitude is reduced until a stimulus no longer triggers a response from the heart. The last value that effectively paced is the threshold.



Low pulse amplitude and pulse width: loss of capture

Pulse amplitude and pulse width that are too low for the patient's pacing threshold can prevent effective pacing.

The pacing threshold can also change over time, so that a pulse amplitude and pulse width that was previously effective can become too low.

Measure the pacing threshold during implantation and follow-ups and always allow for adequate safety margin when programming the pulse amplitude and pulse width.

WARNING

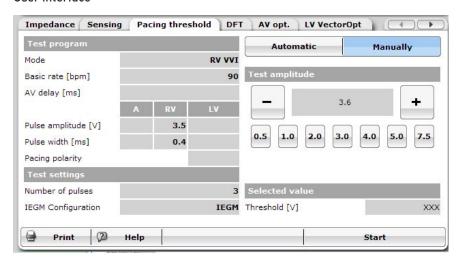
Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH: Raise the programming head by at least 30 cm; the device will switch automatically to the permanent program.
- In the case of wandless telemetry: Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

User interface



Performing the threshold test

If you want to conduct the threshold test with default settings or adjusted parameters of the Test program group box, proceed as follows:

- 1. Evaluate the default parameter values for the test program and adjust them if necessary.
- 2. Select [Start].
- During the test, observe the ECG monitor to obtain the pacing threshold and to modify the test amplitude if a particular pacing pulse is no longer effective.
- 4. To end the test, press the following button: [Stop]
- 5. Accept the measured pacing threshold by selecting the value in the Threshold window.

Select derivation

Note

Set the derivation for the test signal required specifically in each case by selecting **[ECG]**, **[IEGM]**, and **[FF]** for far-field ECG (leadless ECG).

Navigation: Tests \rightarrow Pacing threshold \rightarrow Test settings \rightarrow IEGM Configuration

Select test amplitude

Choose from the following options:

Select a test amplitude from the table	The selected test amplitude will be applied.
Increase or reduce test amplitude	 Choose from the following options: Either select the desired test amplitude from the table. Or select [+] or [-].
	As long as the test pulses are active, capture waveform windows are displayed under the ECG for the test pulses. See also: Show and hide capture waveform windows [Page 230]

Show and hide capture waveform windows

In the ECG window, capture waveform windows show extracts from the ECG for the test pulses. From here you can show or hide these windows permanently:

 ${\sf Preferences} \to {\sf Tests} \to {\sf Capture\ waveform\ window}.$

Evaluating and adopting the results

Accept the threshold value in the Threshold window. You can print out the results if required.

Adjusting the permanent program

Adjust the permanent program if required: Parameters \rightarrow Bradycardia/CRT and transfer the settings to the device with [Program].

Threshold test - parameters

Navigation: Tests \rightarrow Pacing threshold

Setting the parameters of the test program

In most cases, the factory settings of the test program are suitable for the threshold test. You can change the parameters if necessary.

Meaning of parameters

The meaning of selected parameters:

Parameter	Meaning
[Automatic] or [Manual]	Threshold test will be performed automatically or manually.
Number of pulses	 After each of the programmed number of test pulses, the pacemaker automatically returns to a safe start amplitude. Where the threshold is not reached, the patient is left without effective pacing for the set number of test pulses at most. When the (∞) function is activated, the set test pulse remains active until the next value is set or the threshold test is completed.
[ECG] (with capture waveform window = ON)*	Conventional Einthoven-based ECG
[IEGM] (with capture waveform window = ON)*	Intracardiac electrogram
[FF] (with capture waveform window = 0N)*	Far-field ECG: wireless far-field derivation between distal shock coil and housing; for left-side implantation of the device this corresponds to Einthoven's Derivation III

^{*} Capture waveform window, see: Show and hide capture waveform windows [Page 230]

Determining the Defibrillation Threshold (DFT Test)

Definition

The defibrillation threshold is the lowest required energy to successfully terminate a tachyarrhythmia.

Objective

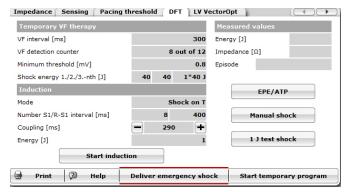
You can obtain the defibrillation threshold with the help of the DFT (defibrillation threshold) test.

The results of the DFT test can be used to program the ICD so that it can usually terminate VT/VF episodes requiring therapy with the first shock and with optimal energy utilization.

In addition to this, it is possible to conduct electrophysiological examinations (EP studies)

User interface

The DFT tab



Preparation of the DFT test

Evaluating the system integrity of the shock coil

The painless shock impedance measurement is available as an alternative to the 1 J test shock.

Select $\mathsf{Tests} \to \mathsf{Impedance} \to \mathsf{Start}$, to perform the measurement. The measured values for shock impedance and pacing impedance are displayed in the Measured values group box.

VT/VF induction

Navigation: Tests ightarrow DFT ightarrow Induction

Objective

A VF is induced for the DFT test in order to test the effectiveness of therapy parameters for detection and termination of tachyarrhythmias.

Mode

The following modes are available for VF induction:

Induction modes	Description
HF burst	Burst with high rate
Shock on T	Shock at the end of a burst, synchronized with a T-wave

HF burst

The following parameters are available for the HF burst:

Parameter	Description
Duration	HF burst duration Alter the duration of the HF burst interactively: To extend it: hold down the [Deliver HF burst] button Complete the change: release the [Deliver HF burst] button
Rate	HF burst rate

Shock on T

The following parameters are available for the shock on T:

Parameter	Description
Number S1	Number of S1 stimuli for the burst
R-S1 interval	Start interval with which the system couples the burst to the R-wave
Coupling	Interval with which the system couples the shock on T without confirmation to the last S1 stimulus of the burst
Energy	Total energy that the shock on T is to emit; when set to OFF, a burst can be delivered without a shock in order to first locate the T-wave in the IEGM

Evaluate DFT Navigation: Tests \rightarrow DFT

Prerequisites

The following prerequisites must be met in order to carry out a DFT test:

Tested positive:

- Sensing (see Performing the sensing test [Page 227])
- Impedance (see Measuring impedance [Page 226])
- Shock impedance (see Measuring impedance [Page 226])

Parameters set for:

- Detection (see Detection parameters [Page 46])
- ATP and therapy shock (see Tachycardia therapy parameters [Page 61])
- Induction (see VT/VF induction [Page 232])
- Temporary VF therapy
- Manual shock (see Setting a manual shock [Page 236])

Note

The following applies to detection and therapy during the DFT test:

- The parameters of the Temporary VF therapy group box are only temporarily effective, in other words, only when the temporary program has been started and for as long as it remains active.
- As soon as the DFT test has ended or the temporary program has been actively stopped, the parameters for the permanent program become effective again.
- During execution of the DFT test, ICD therapy is activated temporarily in order to test the effectiveness of the therapy.

⚠ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

• Have a properly working external defibrillator ready.

★ WARNING

DFT test: ventricular arrhythmia does not terminate

If the ventricular arrhythmia persists uncontrolled, the patient is at risk of death.

Stop the DFT test by clicking on the following button:

[Stop temporary program]

- ⇒ The parameters of the permanent program will immediately become effective and may be able to terminate the ventricular arrhythmia.
- If the ventricular arrhythmia continues, escalate the measures to terminate it as necessary in the following manner:
 - Manual shock ightarrow Deliver manual shock
 - [Deliver emergency shock]
 - Use an external defibrillator

Performing the DFT test

Step-by-step instructions: Performing the DFT Test [Page 234]

Episode details

Details on the induced episode are displayed in the Measured values group box in the Episode field:

a)	The last episode is identified by the time it occurred.	
b)	***	Click on the symbol to display the IEGM.

Performing the DFT Test

Navigation: Tests \rightarrow DFT

↑ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

Have a properly working external defibrillator ready.

Instruction

To test the DFT, proceed as follows:

- 1. Evaluate the shock impedance values measured automatically: Follow-up \rightarrow Test results \rightarrow Shock impedance.
 - Or measure shock impedance using the 1-J test shock:

Tests \rightarrow DFT \rightarrow 1 J test shock \rightarrow Deliver 1-J test shock.

- 2. Evaluate the default settings in the Induction and Temporary VF therapy group boxes, and adjust the settings if necessary.
- 3. Use **[Start temporary program]** to start the temporary program.
- 4. Induce the tachyarrhythmia using [Start induction].
- 5. Stop the temporary program with [Stop temporary program].
- 6. Evaluate the induced episode in the Measured values group box.

Setting parameters for ATP/ EP study

Navigation: Tests ightarrow DFT ightarrow EPE/ATP

Objective

For EP (electrophysiological) study, you can start ATP manually for test purposes independently of whether you are using implanted device detection.

★ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

• Have a properly working external defibrillator ready.

MARNING

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH:
 Raise the programming head by at least 30 cm; the device will switch
 automatically to the permanent program.
- In the case of wandless telemetry:
 Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

Setting EP study/ATP

Select **[EPE/ATP]** to set the parameters for ATP.

Meaning of parameters

The following parameters are available for EP study/ATP:

Parameter	Description
Туре	Burst, Ramp, Burst+PES, Rapid pacing
Ventricular pacing (triple-chamber devices only)	The chamber in which you want pacing to take place
Number S1	Number of S1 stimuli of ATP
R-S1 interval	Start interval with which the system couples the burst to the R-wave
S1-S2 interval S2-S3 interval S3-S4 interval	Intervals of extrastimuli (PES) to be coupled to the basic interval
S1 decrement	Continuously reduces the pulse interval of the ATP from the second stimulus on, so that the ATP type takes on the form of a ramp

Setting a manual shock

Navigation: Tests ightarrow DFT ightarrow Manual shock

Objective

The manual shock is used in order to test the effectiveness of a therapy shock independently of detection by the device.

⚠ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

• Have a properly working external defibrillator ready.

Polarity

Normal:

	1st phase	2nd phase
RV shock coil	Negative	Positive
SVC shock coil or active housing	Positive	Negative

Reversed:

	1st phase	2nd phase
RV shock coil	Positive	Negative
SVC shock coil or active housing	Negative	Positive

Shock waveform

The parameter settings are defined as follows:

Waveform	Biphasic	Biphasic 2
Pause duration	1 ms	1 ms
Energy	Variable	Variable
End voltage 1st phase	40%	40%
Time 1st phase	Max. 23 ms	Max. 23 ms
End voltage 2nd phase	20%	Variable
Time 2nd phase	Max. 17 ms	2 ms

Rapid pacing

Navigation: Tests \rightarrow DFT \rightarrow EPE/ATP \rightarrow Type \rightarrow Rapid pacing

Objective

Rapid pacing of the ventricle is used to support certain steps of a transcatheter aortic valve implantation (TAVI).

Note

Rapid pacing utilizes high-rate pacing, which increases the risk of induced ventricular tachyarrhythmias.

Description

- The rate range of rapid pacing is between 150 and 300 bpm.
- You can enable or disable rapid pacing by clicking once on [Start] or [Stop].
- The maximum duration of fast overdrive pacing can be set in advance (to a maximum of 50 s). After this time has elapsed the overdrive pacing ceases.

Note

In order to further extend the duration of overdrive pacing within 10 s of the end of the current action by an additional 10 s, press the [+10 s] button

Note

Before you conduct rapid pacing, disable ICD therapy temporarily. Otherwise, rapid pacing will not be possible.

↑ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

• Have a properly working external defibrillator ready.

WARNING WARNING

Rapid pacing: critical pressure-free state of the heart

The pressure-free state of the heart may be poorly tolerated by patients.

- Continuously check with an ECG if the patient tolerates rapid overdrive pacing.
- Expose the patient to rapid overdrive pacing as briefly as is possible.
- Complete the TAVI procedure before terminating rapid overdrive pacing.
- If necessary, extend the duration of rapid overdrive pacing.
- Reactivate ICD therapy at a clinically optimal time. See also Activating and Deactivating ICD Therapy [Page 54].

AV Opt Test

Navigation: Tests \rightarrow AV opt.

or

 ${\sf Parameters} \to {\sf Bradycardia/CRT} \to {\sf AV} \ {\sf delay} \to {\sf AV} \ {\sf optimization} \ {\sf test}$

Optimize AV delays with AV Opt test

Objective

This test is helpful for optimizing the AV delay. Optimized AV delays are determined on the basis of P-wave measurements. These values are displayed for pacing and sensing and can be applied directly to the Dynamic AV delay parameter.

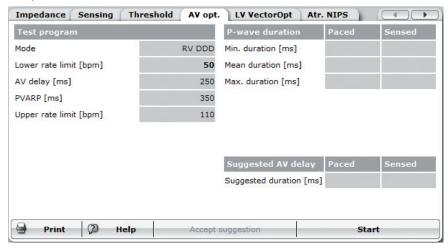
Performing AV optimization test

Proceed as follows:

- Select Tests → AV opt.
 Alternatively, access the test via:
 Select Parameters → Bradycardia/CRT → AV delay → AV optimization test.
- Begin the test immediately with the preset values or edit the parameter prior to the test: Lower rate limit.
 Once it starts, the test is performed by measuring the P waves.
- 3. Various intervals and the optimized AV delay are shown in the field: Suggested AV delay.
- 4. Select [Accept suggestion]. The optimized values will be applied to the AV delay, displayed there, and are available for further editing of the AV delay.

User interface

AV optimization test



Parameters for AV optimization test

The following parameters control the test:

Parameter	Meaning
Mode RV DDD	The test is performed in DDD mode and determines the perceived and paced duration of P-waves. RV indicates that pacing is only performed in the right ventricle.
Lower rate limit	Can be selected within the rate range.
AV delay	Fixed default
PVARP	Fixed default
Upper rate limit	Fixed default

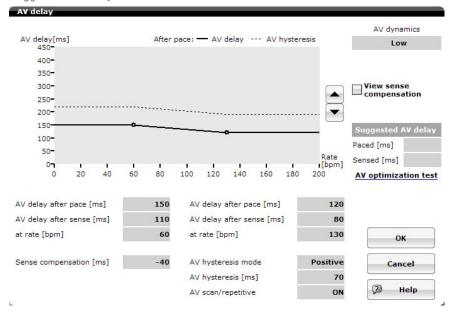
Using optimized values

The values determined for the AV delays were applied and are displayed in the AV delay window in the Suggested AV delay field.

The AV delay can be further edited using these optimized values.

User interface

Suggested AV delay



LV VectorOpt

LV pacing testing

Navigation: Tests \rightarrow LV VectorOpt

Testing and setting the parameters for LV VectorOpt

It is possible to test LV polarities and their parameters in the LV $\mbox{VectorOpt}$ tab, and to transfer these settings directly into the permanent program.

The following parameters can be displayed, tested and set:

- Polarities of LV pacing pacing polarities
- Pacing threshold of LV pacing with details on pulse amplitude and pulse width
- Pacing threshold for phrenic nerve stimulation (PNS) with values for pulse amplitude and pulse width
- Lead impedance
- Conduction times from RVp to LVs and from RVs to LVs

Setting general test parameters

Program the following parameters before the start of the test if the standard values are not sufficient:

- Mode: LV DDD; LV DDI; LV VVI
- Basic rate
- Start pulse

Automatic testing of LV pacing thresholds

The LV pacing threshold can be measured automatically. For this, select the **[Auto]** button. By selecting the individual check boxes in front of the vectors, the measurement can be selected or deselected. With an HF-T QP device, you can alternatively choose from 20 possible pacing polarities for the automatic LV threshold test under **[Settings]**.

• Select **[Start]** to automatically perform the LV threshold test with the selected pacing polarities.

Automatically measured values are stored automatically.

Manual testing of LV and PNS pacing thresholds

The LV pacing threshold and the PNS threshold can be measured manually.

- Select the [Manual] or [PNS] button to manually test the respective pacing thresholds.
- Set the LV polarity with up to 20 possible configurations by using the forward or backward arrow.
 - The LV polarity can also be set by clicking on the pacing polarity directly in the Pacing polarity dialog window.
- Select [Start] to manually perform the LV threshold test or the PNS test with the selected pacing polarities.

Saving manually determined measured values

Manually measured values can be saved separately for the LV pacing and phrenic nerve stimulation thresholds.

- Select [Save threshold] to manually save the determined pacing threshold.
- Select [Save PNS threshold] or [No PNS] to manually save the determined PNS threshold or a value of > 7.5 V if no phrenic nerve stimulation was noted.

Display of the measured values with direct programming

The most important measured values are displayed in the table on the left side of the window.

A more detailed list of all measured values can be found under [Results]. In addition to the important parameters in the table on the left of the window, the impedances, the usable range and a relative service time indication of each of the individual vectors compared to the vector with the relatively longest service time are also displayed here. Moreover, the LV polarities can be directly programmed from here as well.

Accept the appropriate polarity as the permanent program:

- Select [Results] and choose the appropriate pacing polarities from the result table by clicking on a measured LV polarity. The pacing polarities chosen in the table are automatically applied for the 1st LV stimulus and, in the case of MultiPole Pacing, also for the 2nd LV stimulus.
- Select [Program].
 - The selected settings are transferred to the parameters tab and become effective as the permanent program.
- The remaining time column indicates the impact on device service time for the displayed pacing configurations, where the RA and RV parameters are constant, and the LV parameters are adapted to the determined measurements. The designation Best indicates the longest service time among the measured pacing configurations. The following reduced service times refer to the specification Best.

The conditions for relative longevity calculation are:

- RA and RV: 3.0 V at 0.4 ms
- LV: derived from the measurement results
- 100% pacing in RA, RV and LV at 500 Ω lead load per channel
- Home Monitoring: OFF

History of the measured values

To display the measured value history:

• Select [History] to display the time sequence of the threshold measurements.

Measuring RV-LV conduction time in an HF-T QP device

Navigation: Tests \rightarrow LV VectorOpt

Parameters for measurement

This function serves to measure and evaluate the conduction time between an RVs or RVp and the various LV poles of a quadripolar LV lead.

 $\mathsf{Select} \ \mathsf{Tests} \to \mathsf{LV} \ \mathsf{VectorOpt} \to \mathsf{RV-LV} \ \mathsf{cond.} \ \mathsf{time}.$

The measurement can be performed with the following parameters:

- Measured path: $[RVs \rightarrow LVs]$ and/or $[RVp \rightarrow LVs]$
- Available modes: RV DDD, RV DDI; RV VVI
- Basic rate
- AV delay, set by default, cannot be changed

The selected measurement configuration can be set and used as standard by selecting the [Set as default] and [Use default] buttons.

The selection also applies to the window LV VectorOpt \rightarrow Settings for selecting the pacing polarities to be measured and for conduction time measurements [RVs \rightarrow LVs] and/or [RVp \rightarrow LVs].

Measuring RV-LV conduction time

This function serves to measure and evaluate the conduction time between an RV tip and the LV poles.

There are two ways to do this:

- Measure the purely intrinsic conduction time [RVs \rightarrow LVs]
- Measure the conduction time generated after the delivery of a right ventricular pace [RVp → LVs]
- Choose the desired measurement method, or both, by selecting or deselecting the appropriate check boxes.
- Select [Measure] to measure the conduction time.

The measured conduction times are displayed in the window of the same name, as well as in further windows: [LV VectorOpt]; [Results].

If the measurements must be repeated, the check boxes must be selected again.

The longest conduction time is highlighted in various result or selection dialogs of the LV VectorOpt test to facilitate the selection of potential LV polarities. Thus supporting the principle that pacing is optimal when the left ventricular area is last activated.

NIPS - Non-Invasive Programmed Stimulation

NIPS – select therapy Navigation: Tests \rightarrow Atr. NIPS

Objective

Pulse delivery of the device can temporarily be controlled using the programmer for the acute therapy of atrial arrhythmias.

Burst and programmed pacing is possible on the Atr. NIPS tab only in the atrium for multi-chamber devices.

M WARNING

NIPS: triggering arrhythmias

Depending on the type of high-rate pacing and the predispositions of the patient, dangerous arrhythmias, including ventricular fibrillation, may be triggered.

- NIPS may only be performed by physicians familiar with high-rate pacing procedures.
- During electrophysiological studies, observe the usual precautionary measures.

⚠ WARNING

Display of incorrect data in case of interrupted telemetry

Interrupted telemetry between the device and the programmer can cause false data to be displayed on the programmer.

 In order to continuously monitor the effectiveness of pacing and the plausibility of the test results at any time, use an external ECG device during tests.

Selecting the form of therapy

Proceed as follows:

If	Then
you want to trigger a pulse train with fixed or variable rate,	select the Burst pacing form of therapy.
you want to trigger a full electro- physiological pacing program with up to three extrastimuli,	select the Programmed stimulation form of therapy.

Starting the backup program

Proceed as follows in order to ensure backup pacing (backup program):

- 1. Select **Tests** \rightarrow **Atr. NIPS**.
- 2. Select Backup stimulation and the pacing rate you want to achieve. Backup pacing is performed in VVI mode as a temporary program with the selected rate.
 - Select [Start backup program].
- 3. Select OFF if you want to carry out NIPS without backup pacing.

Cancel backup program

The rate of backup pacing cannot be changed during burst pacing and programmed pacing.

Step	Action	Remark
1	Select [Stop backup program].	The backup program is canceled and the permanent program is transmitted to the device.

Note

Running follow-ups by applying the programming head

Independent of the option of canceling, NIPS can be stopped at any time by lifting the programming head (at least 30 cm). The device then switches back to its permanent program.

Switching the report ON and OFF

An automatic report is offered for NIPS. If it is activated, the ECG is printed automatically.

The report can be switched on or off under: $\mathbf{Preferences} o \mathbf{Tests} o \mathbf{NIPS} o$ Print setup

NIPS - description of burst pacing

The report can be switched on or off under: **Tests** \rightarrow **Atr. NIPS**

Description

Using burst pacing it is possible to deliver a pulse sequence with a fixed or variable rate as long as you keep the [Burst] button pressed down.

The parameters for burst pacing are located on the right-hand side of the NIPS window.

Parameter	Description
Start	Initial rate for burst stimulation
Min.	Minimum rate with decreasing ramp
Max.	Maximum rate with increasing ramp
Burst rate (Ramp)	The step size for increases or reductions in the ramp function is permanently fixed at 10 bpm/s.

NIPS - executing burst pacing

Navigation: Tests \rightarrow Atr. NIPS



★ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

• Have a properly working external defibrillator ready.

Starting/stopping burst pacing

Proceed as follows:

Step	Action	Result
1	Select [Start backup program].	NIPS is activated as a temporary program in the device. The status bar displays: Transmission of the temporary program was successful The backup packing is ensured and controlled by the backup program.
2	Press the middle section of the [Burst] button and hold down the button for the duration of the burst.	As long as the button remains pressed, burst pacing at the specified rate will accompany backup pacing. When the button is released, only backup pacing is active.
3	Select [Stop backup program].	The backup program is canceled and the permanent program is transmitted to the device.

Varying the burst rate during pacing

The burst rate can be gradually changed during pacing (ramp function). This ramp function is facilitated by a three-part button.

If	Then
you wish to increase the burst rate,	press the right-hand [+] section of the [Burst] button and hold down the button for the duration of the burst. Based on the preset value, the burst rate is increased incrementally until the specified maximum has been reached.
you want to decrease the burst rate,	press the left-hand [-] section of the [Burst] button and hold down the button for the duration of the burst. Based on the preset value, the burst rate is decreased incrementally until the specified minimum has been reached.
you want to cancel burst stimulation,	release the [Burst] button. After releasing the button, the burst pacing is automatically ended. Backup pacing remains active.

⚠ WARNING

NIPS: reduction in pulse amplitude due to battery voltage drop

If the rate and pulse amplitude are set very high and the pulse width is set too long at the same time, the battery voltage can temporarily drop so low that the actual pulse amplitude drops well below the programmed value.

• Continuously check the pacing efficiency using ECG monitoring.

NIPS – description of programmed stimulation

$\textbf{Navigation: Tests} \rightarrow \textbf{Atr. NIPS}$

With programmed stimulation, it is possible to trigger a full electrophysiological pacing program with up to three extrastimuli.

Programmed stimulation is used in the ventricle using the EPE/ATP function. See the DFT tab: Tests \rightarrow DFT \rightarrow EPE/ATP

Description

The following parameters can be set for programmed stimulation:

Parameter	Description
S1-S1 interval	Basic interval for programmed stimulation
S1 cycles	The basic interval is repeated for the specified number of cycles before the extrastimuli are added. If the value 0 is specified, the extrastimuli become effective immediately after the start of the basic interval.
S1-S2 interval S2-S3 interval S3-S4 interval	Intervals of the extrastimuli that are coupled to the basic interval. The method is described below and applies to all intervals of the extrastimuli.

Couple the pacing intervals

The extrastimuli are coupled to the basic interval as follows:

If	Then
pacing is to be carried out without the first extrastimulus (S1-S2 interval = None),	all further extrastimuli are not coupled, either.
a numerical interval value is selected for the S1-S2 interval,	the first extrastimulus is coupled after the set cycles of the basic interval are complete. Stimulation takes place at the end of the S1 - S2 interval.
<pre>pacing is to be carried out without the second extrastim- ulus (S2-S3 interval = None),</pre>	all further extrastimuli are not coupled, either.
a numerical value is selected for the S2-S3 interval,	the first extrastimulus and then the second extrastimulus is coupled after the set cycles of the basic intervals are complete. Pacing occurs at the end of the S1-S2 and S2-S3 intervals respectively.
a numerical value is selected for the S3-S4 interval,	the first extrastimulus, then the second extrastimulus, and finally the third extrastimulus is coupled after the set cycles of the basic intervals are complete. Pacing occurs at the end of the S1-S2, S2-S3, and S3-S4 intervals respectively.

NIPS – executing programmed stimulation

Navigation: Tests \rightarrow Atr. NIPS

Executing programmed stimulation

Proceed as follows:

Step	Action	Result
1	Select [Start backup program].	NIPS is activated as a temporary program in the device. The status bar displays: Transmission of the temporary program was successful. Backup pacing is ensured and controlled by the backup program.
2	Select [Start programmed stimulation].	NIPS is activated as a temporary program in the device. Programmed stimulation commences in addition to backup stimulation. This remains active until the set sequence has been carried out in full or until the function is ended manually. After this, only backup pacing is active.
3	Select [Stop backup program].	The backup program is canceled and the permanent program is transmitted to the device.

⚠ WARNING

NIPS: reduction in pulse amplitude due to battery voltage drop

If the rate and pulse amplitude are set very high and the pulse width is set too long at the same time, the battery voltage can temporarily drop so low that the actual pulse amplitude drops well below the programmed value.

Continuously check the pacing efficiency using ECG monitoring.

⚠ WARNING

Tests with high pacing rates: increased risk of induced ventricular arrhythmias

During testing, the risk of inducing ventricular arrhythmia is increased.

• Have a properly working external defibrillator ready.

Retrograde Conduction Test

Performing the retrograde conduction test

Navigation: Tests \rightarrow Retrogr. conduct.

Objective

Starting from the measured conduction times, you can set the temporal control parameters in order to optimize hemodynamics and prevent pacemaker-mediated tachycardias.

WARNING

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH: Raise the programming head by at least 30 cm; the device will switch automatically to the permanent program.
- In the case of wandless telemetry: Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

Performing the test

- 1. Evaluate the default parameter values for the test program and adjust them if necessary.
- 2. In the Basic rate field, select the rate with which pacing is required during testing. The rate must be above the intrinsic rhythm.
- 3. Start the test by pressing [Start].

The test ends automatically after 5 conductions or 10 seconds. During measurement, the system displays the following on the screen:

- On the IEGM display: the current measured conduction time
- under Measured values: the minimum, mean and maximum conduction time measured over a number of periods
- 4. Use [Cancel] to abort the test if necessary.

Details

Test for retrograde conduction – details [Page 247]

Test for retrograde conduction - details

Navigation: Tests \rightarrow Retrogr. conduct.

Description

This test determines whether retrograde conduction occurs and, if so, how long latency is.

The following latencies are measured:

- Right ventricle (pacing) and atrium (dual-chamber devices)
- Left or right ventricle and atrium (triple-chamber devices)

Prerequisites

The test can be performed only under the following conditions:

- The device was successfully interrogated.
- Pacing is possible in the right or left ventricle.
- Sensing is possible in the right atrium.

Process sequence

- The system updates the display with each new measurement, shows a progress bar on the information line and displays the [Cancel] button instead of the [Start] button.
- The user can print out the measurements and parameters.
- The user can select a different chamber, change parameters if necessary and start a new measurement process.

2.10 ProMRI

Preparing the MRI Scan

MRI program - device preparation

MRI manual Note

Always observe the information given in the MRI manual by BIOTRONIK:

 It can be found at: manuals.biotronik.com/ Product Group: ProMRI -> Product: ProMRI

↑ WARNING

Transmission of incorrect parameter values in case of interrupted telemetry

Distortion of parameter values during transmission may occur if telemetry is interrupted between the programmer and the device.

Ending temporary program:

- In the case of telemetry with PGH:
 Raise the programming head by at least 30 cm; the device will switch
 automatically to the permanent program.
- In the case of wandless telemetry:
 Stop the temporary program using the user interface of the programmer: The permanent program will become active immediately.
- If these measures do not work, turn the programmer off, restart it and, if necessary, reposition the programming head.

Selecting a program

Select your program setting with the $MRI \rightarrow MRI$ program function:

Parameter setting	Program
ON	MRI program: activate
OFF	MRI program: deactivate
AUTO	MRI program = automatic activation upon detection of a magnetic field: The default MRI program remains active for as long as the MRI scan continues.

Device preparation

Step	Action
1	MRI checklist group box:
	Make sure that all the preconditions for an MRI scan are fulfilled.
	• Tick the [Patient is approved for MRI scan] check box.
2	Only when Program = AUTO:
	Select Expiration date. Enter a date that is not more than two weeks in the future. The magnetic sensor will then be enabled during the set period.
3	Select an MRI mode:
	OFF – recommended for patients who are not pacemaker- dependent
	D00, V00 – recommended for pacemaker-dependent patients, depending on the particular indication
	D00/BiV or V00/BiV – recommended for pacemaker- dependent patients with a triple-chamber pacemaker for biventricular pacing
4	You can use the [Test MRI] button to test whether the pacing settings are suitable for the patient before sending the MRI program.
5	Select [Program] to transmit the settings to the device.

Patient information

Radiological information for the patient [Page 251]

MRI program - details

MRI program: AUTO Note

Using the MRI AutoDetect function requires a bipolar sensing polarity in the permanent program. This function is only available for the models of the 5 and 7 series.

- With the MRI AutoDetect function, the device has a sensor which recognizes
 the fields of an MRI scanner and automatically switches into the predefined
 MRI mode. 1 minute after leaving the MRI scanner, the device automatically
 switches back to the permanent program.
- The MRI AutoDetect function is active for a maximum of 14 days from the day it is programmed and allows for an indefinite number of MRI scans during this period. The programming expires at 23:59 h of the selected day.
- Thus even as early as the day of the preliminary examination the device can be set to an automatic MRI mode as long as the planned MRI scan is to take place within the next 2 weeks. The device does not need to be reprogrammed after the MRI scan.
- When Home Monitoring is activated, a Home Monitoring-supported follow-up is performed during the night after the MRI scan, which documents the device status after an MRI scan.

ProMR

MRI program: 0N

- With devices containing MRI AutoDetect, you can also switch on the MRI program manually.
- Switch off the MRI program after the MRI scan.

Patient information Radiological information for the patient [Page 251]

Radiological information for the patient

Display and print information

By using the **[Radiological information]** button, you can view radiological information and print it out to pass it on to the patient for MR scanning if required.

3 Technical Data

3.1 Parameters

Note: Unless described separately, information for device type HF also applies to device type HF QP.

Tachycardia

General ICD therapy

Therapy readiness:

Parameter	Range of values	Standard	VR	DX	DR	HF
ICD therapy	OFF; ON	ON	Х	Х	Х	Х
Programs	Display standard program; Display safe program; Display first interrogated program; Individual 1, 2, 3; ProgramConsult	_	X	X	X	X

Detection

Note: Values can be set both in bpm and in ms.

Interval rates

Parameter	Range of values	Standard	VR	DX	DR	HF
Interval AT/AF	240 600 ms 100 (10) 250 bpm	300 ms 200 bpm		Х	Х	X
Interval VT1	OFF; 100 222 bpm	OFF	Х	Х	Х	X
Interval VT2	OFF; 120 222 bpm	OFF	Х	Х	Х	Х
Interval VF	OFF; 150 250 bpm	200 bpm	Х	Х	Х	X

Detection counter and redetection counter

Parameter	Range of values	Standard	VR	DX	DR	HF
Detection counter VT1	10 (2) 100	28	X	Х	Х	Х
Detection counter VT2	10 (2) 80	20	Х	Х	Х	Х

Detection counter and redetection counter

	-					
Parameter	Range of values	Standard	VR	DX	DR	HF
Detection counter VF	6 out of 8; 8 out of 12; 10 out of 14; 12 out of 16; 16 out of 20; 18 out of 24; 20 out of 26; 22 out of 30; 24 out of 30; 30 out of 40	18 out of 24	X	X	X	X
Redetection counter VT1	10 (2) 50	20	Х	Х	Х	Х
Redetection counter VT2	10 (2) 40	14	Х	Х	Х	Х
Redetection counter VF	6 out of 8; 8 out of 12; 10 out of 14; 12 out of 16; 16 out of 20; 18 out of 24; 20 out of 26; 22 out of 30; 24 out of 30	8 out of 12	X	X	X	X

Smart detection, onset, and stability criterion

Parameter	Range of values	Standard	VR	DX	DR	HF
SMART detection VT1/VT2	OFF; ON	ON		Х	Х	X
SMART detection ON: Onset VT1/VT2	4 [4] 32%	20%		Х	Х	X
SMART detection ON: Stability VT1/VT2	8 [4] 48%	12%		Х	Х	X
SMART detection OFF: Onset VT1/VT2	OFF; 4 (4) 32%	20%	Х	Х	Х	X
SMART detection OFF: Stability VT1/VT2	OFF; 8 (4) 48% 8 (4) 48 ms	48 ms	Х	X	X	X

Morphology criterion

Parameter	Range of values	Standard	VR	DX	DR	HF
SMART detection OFF: MorphMatch VT1/VT2	OFF; Monitoring; ON	ON	Х	X	Х	Х
MorphMatch threshold	Low (maximum value for threshold 58); STD (maximum value for threshold 76); High (maximum value for threshold 86)	STD	X	X	X	X

Sustained VT

Parameter	Range of values	Standard	VR	DX	DR	HF
Sustained VT	OFF; 1; 2; 3; 5; 10; 20; 30 min	OFF	Х	Х	Х	X

Therapy: atrial therapy

The following parameters apply to series 7 devices:

Atrial therapy in the presence of stable atrial flutter

Parameter	Range of values	Standard	VR	DX	DR	HF
ATP type	OFF; Burst; Ramp	OFF	'		Х	Х
Number S1	2 (1) 10	5			Х	Х
P-S1 interval	70 (5) 95%	80%			Х	Х
S1 decrement	5 (5) 40 ms	10 ms		-	Х	Х
Backup stimulation	OFF; 70; 90	OFF			Х	Х

The following parameters apply to series 7 devices:

Atrial therapy in the presence of instable atrial flutter

Parameter	Range of values	Standard	VR	DX	DR	HF
Therapy	OFF; HF burst (high frequency burst)	OFF			Х	X
Rate	10 (5) 40 Hz	40 Hz			Х	Х
Duration	2 (1) 10	3 s			Х	Х
Backup stimulation	OFF; 70; 90	OFF			Х	Х

Therapy: ventricular ATP

ATP for VT1 and VT2

Parameter	Range of values	Standard	VR	DX	DR	HF
Attempts	OFF; 1 (1) 10	OFF	Х	Х	Х	X
ATP type	Burst; Ramp	Burst	Х	Х	Х	X
Ventricular pacing	RV; LV; BiV	RV				X
Number S1	1 (1) 15	5	Х	Х	Х	X
Add. S1	OFF; ON	ON	Х	Х	Х	X
R-S1 interval	70 (5) 85; 88; 90; 95%	80%	Х	Х	Х	Х
S1 decrement	5 (5) 40 ms	10 ms	Х	Х	Х	Х
Scan decrement	OFF; 5 (5) 40 ms	OFF	Х	Х	Х	X
ATP optimization	OFF; ON	OFF	Х	Х	Х	X

ATP in VF

Parameter	Range of values	Standard	VR	DX	DR	HF
ATP type	OFF; Burst; Ramp	Burst	Х	Х	Х	Х
Ventricular pacing	RV; LV; BiV	RV				X
Number S1	1 (1) 15	8	Χ	Х	Х	Χ
R-S1 interval	70 (5) 85; 88; 90; 95%	88%	X	Х	Х	X
ATP type ramp: S1 decrement	5 (5) 40 ms	10 ms	X	Х	Х	X
Series 5 and 7: Early ATP delivery	OFF; ON	OFF	Х	Х	Х	X

Therapy: shock

Shock in VT1/VT2

Parameter	Range of values	Standard	VR	DX	DR	HF
Possible number of shocks	0; 1; 2; 6; 8	8	Х	Х	Х	Х
1st shock	OFF; 2 (2) 20 (5) 40 J	40 J	Х	Х	X	X
2nd shock	OFF; 4 (2) 20 (5) 40 J	40 J	Х	Х	Х	X
3rd - nth shock	OFF; 4*40 J; 6*40 J	6*40 J	Х	Х	Х	Х

Shock in VF

Parameter	Range of values	Standard	VR	DX	DR	HF
Possible number of shocks	6; 8	8	Х	Х	Х	Х
1st shock	2 (2) 20 (5) 40 J	40 J	Х	Х	Х	Х
2nd shock	4 (2) 20 (5) 40 J	40 J	Х	Х	Х	Х
3rd - nth shock	4*40 J; 6*40 J	6*40 J	Х	Х	Х	Х

Shock polarity, shock waveform, shock path

Parameter	Range of values	Standard	VR	DX	DR	HF
Confirmation	OFF; ON	ON	Х	Х	Х	Х
Series 3: Polarity	Normal; Reverse; Normal -> alternating	Normal	Х	Х	Х	X
Series 5 and 7: Polarity	Normal; Reverse; Normal -> alternating; Reverse -> alternating	Normal	Х	Х	X	X

Shock polarity, shock waveform, shock path

Parameter	Range of values	Standard	VR	DX	DR	HF
Series 3: Shock waveform	Biphasic; Biphasic 2;	Biphasic	Х	X	X	Х
Series 5 and 7: Shock waveform	Biphasic; Biphasic 2; Biphasic -> alternating; Biphasic 2 -> alter- nating	Biphasic	Х	X	X	X
Shock path	RV -> housing + SVC RV -> housing RV -> SVC	RV -> housing + SVC	Х		X	X
		RV -> housing		Х		

Sensing

Sensitivity

Atrial sensing parameters

Parameter	Range of values	Standard	VR D	K DR	HF
Sensing	STD; OFF	STD	Х	Х	Х
Series 5 and 7: DX sensing	ON; OFF	OFF		·	X
Upper threshold	25; 50; 75%	50%		Х	Х
	Series 5 and 7: In the case of DX sensing: 25, 50; 75%	75%	Х		X

Right ventricular sensing parameters

Parameter	Range of values	Standard	VR	DX	DR	HF
Sensing	STD; TWS; VFS; IND	STD	Х	Х	Х	X
Upper threshold	50; 75% In the case of TWS: 75%	50%	Х	Х	X	Х
Upper threshold duration after detection	110; 150 (50) 500 ms VFS: 110 ms	350 ms	Х	X	X	X
Upper threshold duration after pacing	110; 150 (50) 500 ms VFS: 110 ms	400 ms	Х	X	X	X
Lower threshold	25; 50%	25%	X	Х	Х	X
T-wave suppression after pacing	OFF; ON	OFF	Х	Х	X	X

Left ventricular sensing parameters

Parameter	Range of values	Standard	VR DX DR	HF
Sensing	STD; OFF; IND	STD		Х
Upper threshold	50; 75%	50%		X
Upper threshold duration after detection	110; 150 (50) 500 ms VFS: 110 ms	350 ms		X
Upper threshold duration after pacing	110; 150 (50) 500 ms VFS: 110 ms	400 ms		X
Lower threshold	25%	25%		X

Parameters

Thresholds

Parameter	Range of values	Standard	VR	DX	DR	HF
Minimum threshold A	0.2 (0.1) 2.0 mV	0.4 mV		Х	X	Х
Minimum threshold RV	0.5 (0.1) 2.5 mV	0.8 mV	X	X	Х	Х
Minimum threshold LV	0.5 (0.1) 2.5 (0.5) 5.0 mV	1.6 mV				X

Bradycardia/CRT

Timing: basic rate day/night and rate hysteresis

Parameter	Range of values	Standard	VR	DX	DR	HF
Basic rate	30 (5) 100 (10)	40 bpm	Х	Х		
	160 bpm	60 bpm			Х	Х
Rate hysteresis	OFF; -5 (-5)25 (-20) 65 bpm	OFF	X	X	X	Х
Scan/repetitive	OFF; ON	ON	Х	Х	Х	Х
Night rate	OFF; 30 (5) 100 bpm	OFF	Х	Х	X	Х
Night begins	00:00 (1 min) 23:59 hh:mm	10:00 PM hh:mm	Х	Х	Х	Х
Night ends	00:00 (1 min) 23:59 hh:mm	6:00 AM hh:mm	Х	Х	Х	X

Timing: rate adaptation via accelerometer

Parameter	Range of values	Standard	VR	DX	DR	HF
Maximum sensor rate	80 (10) 160 bpm	120 bpm	Χ	Х	Х	Х
Sensor gain	AUTO; Very low (1.3); Low (3); Medium (6); High (12); Very high (26)	Medium (6)	X	X	X	X
Sensor threshold	Very low (0); Low (3); Medium (7); High (11); Very high (15)	Medium (7)	Х	X	X	X
Rate increase	1; 2; 4; 8 bpm/cycle	2 bpm/ cycle	Х	X	X	X
Rate decrease	0.1; 0.2; 0.5; 1.0 bpm/ cycle	0.5 bpm/ cycle	Х	X	X	X
Series 5 and 7: Rate fading	OFF; ON	OFF	Х	Х	Х	Х

Timing: rate adaptation via CLS

The following parameters apply to series 7 devices:

Range of values	Standard	VR	DX	DR	HF
80 (10) 160 bpm	120 bpm	Х	Х	Х	Х
Very low; Low; Medium; High; Very high	Medium	Х	Х	Х	Х
OFF; +10 (+10) +50 bpm	+20 bpm	Х	Х	Х	X
Yes; No	No	Х	Х	Х	
	Yes				Х
	80 (10) 160 bpm Very low; Low; Medium; High; Very high OFF; +10 (+10) +50 bpm	80 (10) 160 bpm 120 bpm Very low; Low; Medium; Medium High; Very high OFF; +20 bpm Yes; No No	80 (10) 160 bpm 120 bpm x Very low; Low; Medium; High; Very high Medium x 0FF; +10 (+10) +50 bpm +20 bpm x Yes; No No x	80 (10) 160 bpm 120 bpm x x Very low; Low; Medium; High; Very high Medium x x 0FF; +10 (+10) +50 bpm +20 bpm x x Yes; No No x x	80 (10) 160 bpm 120 bpm x x x Very low; Low; Medium; High; Very high Medium x x x 0FF; +10 (+10) +50 bpm +20 bpm x x x Yes; No No x x x

Timing: upper rate

Parameter	Range of values	Standard	VR	DX	DR	HF
Upper rate	90 (10) 170 bpm	130 bpm	'	Х	Х	Х
Atrial upper rate	OFF; 175; 200; 240 bpm	200 bpm			Х	X

Timing: mode switching

Parameter	Range of values	Standard	VR	DX	DR	HF
Intervention rate	OFF; 120 (10) 200 bpm	160 bpm	,	Х	Х	Х
Mode	After mode VDD(R): VDI(R)	VDIR		Х	Х	Х
	Series 3: After mode DDD(R): DDI(R)	DDIR			Х	Х
	Series 5 after mode DDD(R), DDD-ADI(R): DDI(R)	DDIR			X	X
	Series 7 after mode DDD(R), DDD-CLS, DDD-ADI(R): DDI(R)	DDIR			X	X
Modification of basic rate	OFF; 5 (5) 30 bpm	10 bpm		X	X	Х
Onset criterion	3 (1) 8 (out of 8)	5		Х	Х	Х
Resolution criterion	3 (1) 8 (out of 8)	5		Х	Х	X
After mode switching: Rate	OFF; 5 (5) 50 bpm	10 bpm		Х	X	Х
After mode switching: Duration	1 (1) 30 min	1 min		Х	Х	Х
Series 5 and 7: Rate stabilization with mode switching	ON; OFF	OFF		Х	X	Х

Pacing: ventricular pacing suppression

The following parameters apply to series 5 and series 7 devices:

Parameter	Range of values	Standard	VR DX	DR	HF
Vp suppression	OFF; ON	OFF		Х	Х
Pacing suppression after consecutive ventricular sensing	1 (1) 8	6		Х	Х
Pacing supported after X-out-of-8 cycles	1; 2; 3; 4	3		Х	Х

Pacing: ventricular pacing

Parameter	Range of values	Standard	VR DX DR	HF
Permanent	RV; BiV; LV	BiV		Х
Triggering	OFF; RVs; RVs+PVC	RVs		Χ
LV T-wave protection	OFF; ON	ON		Χ
Maximum trigger rate: DDD-CLS, DDD(R), VDD(R)	UTR + 20; 90 (10) 160 bpm	UTR + 20		X
Maximum trigger rate: DDI(R), VDI(R), WI-CLS, VVI(R), D00, V00	90 (10) 160 bpm	130 bpm		X
Initially paced chamber	RV; LV	LV		Х
VV delay after Vp	0 (5) 100 ms	0 ms		X

The following parameters apply to series 7 devices:

Parameter	Range of values	Standard	VR DX DR HF
CRT AutoAdapt	OFF; AVadapt; ON	OFF	Х
Adaptive AV reduction	0.5 (0.1) 0.9	0.7	Х
Lower limit adaptive AV delay	50 (10) 150 ms	50 ms	X

Timing: AV delay

Parameter	Range of values	Standard	VR	DX	DR	HF
AV dynamics	Low; Medium; High; Fixed; (Individual)	Low		Х	Х	Х
AV delay 1 after pacing	40 (5) 350 ms Only for Fixed, also: 15	_			Х	X
AV delay 1 after sensing	Either automatic: AV delay 1 after pacing + sense compensation	_			X	X
	Or: 15 (for Fixed); 40 (5) 350 ms	_		Х		
AV delay 1 for rate 1	50 (10) 130 bpm	60 bpm		Х	Х	Х
AV delay 2 after pacing	40 (5) 350 ms Only for Fixed, also: 15	_			Х	X
AV delay 2 after sensing	Either automatic: AV delay 2 after pacing + sense compensation	_			X	X
	Or: 15 (for Fixed); 40 (5) 350 ms	_		Х		
AV delay 2 for rate 2	60 (10) 140 bpm	130 bpm		Х	Х	Х
Sense compensation	OFF; -5 (-5)120 ms	-40 ms			Х	Х
	-5 (-5)120 ms				-	

Parameter	Range of values	Standard	VR	DX	DR	HF
AV hysteresis mode	OFF; Positive; Negative; IRSplus	OFF	'	X	X	
	OFF; Positive; Negative	OFF				X
AV hysteresis (positive)	70; 110; 150; 200 ms	70 ms		Х	Х	Х
CLS modes: AV hysteresis (positive)	70; 110; 150 ms	110 ms			Х	X
AV hysteresis (negative)	10 (10) 150 ms	50 ms		Х	Х	Х
AV scan and repetitive (positive)	OFF; ON	ON		Х	X	X

Pacing: post-shock

Parameter	Range of values	Standard	VR	DX	DR	HF
Post-shock duration	OFF; 10 s; 30 s; 1 min; 2 min; 5 min; 10 min	10 s	Х	X	X	X
Post-shock basic rate	30 (5) 100 (10) 160 bpm	60 bpm	Х	Х	Х	X
AV delay post shock	50 (10) 350 ms	140 ms			Х	X
Ventricular post-shock pacing	RV; BiV	RV				X
Post-shock LV T-wave protection	OFF; ON	OFF				Х
Post-shock trigger	OFF; RVs; RVs+PVC	OFF		-		Х

Pacing: atrial and ventricular pacing

Parameter	Range of values	Standard	VR	DX	DR	HF
Pulse amplitude A	0.5 (0.25) 4.0 (0.5) 6.0; 7.5 V	AUT0			X	×
Pulse width A	0.4; 0.5 (0.25) 1.5 ms	0.4 ms			Х	X
Pulse amplitude RV	0.5 (0.25) 4.0 (0.5) 6.0; 7.5 V	AUT0	Х	X	X	X
Pulse width RV	0.4; 0.5 (0.25) 1.5 ms	0.4 ms	Х	Х	X	Х
Pulse amplitude LV	0.5 (0.25) 4.0 (0.5) 6.0; 7.5 V	AUT0				Х
Pulse width LV	0.4; 0.5 (0.25) 1.5 ms	0.4 ms				X

Pacing: ventricular MultiPole pacing

Parameter	Range of values	Standard	QP
Pulse amplitude LV and 2nd LV	0.5 (0.25) 4.0(0.5) 6.0; 7.5 V	AUTO	Х
Pulse width LV and 2nd LV	0.4; 0.5 (0.25) 1.5 ms	0.4 ms	X
LV – 2nd LV delay	0 (5) 50 ms	0 ms	Х

Pacing: atrial capture control

The following parameters apply to series 5 and series 7 devices:

Parameter	Range of values	Standard	VR DX DR HF
Atrial capture control	OFF; ATM; ON	ON	х х
Threshold test start	With ON: 2.5 (0.5) 5.0 V	3.5 V	X X
Minimum amplitude	0.5 (0.25) 4.0 V	1.0 V	X X
Safety margin	0.5; 1.0; 1.2 V	1.0 V	ХХ

The following parameters apply to series 3 devices:

Parameter	Range of values	Standard	VR DX	DR	HF
Atrial capture control	OFF; ATM	ATM		Х	Х
Threshold test start	With ATM: 3.5 V	Perma- nent		Х	X

Pacing: ventricular capture control

The following parameters apply to series 5 and series 7 devices:

Parameter	Range of values	Standard	VR	DX	DR	HF
Ventricular capture control RV + LV	OFF; ATM; ON	ON	Х	Х	Х	Х
Threshold test start	With ON: 2.5 (0.5) 5.0 V	3.5 V	Х	Х	Х	Х
Minimum amplitude	1.0 (0.25) 4.0 V	1.0 V	Х	Х	Х	X
Safety margin RV	1.0; 1.2 V	1.0 V	Х	X	Х	X
Safety margin LV1 and LV2	0.5; 1.0; 1.2 V	1.0 V				X

Parameters

The following parameters apply to series 3 devices:

Parameter	Range of values	Standard	VR	DX	DR	HF
Ventricular capture control RV + LV	OFF; ATM	ATM	Х	Х	Х	Х
Threshold test start	With ATM: 3.5 V	Perma- nent	Х	Х	Х	Х

Blanking and refractory periods

Parameter	Range of values	Standard VR	DX	DR	HF
PVARP	AUTO; 175 (25) 600 ms	225 ms	X	Х	Х
PVARP extension	OFF; ON	ON	Χ	Х	Х
Blanking RV after atrial pacing	40 (10) 100 ms	50 ms		Х	Х
LV blanking after RV pacing	50 (10) 100 ms	80 ms			Х
RV blanking after LV pacing	50 (10) 100 ms	80 ms			X
Far-field protection after Vs	AUTO; OFF; 25 (25) 225 ms	AUTO	X	Х	X
Far-field protection after Vp	50 (25) 225 ms	75 ms	X	Х	X

PMT protection

Parameter	Range of values	Standard	VR	DX	DR	HF
PMT detection/termina- tion	OFF; ON	ON	·	X	Х	Х
VA criterion	250 (10) 500 ms	350 ms		Χ	Χ	Х

Parameters

LV lead configuration

Parameter	Range of values	Standard	HF	QP
LV pacing polarity (IS-1)	LV1 -> LV2 LV1 -> RV LV1 -> housing	LV1 -> RV	Х	
	LV2 -> LV1 LV2 -> RV			
Pacing polarity LV (IS4)	LV1 -> LV2 LV1 -> LV3 LV1 -> LV4 LV1 -> RV LV1 -> housing LV2 -> LV1 LV2 -> LV3 LV2 -> LV4 LV2 -> RV LV2 -> housing LV3 -> LV1 LV3 -> LV2 LV3 -> LV4 LV3 -> RV LV3 -> RV LV3 -> RV LV4 -> LV1 LV3 -> RV	LV1 -> LV2		X
	LV4 -> housing			

Parameter	Range of values	Standard	HF	QP
7 series: LV pacing polarity (IS4, MultiPole Pacing)	OFF LV1 -> LV2 LV1 -> LV3 LV1 -> LV4 LV1 -> RV LV1 -> housing LV2 -> LV1 LV2 -> LV3 LV2 -> LV4 LV2 -> RV LV2 -> RV LV2 -> RV LV3 -> LV1 LV3 -> LV1 LV3 -> LV2 LV3 -> LV4 LV3 -> RV LV4 -> LV4 LV4 -> LV1	OFF		X
	LV4 -> LV2 LV4 -> LV3 LV4 -> RV LV4 -> housing			
Sensing polarity LV (IS-1)	LV1 -> housing LV1 -> LV2	LV1 -> housing	Х	
Sensing polarity LV (IS4)	LV1 -> LV2 LV1 -> housing LV2 -> LV3 LV2 -> housing LV3 -> LV4 LV3 -> housing LV4 -> housing	LV1 -> LV2		X

Home Monitoring

Setting options on the programmer:

Parameter	Range of values	Standard	VR	DX	DR	HF
Home Monitoring	OFF; ON	OFF	Х	Х	Х	Х
Time of transmission	STD; 00:00 (1:00 AM) 11:00 PM hh:mm	STD	Х	X	X	X
IEGM for therapy episodes	OFF; ON	ON	Х	Х	Х	Х
IEGM for monitoring episodes	OFF; ON	ON	Х	Х	Х	Х
Ongoing atrial episode	OFF; 6; 12; 18 h	12 h		Х	Х	Х
QuickCheck	OFF; ON	ON	X	Х	Х	Х

Setting options in the Home Monitoring Service Center (HMSC):

Parameter	Range of values	Standard	VR	DX	DR	HF
Transmission on	XX.XX.XXXX	Follow-up + 91 days	X	X	Х	X
Cycle duration	20 (1) 366 days	91 days	Х	Х	Х	Х
HM follow-up visits (Remote Scheduling)	Any day; any day between Monday and Friday; Monday; Tuesday; Wednesday; Thursday; Friday; Saturday; Sunday	Any day	X	X	X	X

Diagnostics

The following recording parameters can be set:

Parameter	Range of values	Standard	VR	DX	DR	HF
For AT/AF	OFF; ON	ON	'	Х	Х	Х
	Series 7: Extended ON					
For SVT	OFF; ON	ON	Х	Х	Х	Х
FornsT	OFF; ON	ON	Х	Х	Х	Х
For CRT pacing inter- ruption	OFF; ON	ON				X
Periodic recording	When Home Monitoring is deactivated: OFF; 30 (30) 180 days	90 days	Х	X	X	X
IEGM configuration	RA, RV, LV RA, RV, FF FF, RV, LV	RA, RV, LV				X

The following statistical parameters can be set:

Parameter	Range of values	Standard	VR	DX	DR	HF
Start resting period	00:00 (1:00 AM) 11:00 PM hh:mm	02:00 hh: mm	X	Х	X	Х
Duration of resting period	0.5 (0.5) 12 h	4 h	Х	Х	X	X
AV delay adjustment in sensing test	OFF; 300 ms	300 ms		Х	Х	Х
Series 5 and 7: Thoracic impedance (TI)	OFF, ON	OFF	X	X	Х	X

MRI Program

Parameter Range of values Standar		Standard	VR	DX	DR	HF
MRI program	OFF; AUTO; ON	OFF	Х	Х	Х	Х
Expiration date	Today (1) Today + 14 days	Today + 14 days	Х	Х	Х	Х
Mode	V00; OFF	OFF	Х	Х		
	V00; D00; OFF	OFF			Х	
	V00; V00-BiV; D00; D00-BiV; OFF	OFF				X
Basic rate	70 (5) 100 (10) 160 bpm	90 bpm	Х	Х	Х	Х
Pulse amplitude LV	As in permanent program; 0.5 (0.25) 4.0 (0.5) 6.0; 7.5 V	As in perma- nent program				X
Pulse width LV	As in permanent program; 0.4; 0.5 (0.25) 1.5 ms	As in perma- nent program				X
Pacing polarity LV	IS-1: LV1 -> LV2 LV2 -> LV1 IS4: LV1 -> LV2 LV1 -> LV4 LV1 -> LV4 LV2 -> LV1 LV2 -> LV1 LV2 -> LV3 LV3 -> LV4 LV3 -> LV4 LV3 -> LV4 LV3 -> LV1 LV3 -> LV1 LV4 -> LV2 LV4 -> LV4 LV4 -> LV4	As in perma- nent program				X

3.2 Technical Data

Mechanical Characteristics

Housing

Devices with header for DF4 connector

Туре	Lead connector	W x H x D in mm	Volume [cm³]	Mass g
VR	DF4	60 x 61.5 x 10	30	75
VR DX	DF4	60 x 66.5 x 10	32	77
DR	DF4	60 x 66.5 x 10	32	77
HF	DF4	60 x 71.5 x 10	33	78
HF QP	DF4	60 x 75 x 10	35	82

Materials in contact with body tissue

• Housing: titanium

• Header: epoxy resin, polysulfone; DF4 seal: silastic

• Header: epoxy resin, polysulfone

• Silicone plugs and blind plugs (if applicable): silopren or silastic

X-ray identification



Electrical Characteristics

Standards

The specifications are made according to ISO 14708-6:2010(E).

Measuring conditions

Unless otherwise indicated, all specifications refer to the following conditions:

• Ambient temperature: 37°C ± 2°C

• Pacing/Sensing: $500 \Omega \pm 1\%$

• Shock: $50 \Omega \pm 1\%$

Factory settings

Arrhythmia zones VT1, VT2, VF: OFF

• Antibradycardia pacing: OFF

Home Monitoring: OFF

Telemetry data for Home Monitoring

MICS frequency: 402-405 MHz

• Maximum power of transmission: < 25 μW (16 dBm)

International radio certification

Devices with BIOTRONIK Home Monitoring® are equipped with an antenna for wireless communication.

• Telemetry information for Australia:

This product is in compliance with the Australian "Radiocommunications Act 1992", and, therefore, it is labeled according to the "Radiocommunications (Compliance Labeling – Devices) Notice".

• Telemetry information for Canada:

This device must neither interfere with meteorological and earth resources technology satellites nor with meteorological stations working in the 400.150 to 406.000 MHZ band, and it must accept any interference received, including interference that may cause undesired operation.

This device will be registered with Industry Canada under the following number:

IC: 4708A-ICD4200

The code IC in front of the certification/registration number only indicates that the technical requirements for Industry Canada are met.

• Telemetry information for the USA:

This transmitter is authorized by rule under the Medical Device Radiocommunication Service (in Part 95 of the FCC Rules) and must not cause harmful interference to stations operating in the 400.150 to 406.000 MHz band in the Meteorological Aids (i.e., transmitters and receivers used to communicate weather data), the Meteorological Satellite, or the Earth Exploration Satellite Services and must accept interference that may be caused by such stations, including interference that may cause undesired operation. This transmitter shall only be used in accordance with the FCC Rules governing the Medical Device Radiocommunication Service. Analog and

Technical Data

digital voice communications are prohibited. Although this transmitter has been approved by the Federal Communications Commission, there is no guarantee that it will not receive interference or that any particular transmission from this transmitter will be free from interference.

This device will be registered with the Federal Communications Commission under the following number:

FCC-ID: QRI-ICD4200

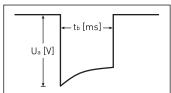
• Telemetry information for Japan:

In accordance with Japanese law, this device has been assigned an identification number under the "Ordinance concerning certification of conformity with technical regulations, etc., of specified radio equipment", Article 2-1-8.

R202-SMG025

Pulse waveform

The pacing pulse has the following form:



The pulse amplitude reaches its maximum value at the beginning of the pulse (Ua). With increasing pacing duration (tb), the pulse amplitude is reduced dependent on the pacing impedance.

Resistance to interference

- Note on device type VR DX (only devices with a DF4/IS-1 connection): The EMC requirements are met as long as atrial sensitivity is set to 1.0 mV (factory settings) or values ≥ 1.0 mV. Measures must be taken to assure interference-free therapy if more sensitive values are set.
- Note on device type HF and HF QP: In the case of unipolar sensing, the requirement for interference voltages of < 0.3 mV (peak-to-peak) is met.

Common mode rejection ratio

Information for device type HF also applies to device type HF QP.

Rate	Common mode rejection ratio			
	Atrium: DX	Atrium: DR, HF	V right: VR, DR, HF	V left: HF
16.6 Hz	73 dB	66 dB	65 dB	58 dB
50 Hz	74 dB	69 dB	69 dB	59 dB
60 Hz	73 dB	70 dB	71 dB	62 dB

Technical Data

ATP amplitude

A burst was measured at 500 Ω , an amplitude of 7.5 V (tolerance \pm 1.5 V), pulse width of 1.5 ms, R-S1 interval of 300 ms and an S1 count of 5:

ATP amplitude	Measured minimum	Measured maximum
RA	7.42 V	7.46 V
RV	7.41 V	7.44 V
LV	7.44 V	7.47 V

Automatic sensitivity control

Measurement of actual values and test signal wave shape: standard triangle. For the device type VR DX, the programmed atrial sensitivity is amplified by a factor of 4.

Sensitivity	Value	Tolerance	Measured value
A: positive	0.2 mV	0.2 0.5	0.32 mV
A: negative	0.2 mV	0.2 0.5	0.31 mV
DX: A: positive	0.2 mV	0.2 0.52 (0.05 to 0.13)	0.11 mV
DX: A: negative	0.2 mV	0.2 0.52 (0.05 to 0.13)	0.11 mV
RV: positive	0.5 mV	0.3 0.7	0.58 mV
RV: negative	0.5 mV	0.3 0.7	0.55 mV
LV: positive	0.5 mV	0.3 0.7	0.54 mV
LV: negative	0.5 mV	0.3 0.7	0.55 mV

Shock energy / peak voltage

With shock path: RV to housing + SVC

Shock energy (Tolerance)	Tolerance peak voltage	Measured value shock energy	Measured value peak voltage
1 J (0.7 1.18)	90 120 V	0.79 J	101 V
20 J (15.9 21.6)	470 510 V	18.20 J	486 V
40 J (33.8 41.4)	670 730 V	37.30 J	684 V

Battery Data

Battery characteristics

The following data is provided by the manufacturers:

Manufacturer	GREATBATCH, INC. Clarence, NY 14031	LITRONIK GmbH 01796 Pirna, Germany		
Battery type	GB 3493	LiS 2592		
System	Li/SVO/CFx	LiMn02		
Battery ID number shown on the programmer	8	9		
Device type	VR, VR DX, DR, HF, HF QP			
Battery voltage at ERI	2.5 V	2.85 V		
Charge time at BOS	8 s	8 s		
Charge time at ERI	10 s	10 s		
Usable capacity until ERI VR, VR DX, DR, HF, HF QP	1770 mAh	1600 mAh		
Usable capacity until EOS	1900 mAh	1730 mAh		

Storage period

The storage period affects the battery service time.

- Devices should be implanted within 25 months between the manufacturing date and the use by date (indicated on the package).
- If the ICD is implanted shortly before the use by date, the expected service time may be reduced by 16.4 months on average.

Calculation of service times

- The service times have been calculated as follows in all chambers depending on the device type:
 - Pulse amplitude: 2.5 V
 - Pulse width: 0.4 ms
 - Pacing impedance: $500 \Omega \pm 5\%$
 - Basic rate VR, VR DX: 40 bpm Basic rate DR, HF, HF QP: 60 bpm
- Home Monitoring: ON, 1 device message each day and 24 IEGM-Online HD transmissions per year
- Diagnostic functions and recordings: permanently set
- Capacitor reforming is performed 2 times per year and therefore at least 2 maximum charges for shocks have to be assumed per year even if less than 2 are delivered.

Calculation of the number of shocks

Calculation of the maximum number of shocks = service time [years] x number of shocks per year

Rivacor 3/5/7 VR-T

Service times with GB 3493 or LiS 2592 battery:

Pacing	Service time [in years] at number of shocks per year					
	2	4	8	12	16	20
0%	15.4	13.3	10.5	8.7	7.4	6.4
15%	15.1	13.1	10.4	8.6	7.3	6.4
50%	14.3	12.5	10.0	8.3	7.1	6.2
100%	13.4	11.8	9.5	8.0	6.9	6.0

Rivacor 5/7 VR-T DX

Service times with GB 3493 or LiS 2592 battery:

Pacing	Service time [in years] at number of shocks per year					
	2	4	8	12	16	20
0%	14.1	12.5	10.0	8.3	7.1	6.2
15%	13.8	12.3	9.8	8.2	7.0	6.1
50%	13.3	11.8	9.5	8.0	6.9	6.0
100%	12.5	11.1	9.1	7.7	6.6	5.8

Rivacor 3/5/7 DR-T

Service times with GB 3493 or LiS 2592 battery:

Pacing	Service time	ervice time [in years] at number of shocks per year						
	2	4	8	12	16	20		
0%	14.1	12.5	10.0	8.3	7.1	6.2		
15%	13.3	11.8	9.5	8.0	6.9	6.0		
50%	11.7	10.5	8.7	7.4	6.4	5.7		
100%	10.0	9.1	7.7	6.6	5.8	5.2		

Rivacor 3/5/7 HF-T, Rivacor 3/5 HF-T QP

Service times with GB 3493 or LiS 2592 battery:

Pacing	Service time [in years] at number of shocks per year						
	2	4	8	12	16	20	
0%	13.0	11.6	9.5	7.9	6.8	6.0	
15%	12.0	10.8	8.9	7.5	6.5	5.8	
50%	10.2	9.3	7.8	6.7	5.9	5.3	
100%	8.3	7.6	6.6	5.8	5.2	4.7	

Rivacor 7 HF-T QP

Service times with GB 3493 or LiS 2592 battery, without MultiPole Pacing:

Pacing	Service time [in years] at number of shocks per year					
	2	4	8	12	16	20
0%	13.0	11.6	9.5	7.9	6.8	6.0
15%	12.0	10.8	8.9	7.5	6.5	5.8
50%	10.2	9.3	7.8	6.7	5.9	5.3
100%	8.3	7.6	6.6	5.8	5.2	4.7

Service times with GB 3493 or LiS 2592 battery, with MultiPole Pacing:

Pacing	Service time	Service time [in years] at number of shocks per year				
	2	4	8	12	16	20
0%	12.9	11.5	9.4	7.9	6.8	6.0
15%	11.7	10.5	8.7	7.4	6.4	5.7
50%	9.4	8.6	7.3	6.4	5.6	5.1
100%	7.3	6.8	6.0	5.3	4.8	4.4

Legend for the Label

The label icons symbolize the following:

سا	Manufacturing date	Use by				
1	Storage temperature REF	Order number				
SN	Serial number PID	Product identification number				
4	Dangerous voltages (€	CE mark				
	Contents	Screwdriver				
manuals.biotronik.com	Follow the electronically available instructions for use!	Follow the instruc- tions for use!				
STERILEEO	Sterilized with ethylene oxide	Non-sterile				
STERMIZE	Do not resterilize	Single use only. Do not re-use!				
	Do not use if packaging is damaged					
(((•)))	Transmitter with non-ionizing radiation at designated frequency					
MR	MR conditional					
TP2	Compatibility with telemetry protocol version 2 of BIOTRONIK Home Monitoring					
Example	Device: NBG code and compatible leads Factory settings for therapy: OFF					
	Examples of the header configuration: DF4/IS-1 • DF4/IS4/IS-1					

Rivacor 3/5/7 ICD Family

VR-T, VR-T DX, DR-T, HF-T, HF-T QP



Revision: C (2019-10-16)

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